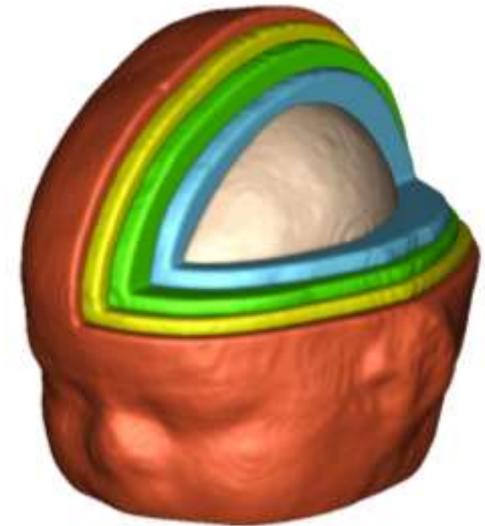


# Spatiotemporal Analysis of Brain Development and Disease Progression

Guido Gerig

Scientific Computing and Imaging  
Institute (SCI), University of Utah



COLLÈGE  
DE FRANCE  
—1530—



THE BRAIN INSTITUTE  
— THE UNIVERSITY OF UTAH



# Collège de France

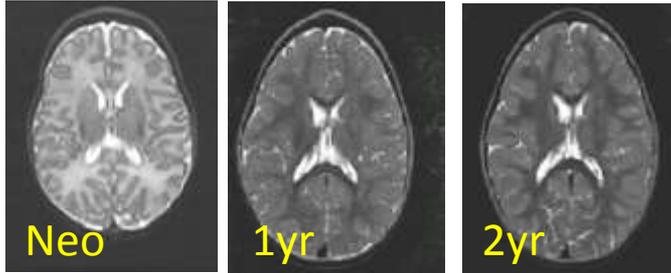
Its motto is *Docet omnia*:  
“All things are taught”.



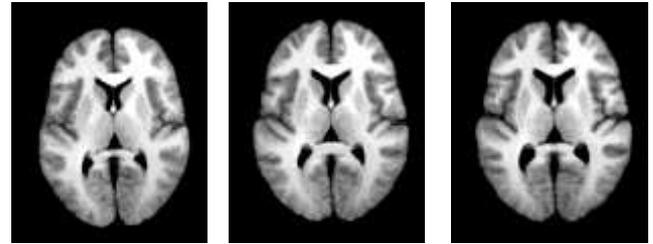
***Ayache Symposium: From Medical  
Images to Computational Medicine***

# Longitudinal/Serial Image Data

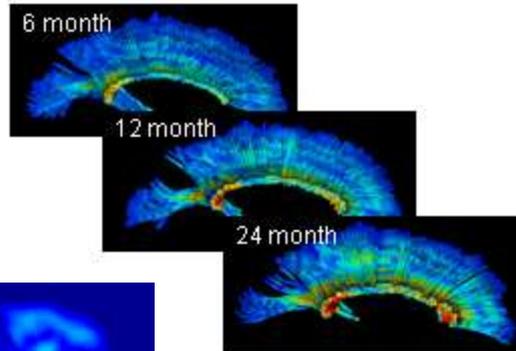
## Pediatrics: Brain Growth



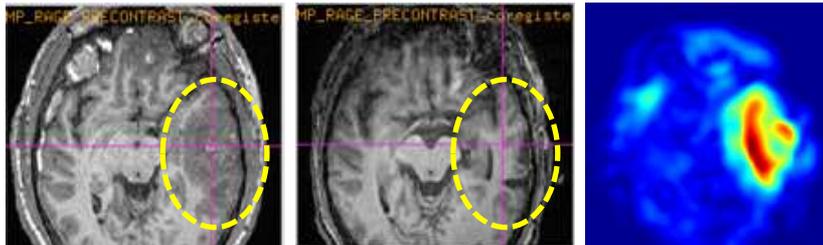
## Aging / Neurodegeneration



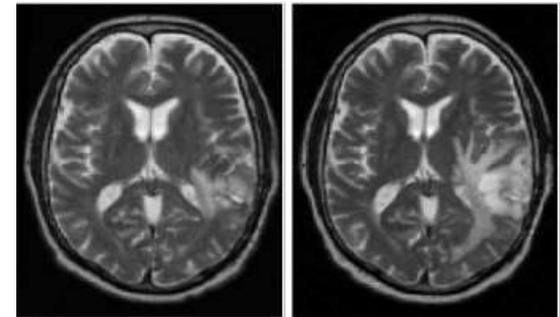
## WM Maturation



## Trauma: Baseline – Follow-up



## Tumor Growth



- Image analysis technology for 4-D data is lagging behind acquisition
- Often: individual time-point analysis, ignores causality of repeated imaging

# Spatiotemporal Modeling: Natural Task in Clinical Reasoning

## Motivation:

Development, degeneration, monitoring therapeutic interventions are dynamic processes.

## Clinical terminology:

Departure from typical development, deviation from healthy

Typical but delayed growth patterns, catch-up, atypical development

Analysis of recovery for a patient

Prediction of onset of clinical symptoms

Monitoring of efficacy of treatment

Personalized health care: Individual trajectories compared to expected “norm”.

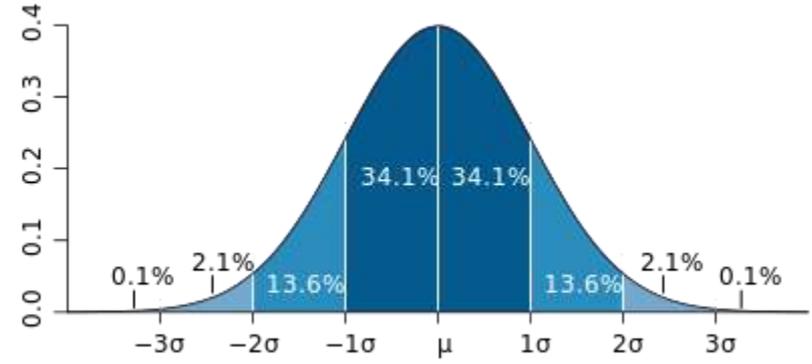
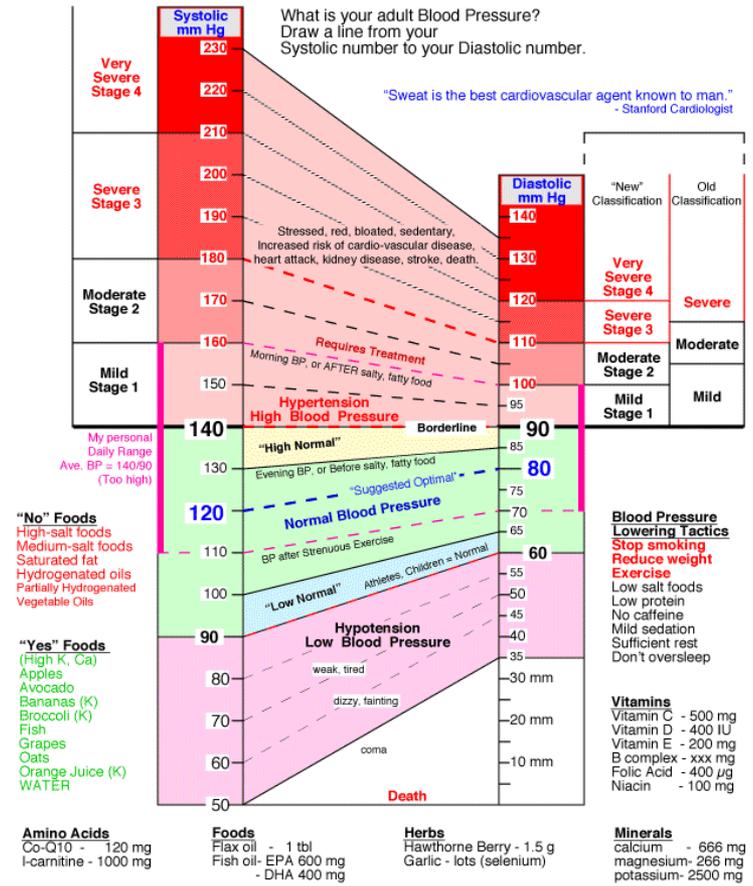
→ **Focus on longitudinal design & longitudinal analysis**

# Normative Data

Vaughns-1-Pageys.com

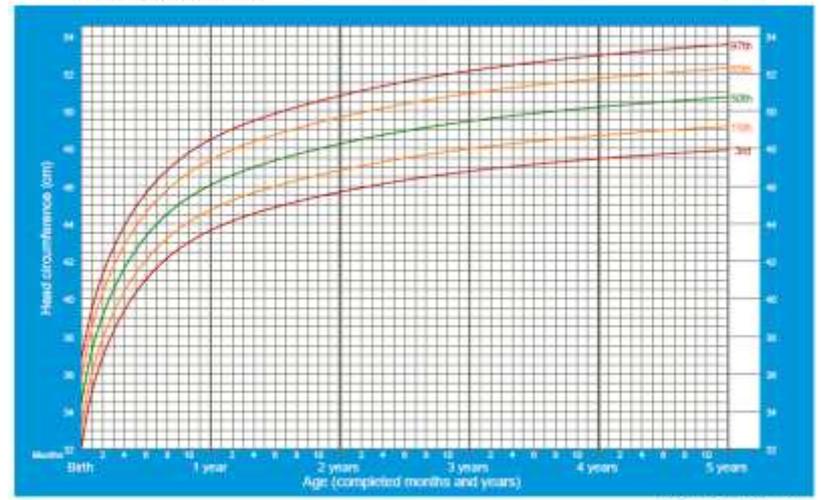
MedicalSummaries

## Blood Pressure Chart



## Head circumference-for-age BOYS

Birth to 5 years (percentiles)

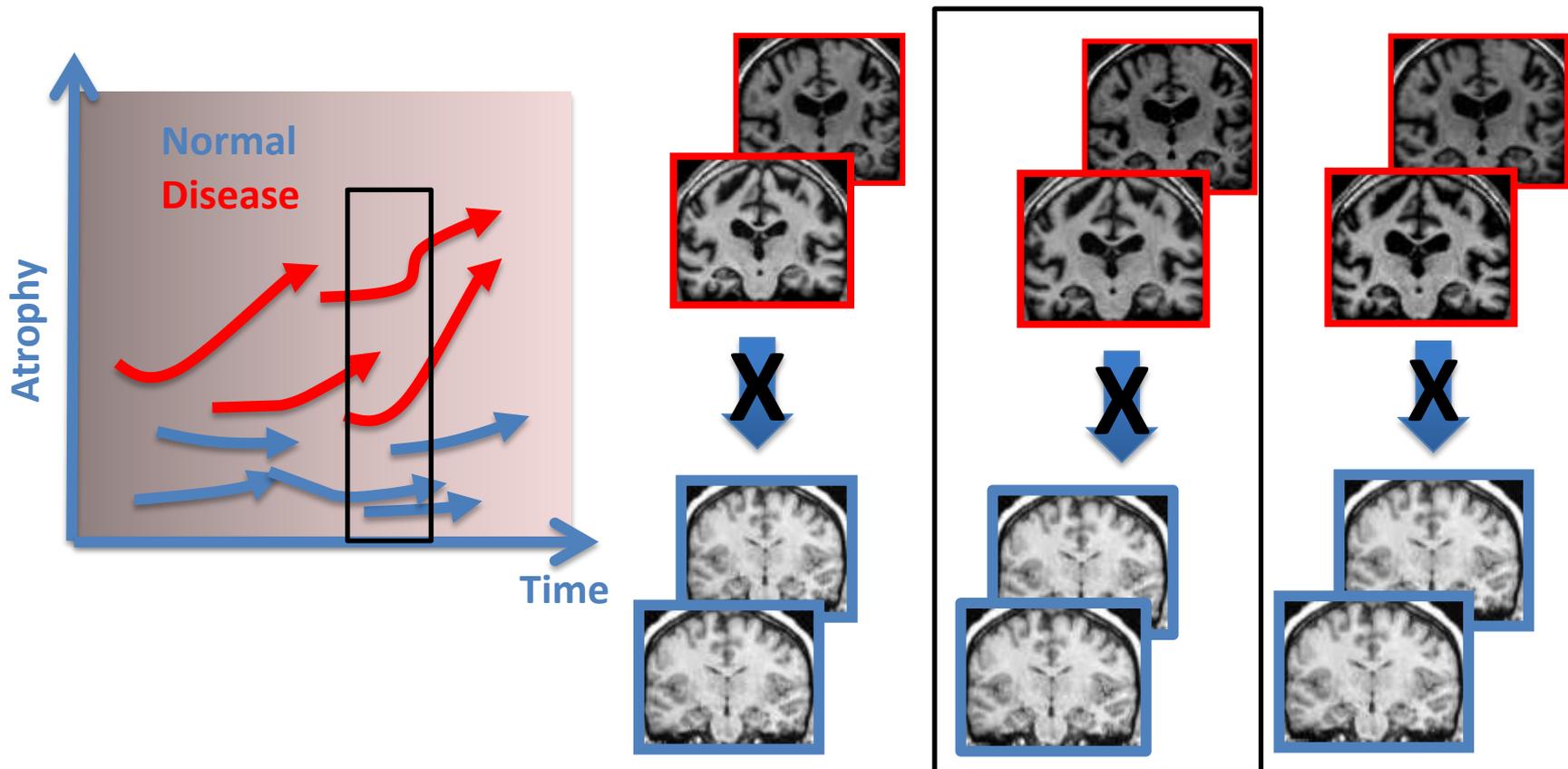


These are the personal thoughts of the author - nothing is implied, promised or guaranteed - no advice is intended.

Frame: md-11.blood-pressure.18

# Spatiotemporal Morphometry

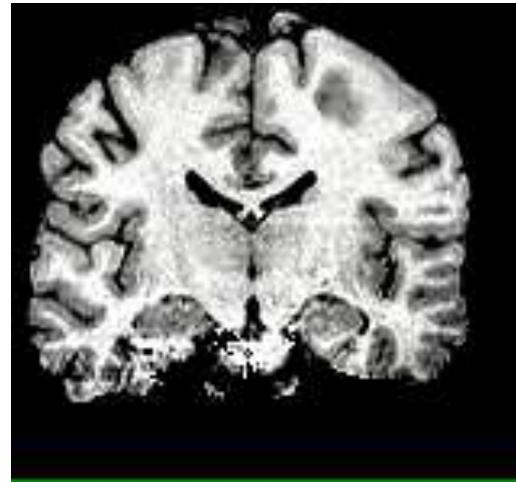
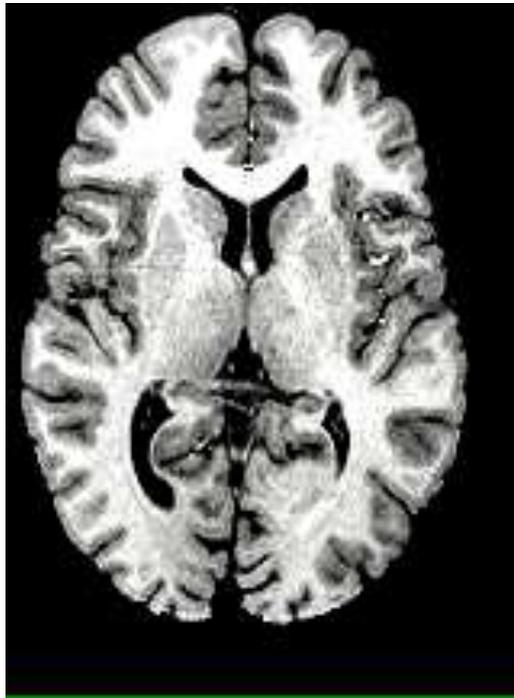
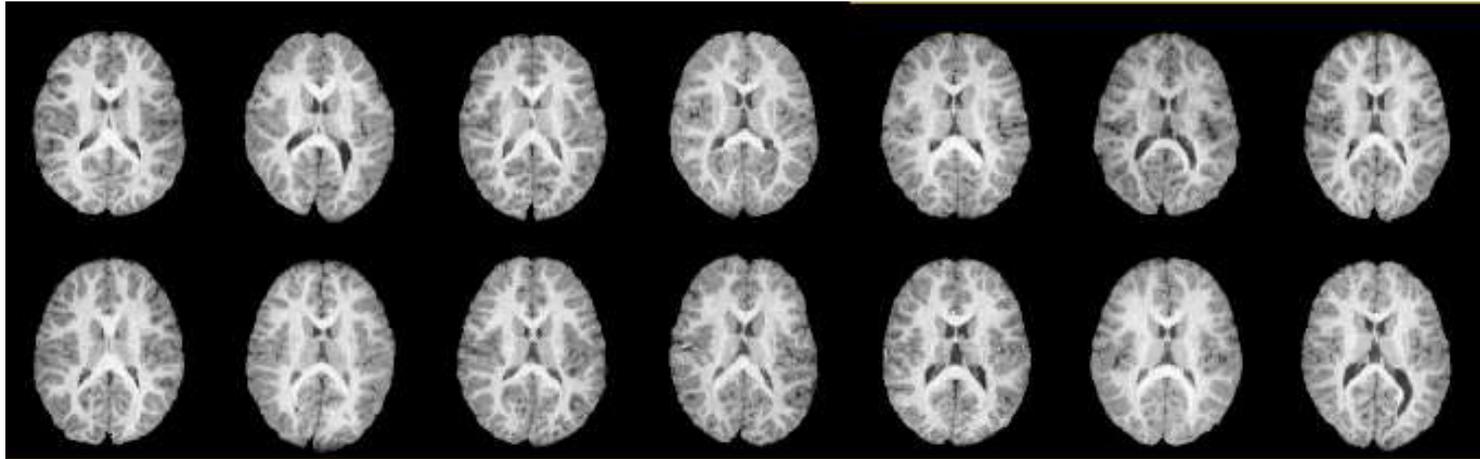
Cross-sectional paradigm



Inter-subject variability  $\gg$  Intra-subject changes

Courtesy of Lorenzi & Pennec, INRIA

# Population Variability

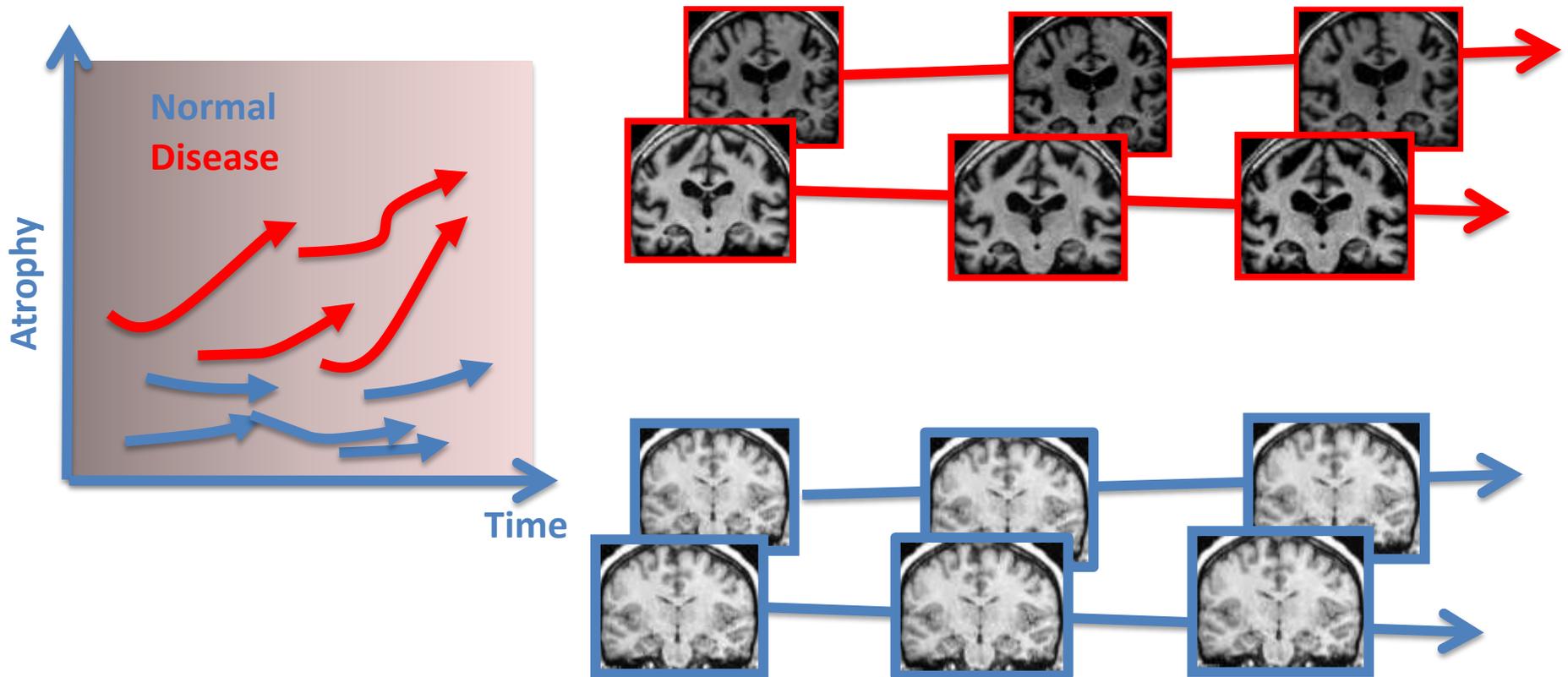


Normal Aging (50 subjects, 20 to 70 years)

Courtesy S. Joshi

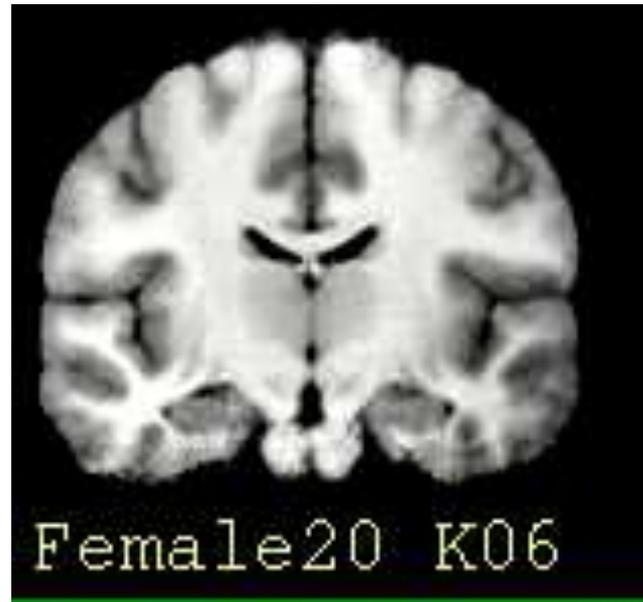
# Spatiotemporal Morphometry

Longitudinal paradigm



courtesy of Lorenzi & Pennec, INRIA

# Aging Brain via Population Shape: Manifold Kernel Regression



- B. Davis, S. Joshi, T. Fletcher, E. Bullitt, (UNC/Utah)
- D. Marr Prize, ICCV'07

# Clinical Driving Problem: Huntington's Disease (HD)

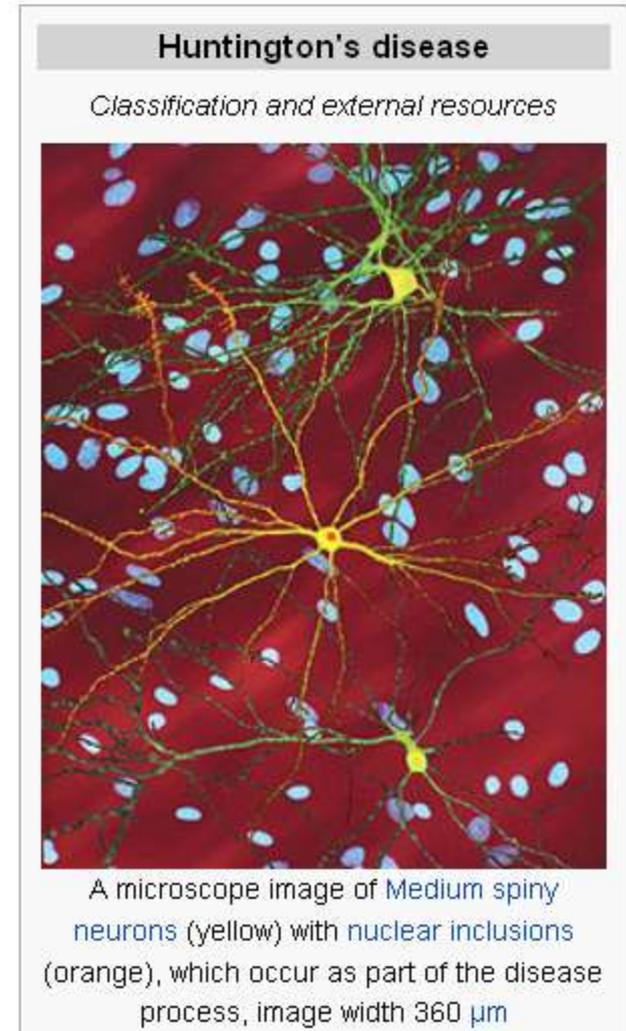
- Neurodegenerative genetic disorder, hereditary disease.
- Causes severe debilitating symptoms by middle age.
- All affected individuals have the same root cause: Huntingtin gene.
- **NIH: PREDICT-HD Study:** Define neurobiological **progression** of HD in at-risk individuals so that therapies can be performed before symptoms reach a debilitating stage.
- Collaboration with U of Iowa via NA-MIC.



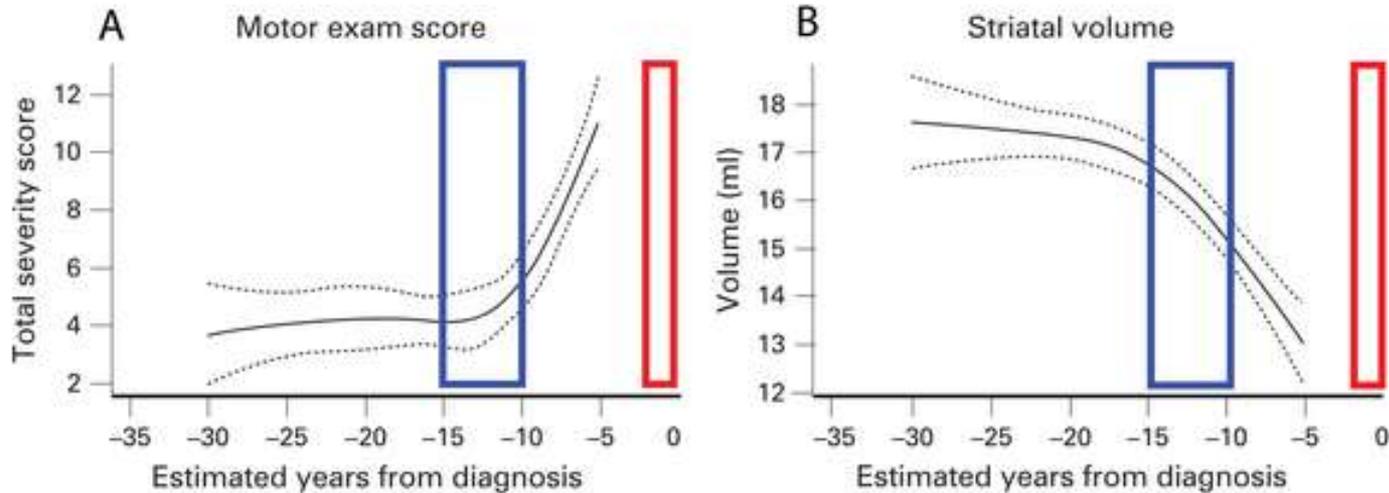
**National Alliance for Medical Image Computing**

A National Center for Biomedical Computing  
Funded under the NIH Roadmap Initiative

Google™ Duster



# PREDICT-HD



Relationship between estimated years to diagnosis of Huntington's disease and motor exam score (A) and striatal volumes (B).

Red indicates most likely time of diagnosis. Blue line is proposed time period when interventional therapies would have greatest impact.

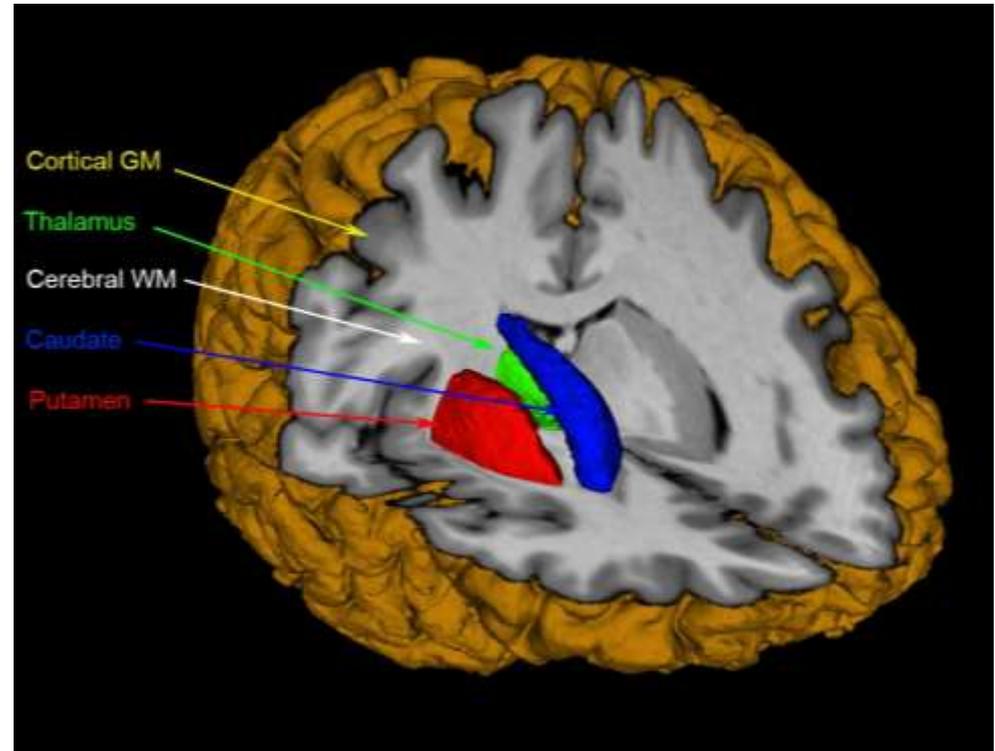
→ PREDICT Study: Longitudinal imaging study (3-5 scans 2yr intervals).

# PREDICT-HD



Search for noninvasive biomarker with imaging...

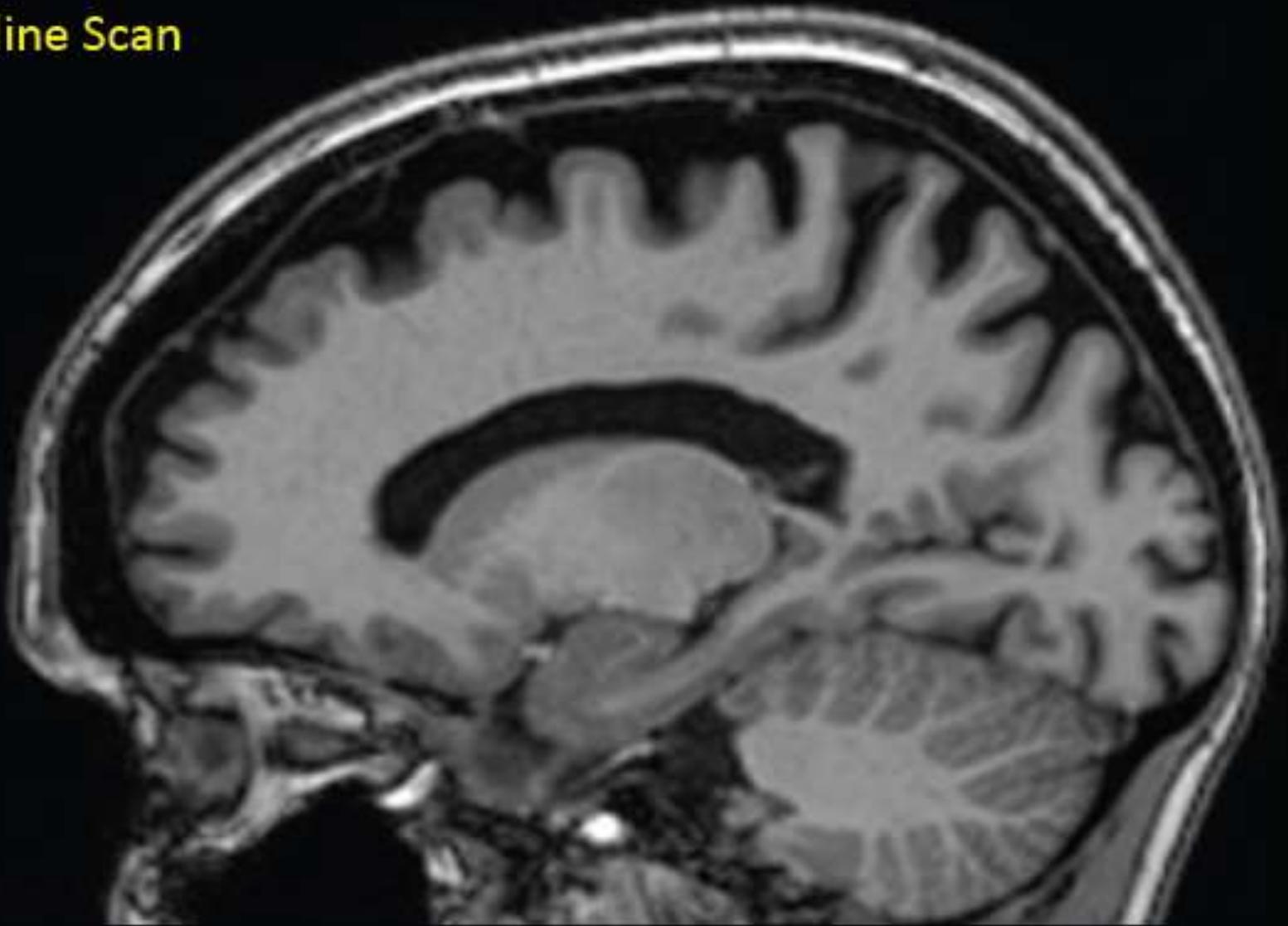
- Symptomatic HD imaging findings
  - Atrophied caudate and putamen
  - Disproportionate loss of white matter
- Prodromal HD imaging findings
  - Striatal atrophy correlates with:
    - Neurological impairment
    - Poorer performance on cognitive assessments
    - Years to motor symptom onset



Courtesy Jane Paulsen, Hans Johnson, U-Iowa

# TRACK-HD Stage 1 HD Subject

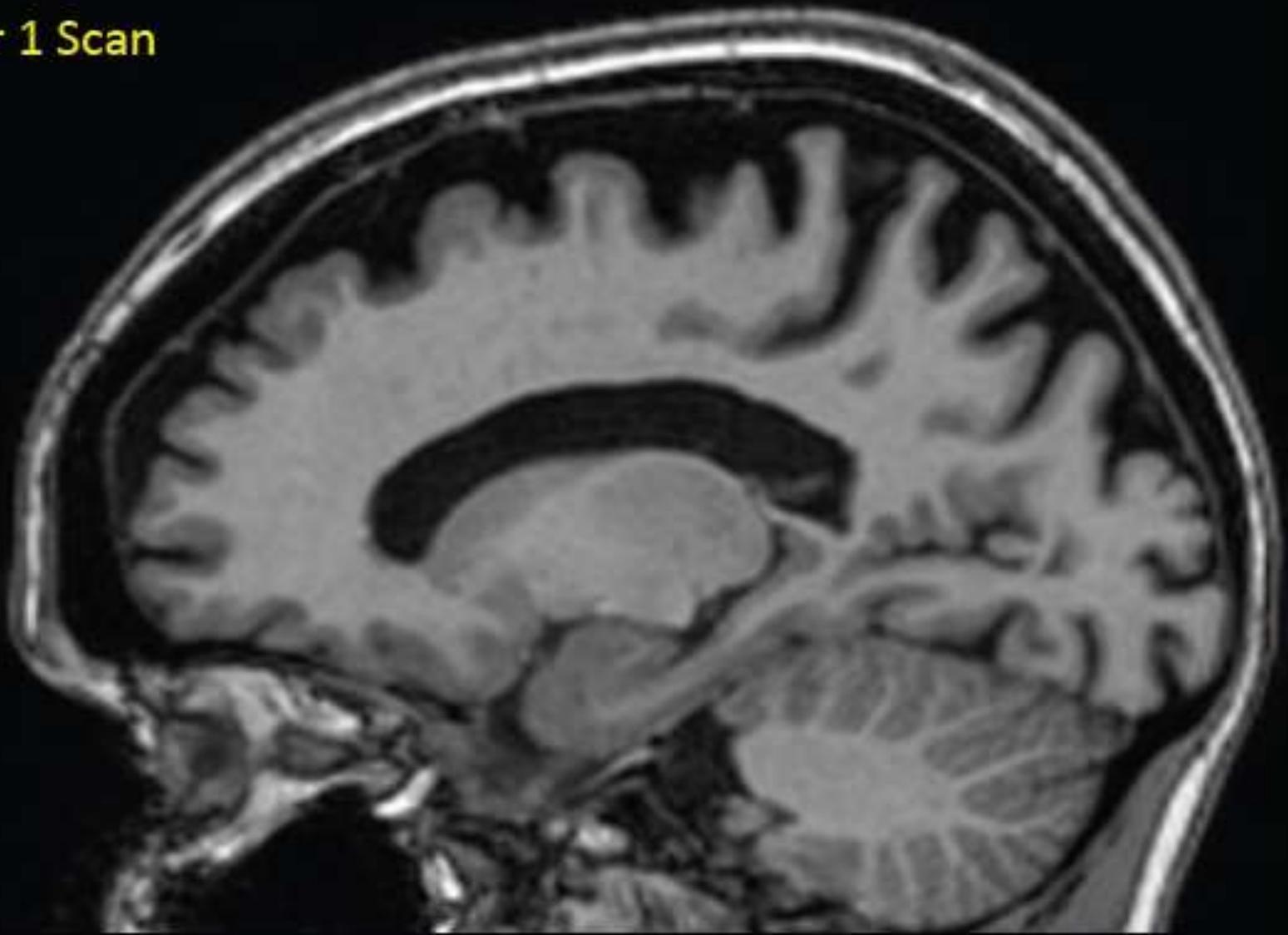
Baseline Scan



Courtesy Hans Johnsen, Jane Paulsen, IOWA

# TRACK-HD Stage 1 HD Subject

Year 1 Scan

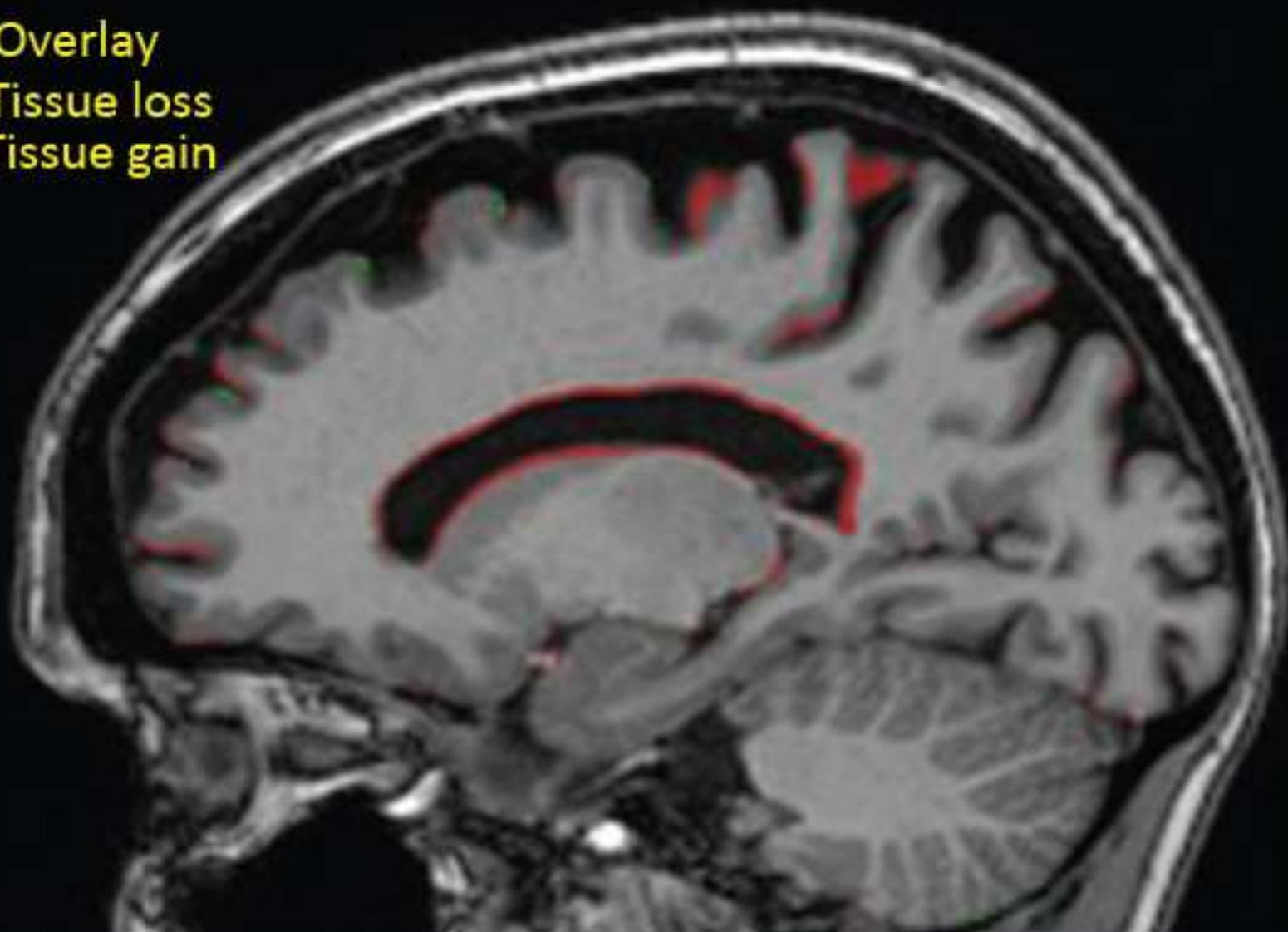


Courtesy Hans Johnsen, Jane Paulsen, IOWA

# TRACK-HD Stage 1 HD Subject

BSI Overlay

- Tissue loss
- Tissue gain



Atrophy Rate: 1.9%    Premanifest Rate: 0.7%    Control Rate: 0.2%

# Clinical Driving Problem: Understanding Early Development



## Brain Development in High Risk Children

- Understanding rate and variability of normal development
- Detect differences from typical development (autism, drug addiction, alcohol)
- **Early diagnosis → early therapy → better life quality and future for infants and families**

# Early Brain Development Studies



EDDS HOME

- John Gilmore, M.D.  
*Principal Investigator*
- Studies
- Investigators
- Image Analysis
- Progress/Publications
- Training Opportunities
- Links
- Contact Us

## Early Brain Development Studies

[Normal Controls](#)

[Twins](#)

[Mild Ventriculomegaly \(MVM\) \(Brain\)](#)

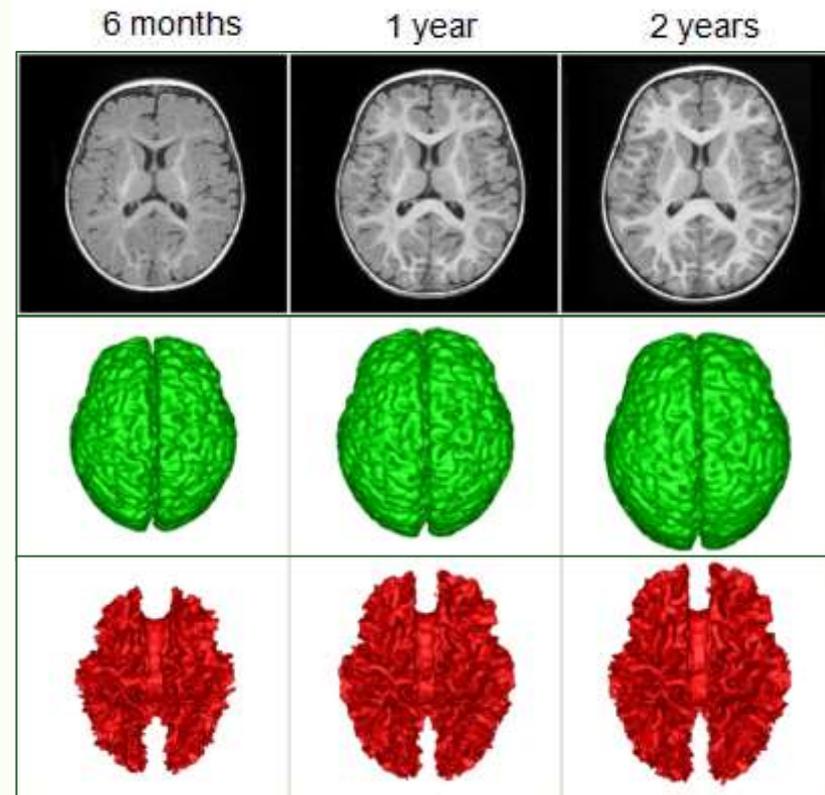
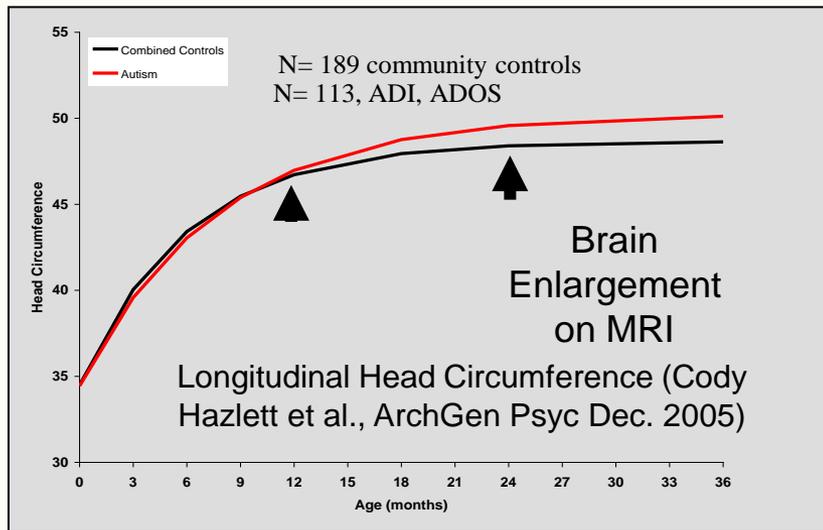
[Babies of Mothers with Schizophrenia](#)

**Offsprings of cocaine-addicted mothers**

## Neonatal Brain Development in High Risk Children (J. H. Gilmore, MD)

- Understanding rate and variability of normal development
- Detect differences from typical development
- Early diagnosis → early therapy → help families

# Autism: Longitudinal Infant Neuroimaging Study



Brain enlargement in autism starts at year 1.  
Why? What? Effect?

**Autism-Centers-Excell.-IBIS NIH Study:**  
UNC, McGill, Seattle, WU, CHOP, Utah  
Longitudinal MRI/DTI study, > 1500 MRI/DTI

**Better understanding → Early intervention to improve outcome**



# Brain Development in Autism: Infant Siblings



Home

Study Goal

What is MRI?

Why Study Siblings?

Study Sites

**Seattle**



**Montreal**



**Salt Lake City**



**St Louis**



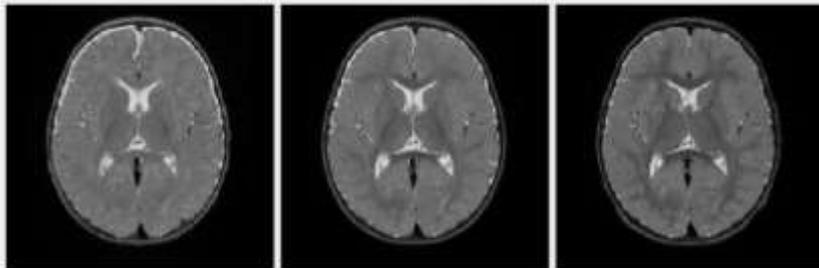
**Philadelphia**



**Chapel Hill**



**Longitudinal scans at 6, 12, 24 months**



**Goal: Pre-diagnostic imaging biomarkers  
PI: Dr. Joseph Piven, UNC**

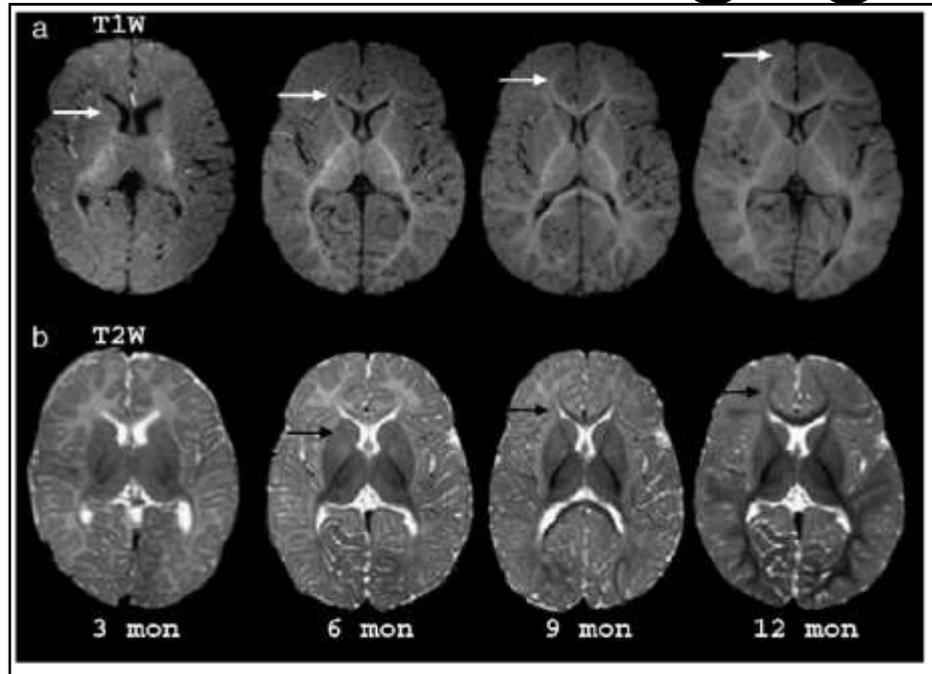
# ACE: Autism Network of Excellence

## Infant Brain Imaging Study IBIS

- P.I. Joseph Piven, UNC
- ACE grant: Autism Center of Excellence.
- Longitudinal study of infant siblings at risk for Autism scanned at **6mo, 1y and 2yr (total >1500 MRI/DTI)**
- 4 scanning sites:
  - Seattle
  - St Louis
  - Philadelphia
  - Chapel Hill
- DCC: MNI Montreal
- Image analysis: Utah & UNC



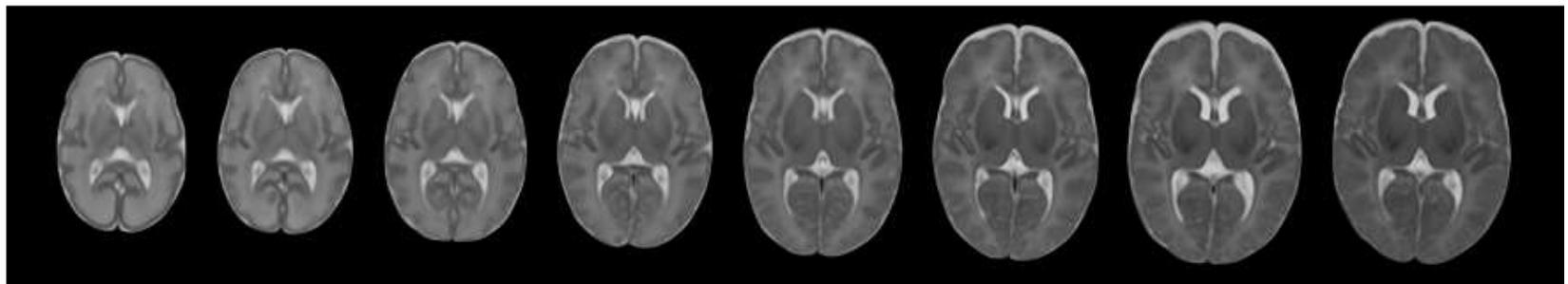
# Longitudinal Magnetic Resonance Imaging (MRI)



Paus et al. 2001



Courtesy LeBihan 2005



A. Serag et al., Neuroimage, 2012

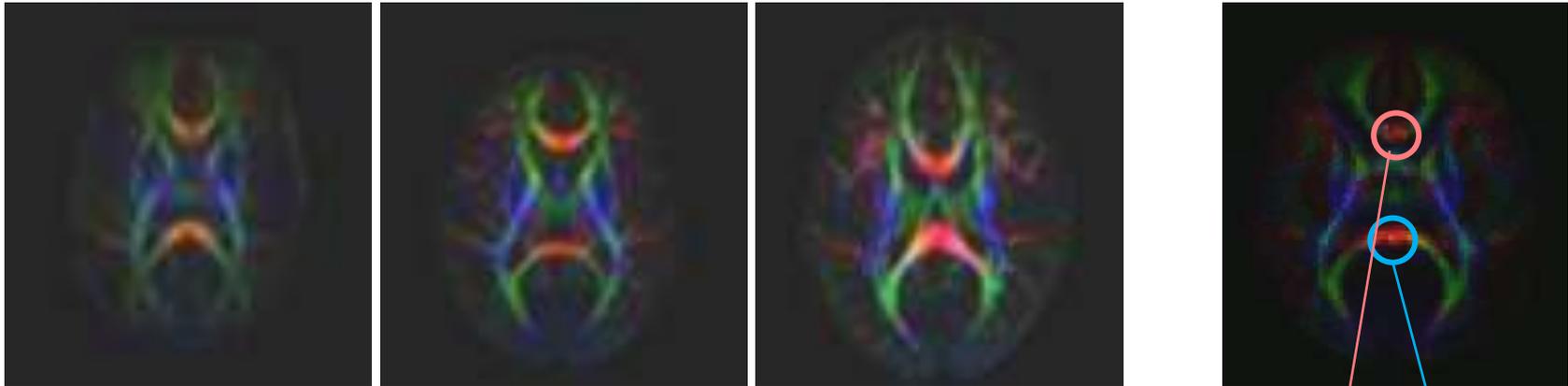
# Longitudinal MR Diffusion Imaging

Neonate

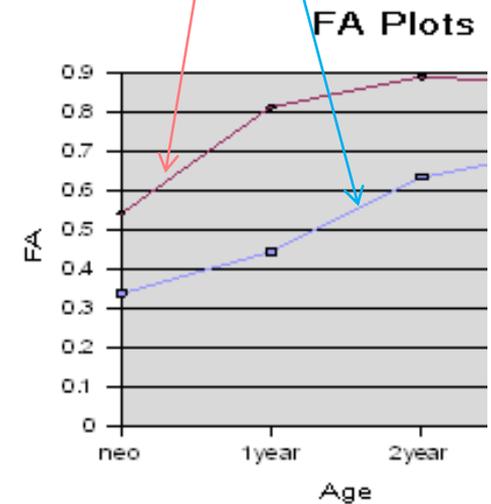
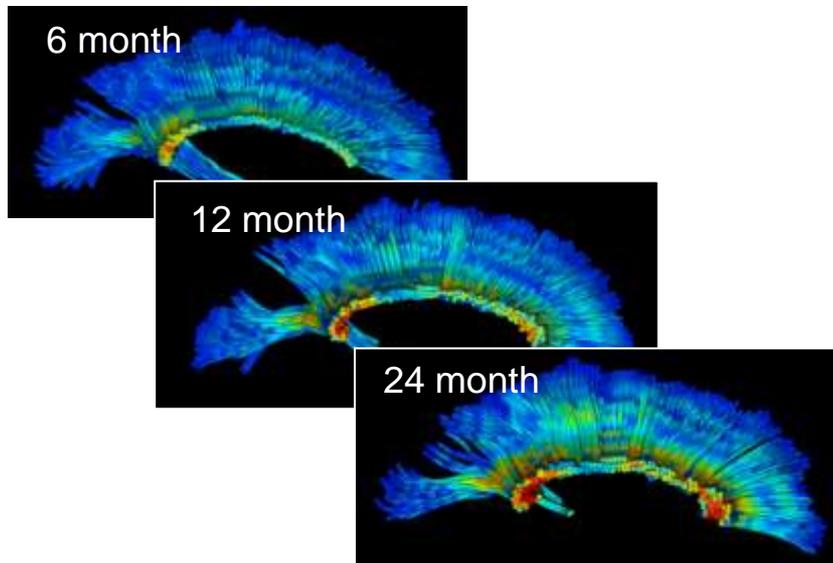
1 year

2 years

Cine

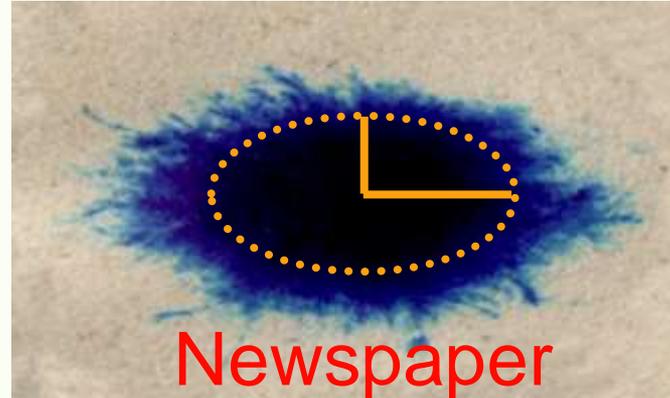


FA



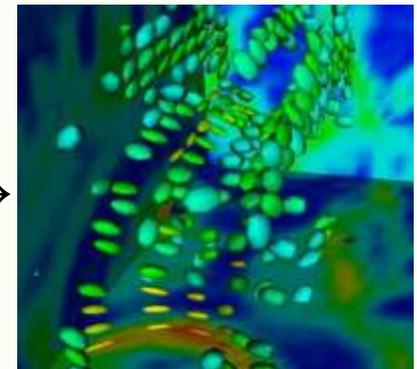
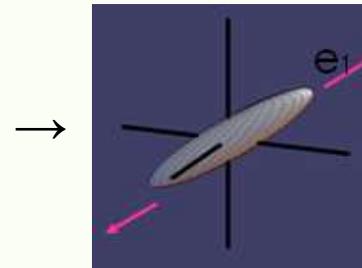
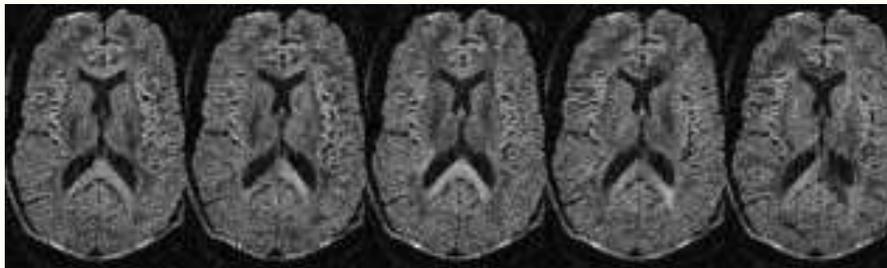
# Diffusion in Biological Tissue

- Brownian motion of water through tissue

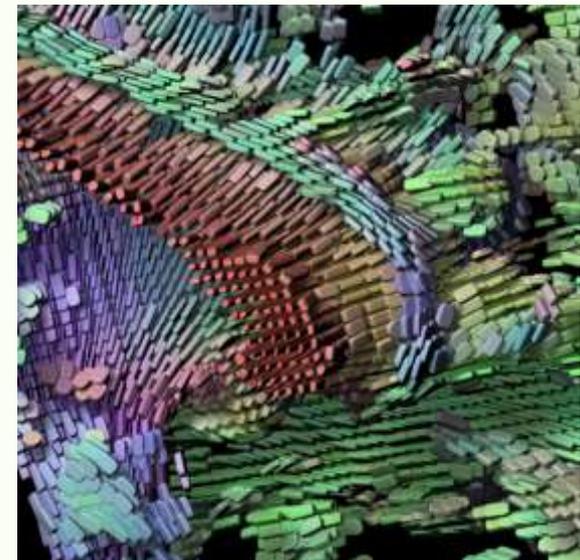
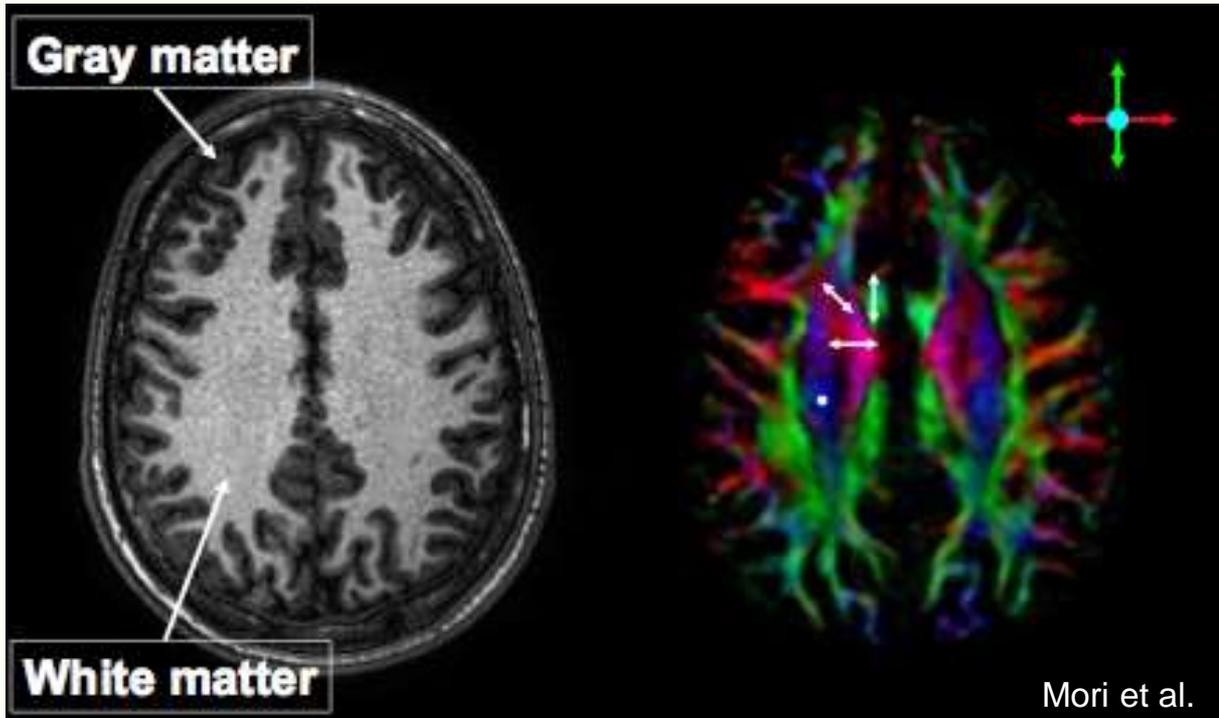


G. Kindlmann

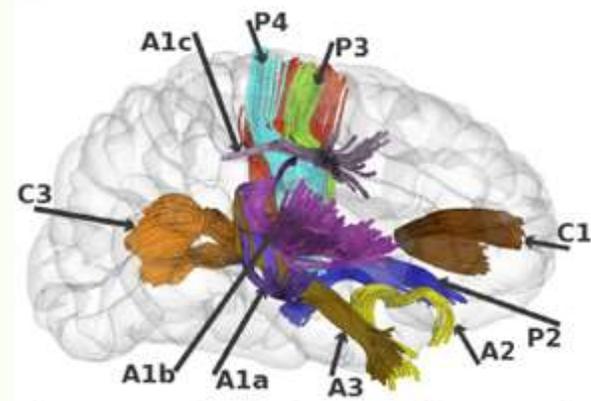
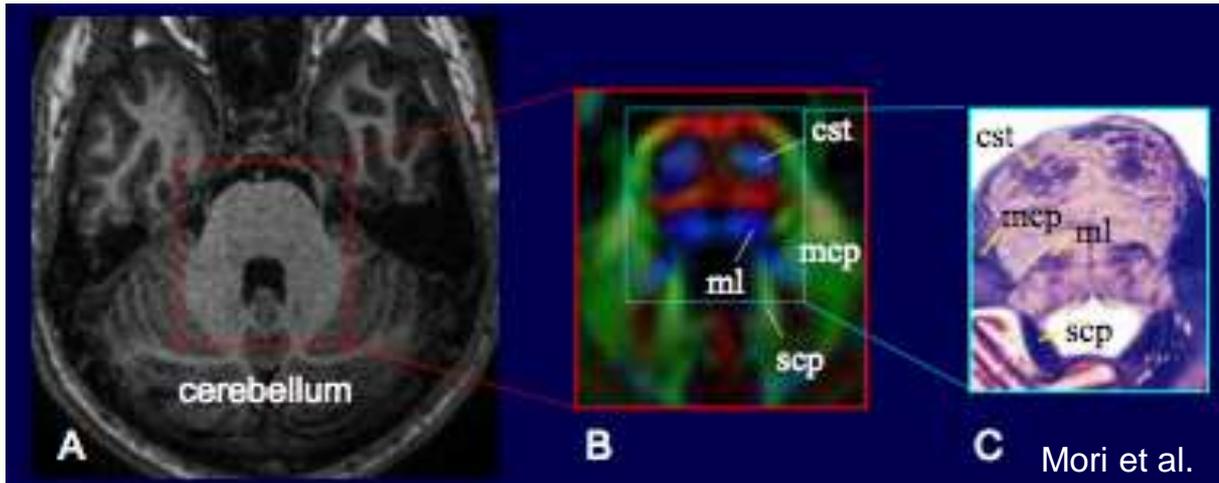
- Anisotropy: diffusion rate depends on direction
- Le Bihan 1984 (C R Acad Sci): Diffusion MRI



# Diffusion tensor imaging reveals white matter anatomy



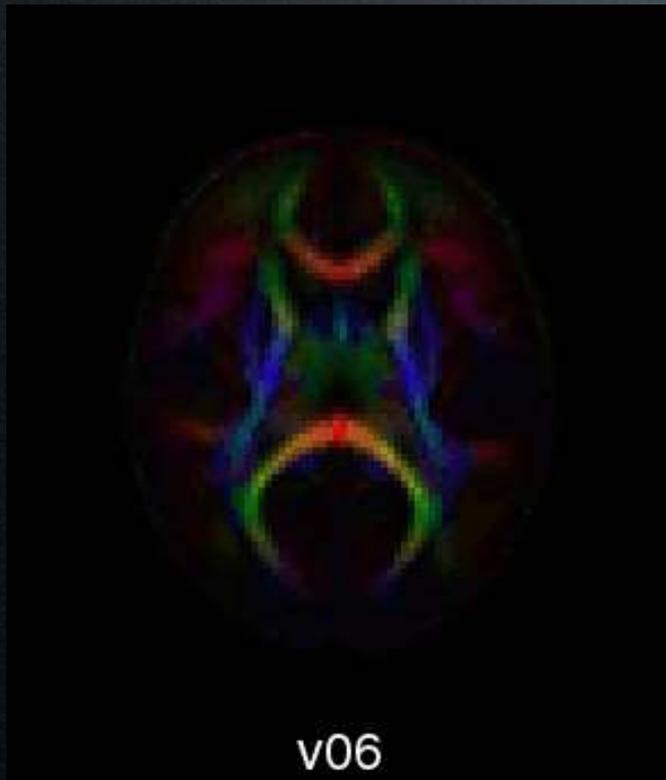
Kindlman et al.



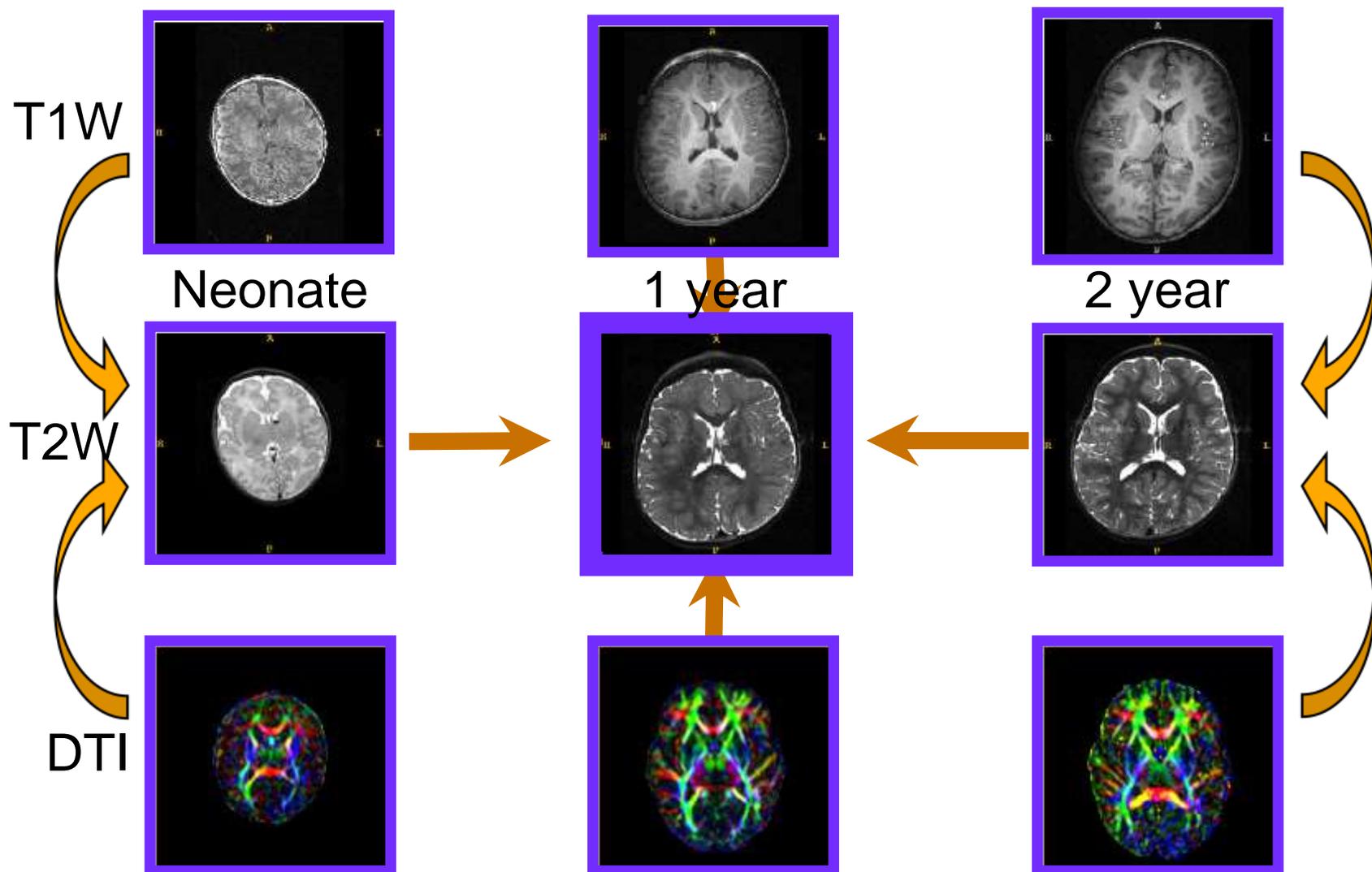
Geng et al., 2012

# Longitudinal Model

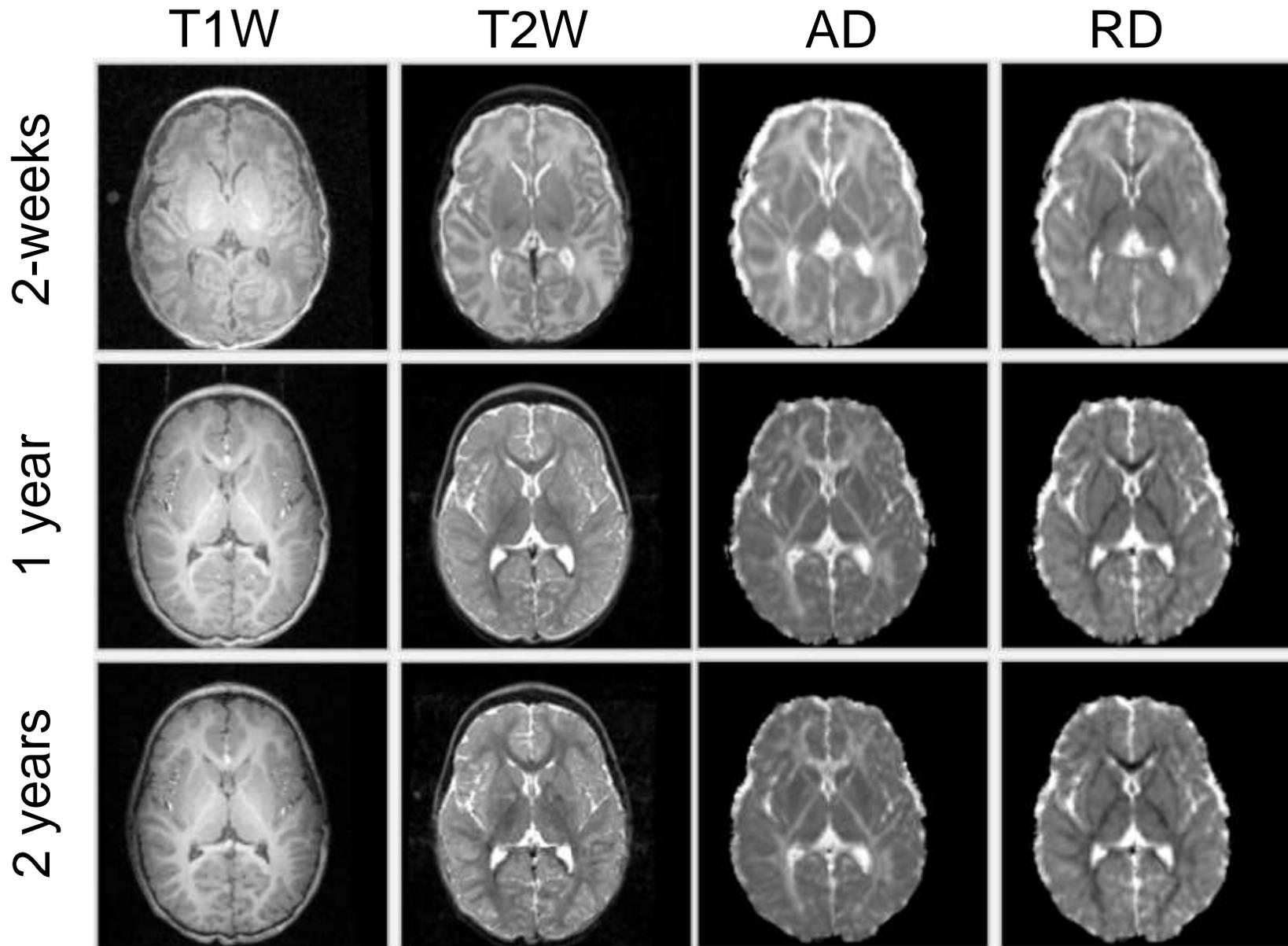
Generated with 978 Diffusion MRI (481 subjects)



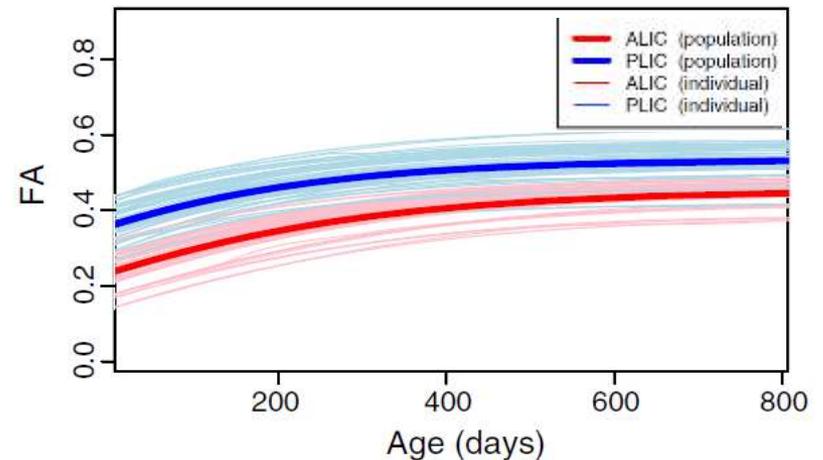
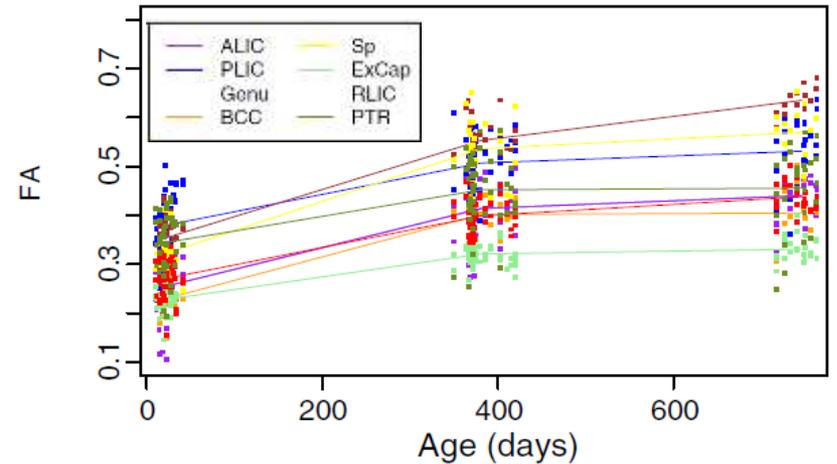
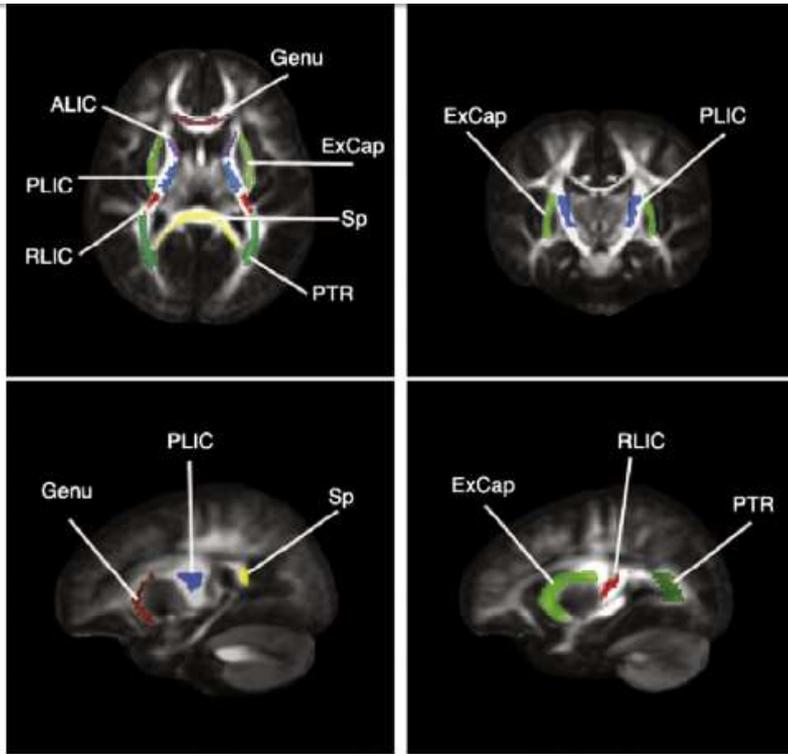
# Co-Registration (Age, Modalities)



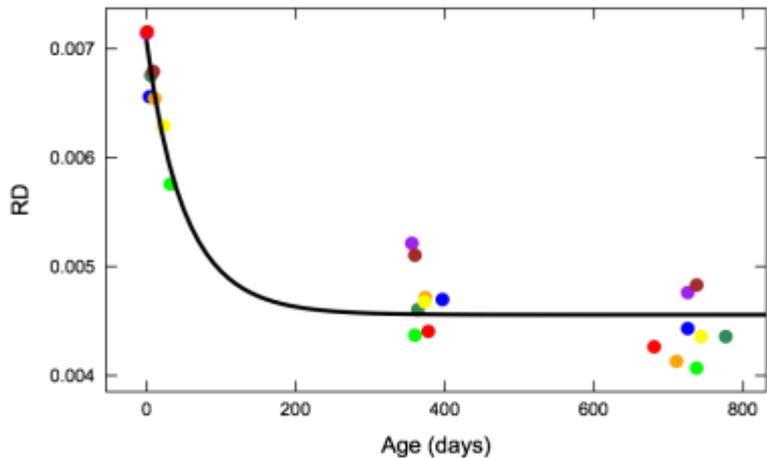
# Co-Registration (Age, Modalities)



# Longitudinal analysis of DTI: Nonlinear mixed-effect modeling



# Modeling nonlinear change via Gompertz function

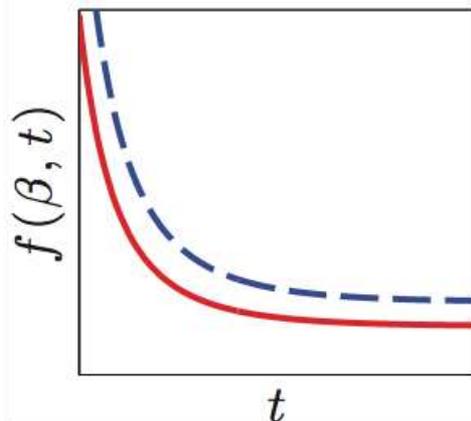


$$y = \text{asymptote} \exp(-\text{delay} \exp(-\text{speed} t))$$

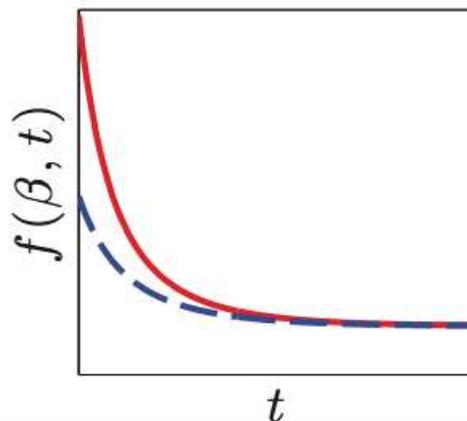
$$y = f(\beta, t) = \beta_1 \exp\{-\beta_2 \beta_3^t\}$$

$$\beta_3 = \exp(-\text{speed})$$

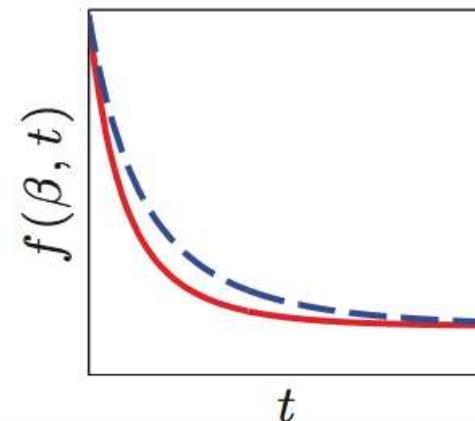
varying asymptote



varying delay

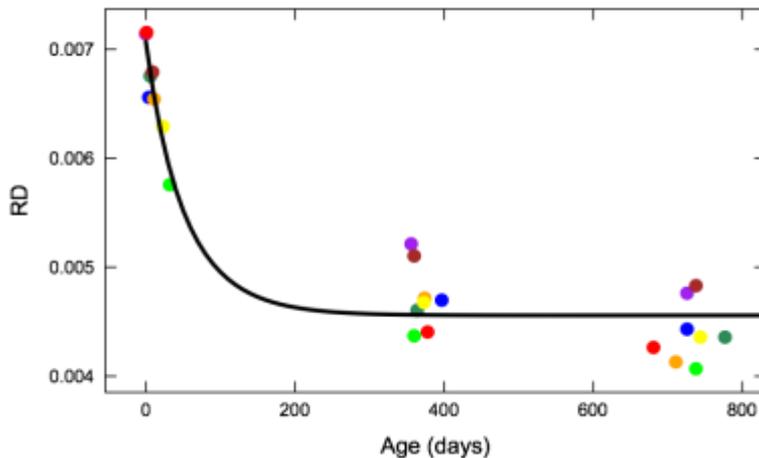


varying speed

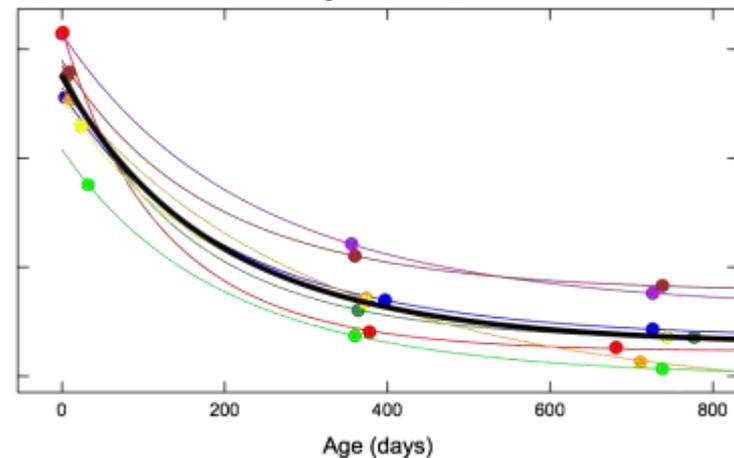


# “True” Longitudinal Analysis: Data and Model

Regression of Longitudinal Data:  
Disregard repeated measures



Longitudinal Modeling of Longitudinal Data:  
Explicit modeling of repeated measures.



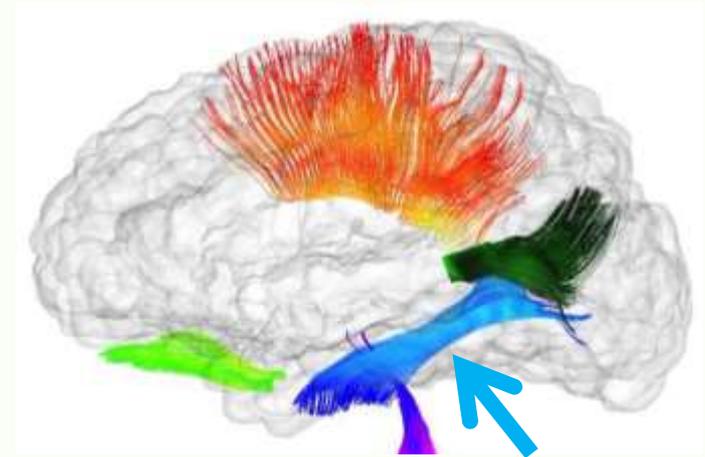
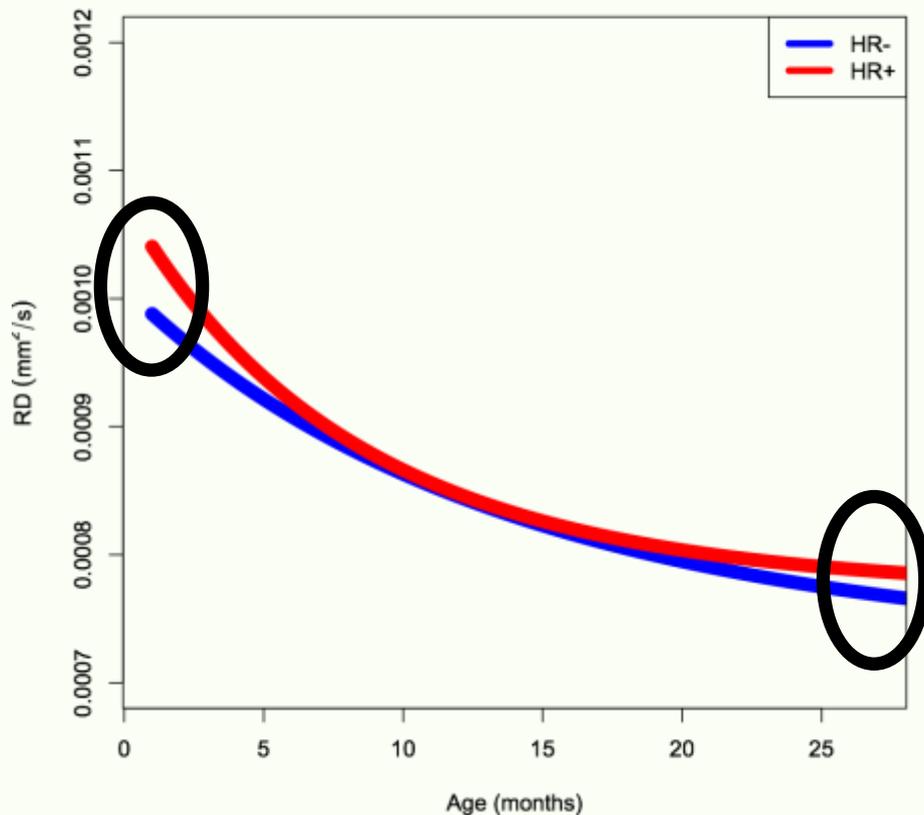
Regression is not an appropriate model of longitudinal data, the growth trajectory is not representative of individual trajectories

➔ Mixed Effect Models

# Population Trajectory Differences

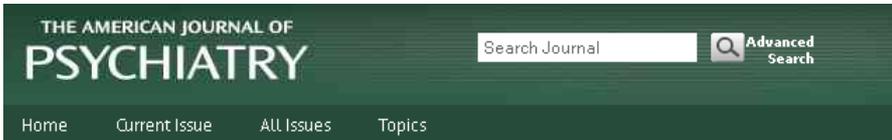
**HR+:** High risk for autism, positive diagnosis

**HR-:** High risk for autism, negative diagnosis



**Hypothesis testing on DTI:  
ILF: Speed & Asymptote ( $p < 0.05$ )**

# Longitudinal DTI in Autism



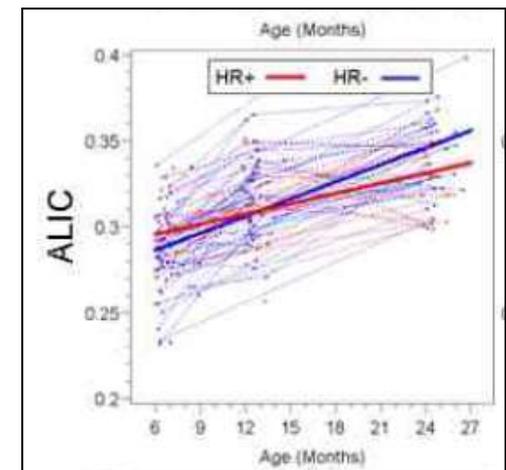
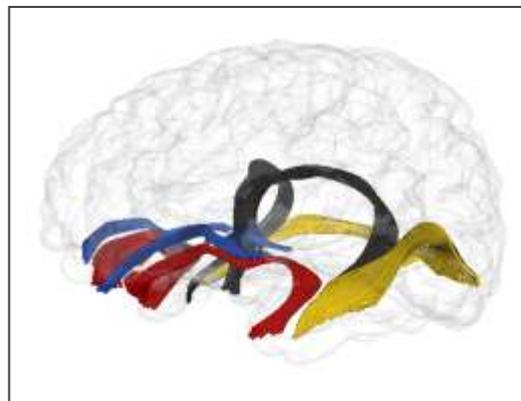
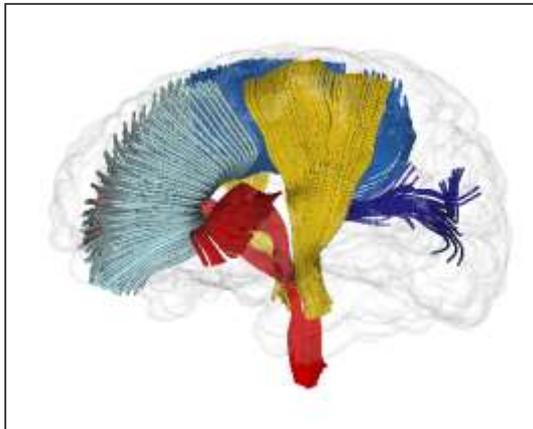
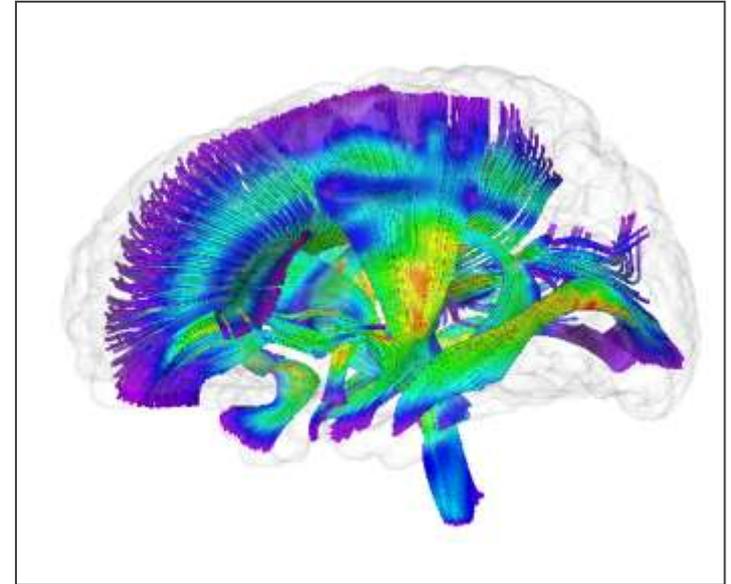
The American Journal of Psychiatry, VOL. 169, No. 6

ARTICLES | June 01, 2012

## *Differences in White Matter Fiber Tract Development Present From 6 to 24 Months in Infants With Autism*

Jason J. Wolff, Ph.D.; Hongbin Gu, Ph.D.; Guido Gerig, Ph.D.; Jed T. Elison, Ph.D.; Martin Styner, Ph.D.; Sylvain Gouttard, M.S.; Kelly N. Botteron, M.D.; Stephen R. Dager, M.D.; Geraldine Dawson, Ph.D.; Annette M. Estes, Ph.D.; Alan C. Evans, Ph.D.; Heather C. Hazlett, Ph.D.; Penelope Kostopoulos, Ph.D.; Robert C. McKinstry, M.D., Ph.D.; Sarah J. Paterson, Ph.D.; Robert T. Schultz, Ph.D.; Lonnie Zwaigenbaum, M.D.; Joseph Piven, M.D.; the IBIS Network

**RESULTS:** FA trajectories differed significantly between infants who did versus did not develop ASDs for 12 of 15 fiber tracts. Development for most fiber tracts in infants with ASDs was characterized by elevated FA at 6 months followed by slower change over-time relative to infants without ASDs. Thus, by 24 months of age, lower FA values were evident for those with ASDs.



# Study: Brain scans detect early signs of autism

[Link to CBS News](#)

comments 3 | Like 66 | Tweet 57 | +1 8 | Share 6 | More +



## Researchers See Differences in Autism Brain Development as Early as 6 Months



Scientists created 3D images of major brain pathways in infants at high risk for developing autism. [Credit: UNC]

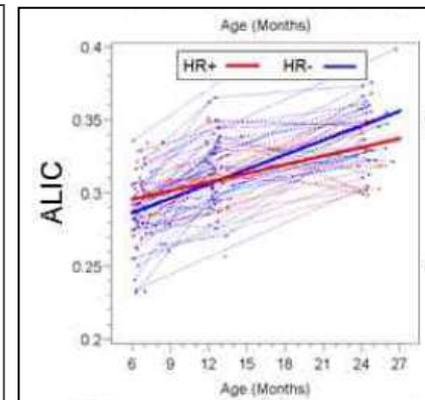
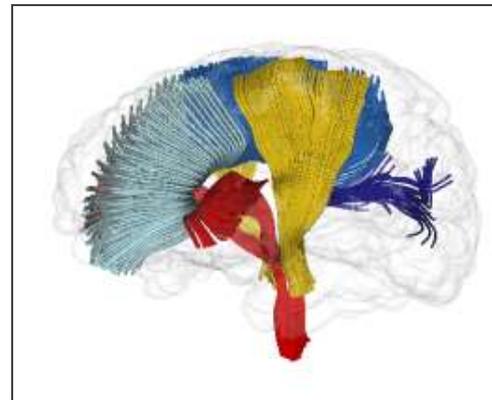
The defining features of autism—hampered communication, social challenges and repetitive actions—may not become obvious until after a baby's first birthday. But the changes in brain development that underlie these behaviors may be detectable much earlier. In a new study, researchers found clear differences in brain communication pathways starting as early as 6 months and continuing through 2 years of age in children who were later diagnosed with autism spectrum disorder (ASD). The findings appear online today in the *American Journal of Psychiatry*.

The American Journal of Psychiatry, VOL. 169, No. 6

ARTICLES | June 01, 2012

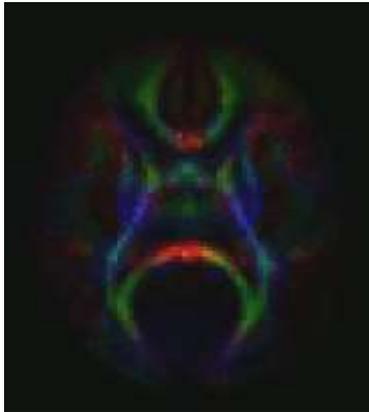
### Differences in White Matter Fiber Tract Development Present From 6 to 24 Months in Infants With Autism

Jason J. Wolff, Ph.D.; Hongbin Gu, Ph.D.; Guido Gerig, Ph.D.; Jed T. Elison, Ph.D.; Martin Styner, Ph.D.; Sylvain Gouttard, M.S.; Kelly N. Botteron, M.D.; Stephen R. Dager, M.D.; Geraldine Dawson, Ph.D.; Annette M. Estes, Ph.D.; Alan C. Evans, Ph.D.; Heather C. Hazlett, Ph.D.; Penelope Kostopoulos, Ph.D.; Robert C. McKinstry, M.D., Ph.D.; Sarah J. Paterson, Ph.D.; Robert T. Schultz, Ph.D.; Lonnie Zwaigenbaum, M.D.; Joseph Piven, M.D.; the IBIS Network

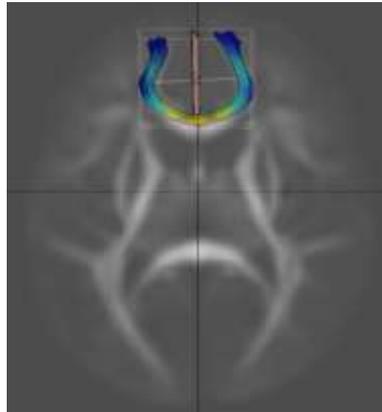


# Longitudinal Tract-Based Modeling

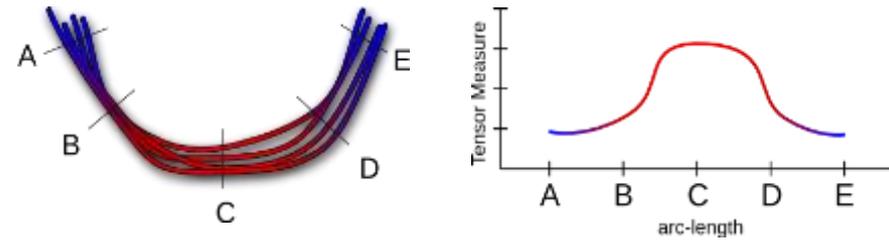
Cine



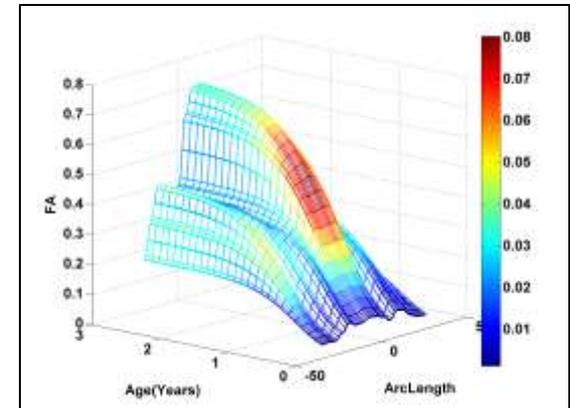
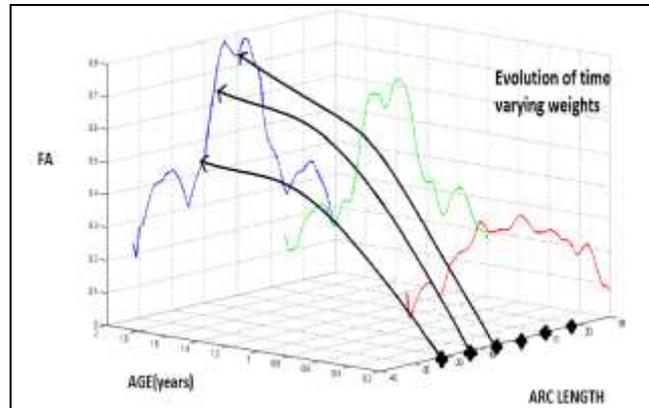
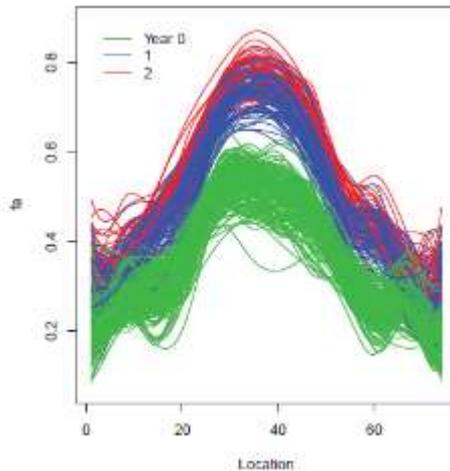
Genu Tract



Parametrization by arc-length

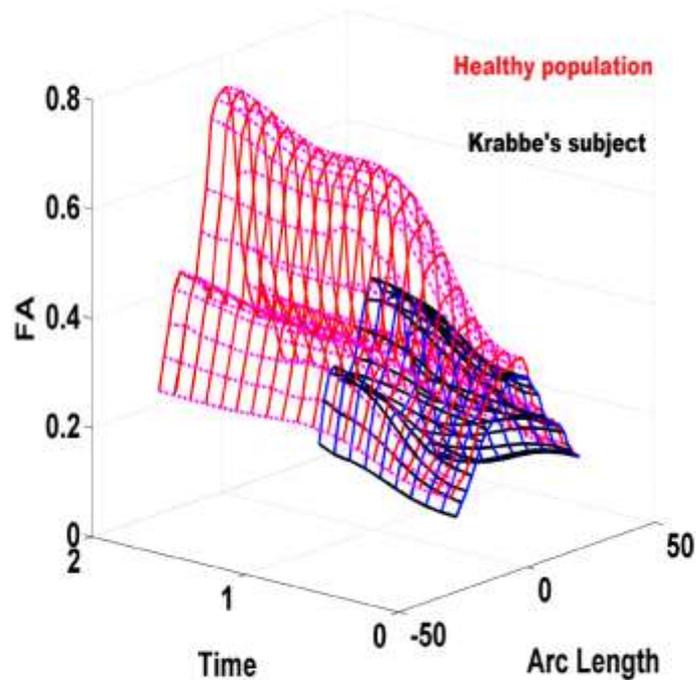


Spatio-temporal statistical tract model

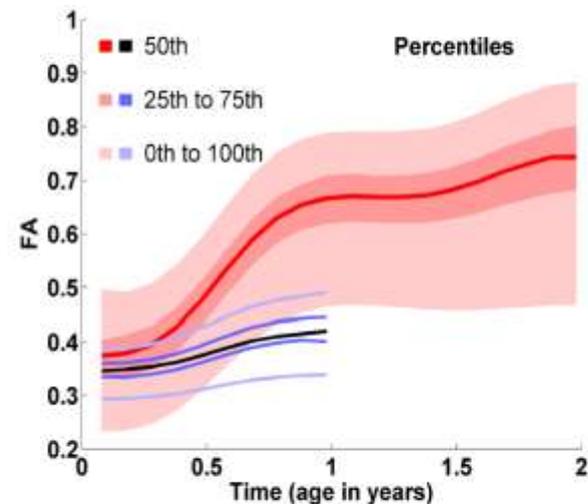


# Subject-specific Analysis: Krabbe's Disease

- ▶ Krabbe's disease affects myelin of the nervous system.
- ▶ Degenerative in nature, often fatal without early therapy.

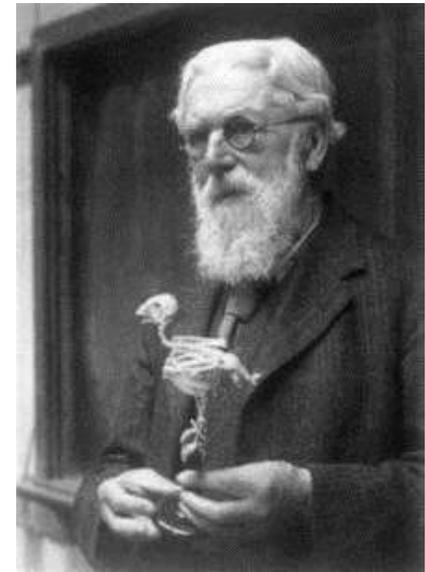
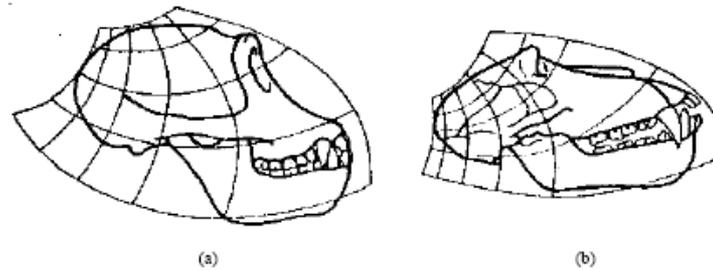
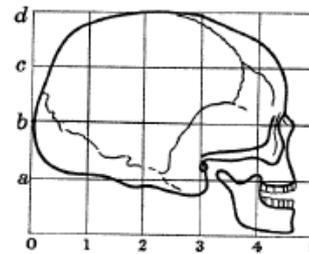
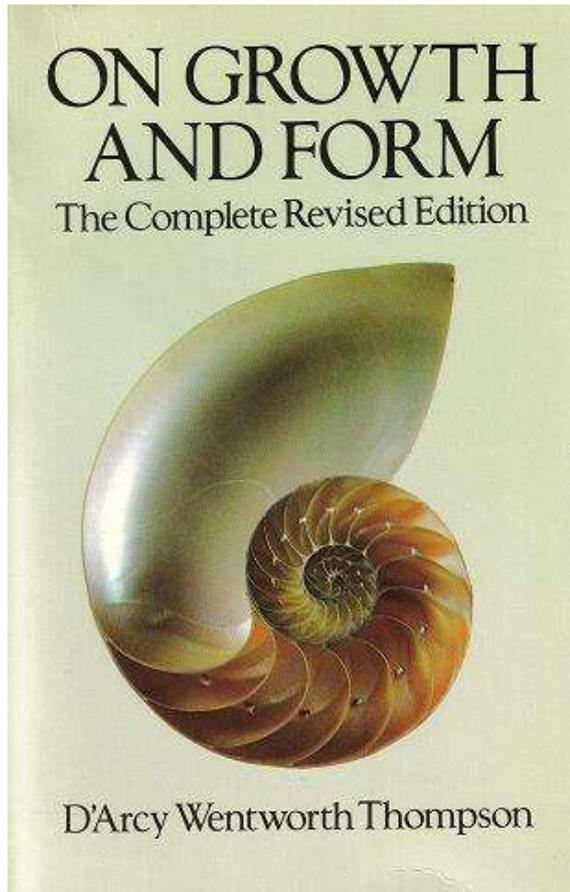


Normative FA trajectory wrt a single Krabbe's subject.

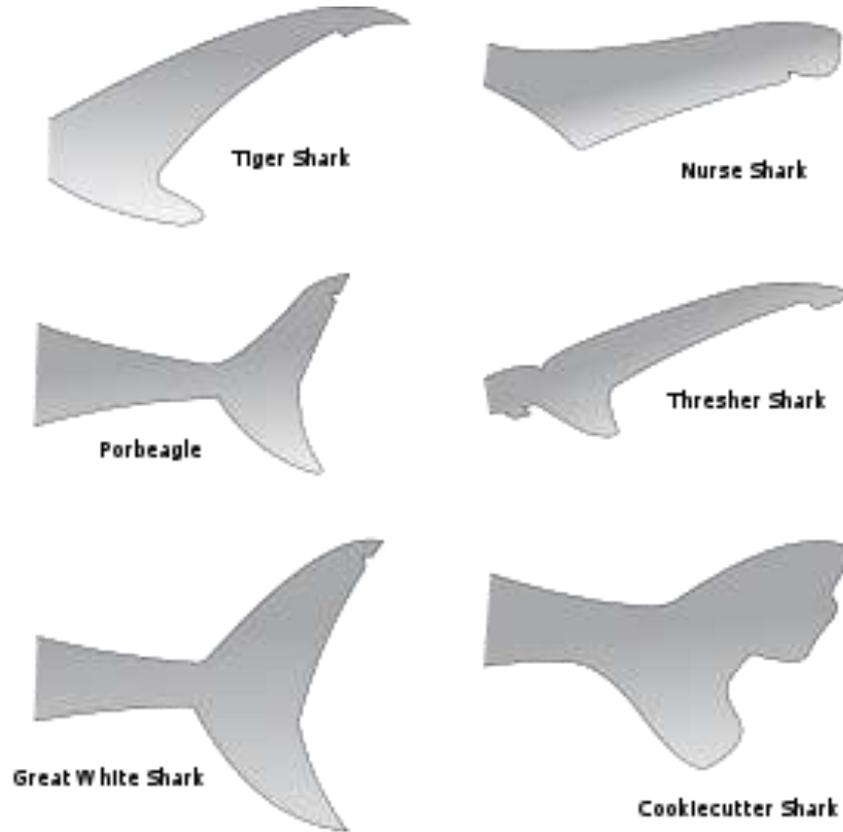


FA quartiles for a single tract location along time.

# Spatiotemporal Shape Analysis



# Why Shape?



---

## Shark Tails

The Diversity of Form and Function

# Shape Variability



## Box of Phrenological Heads

*Made and sold by William Bally, Dublin, 1831.*

The 60 model heads in this box illustrate a wide range of human characteristics which phrenologists believed could be discovered by measuring the shape of the skull.

One of the initiators of the study of phrenology, Johann Caspar Spurzheim (1776-1832), wrote a pamphlet which accompanied the set, describing the qualities to be expected from each head

shape. Number 54, for example, is the bust of a scientist.

science museum

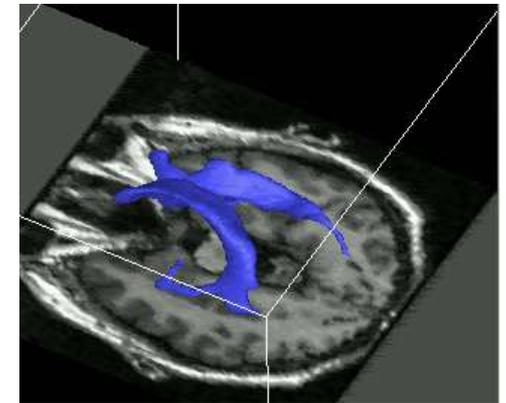
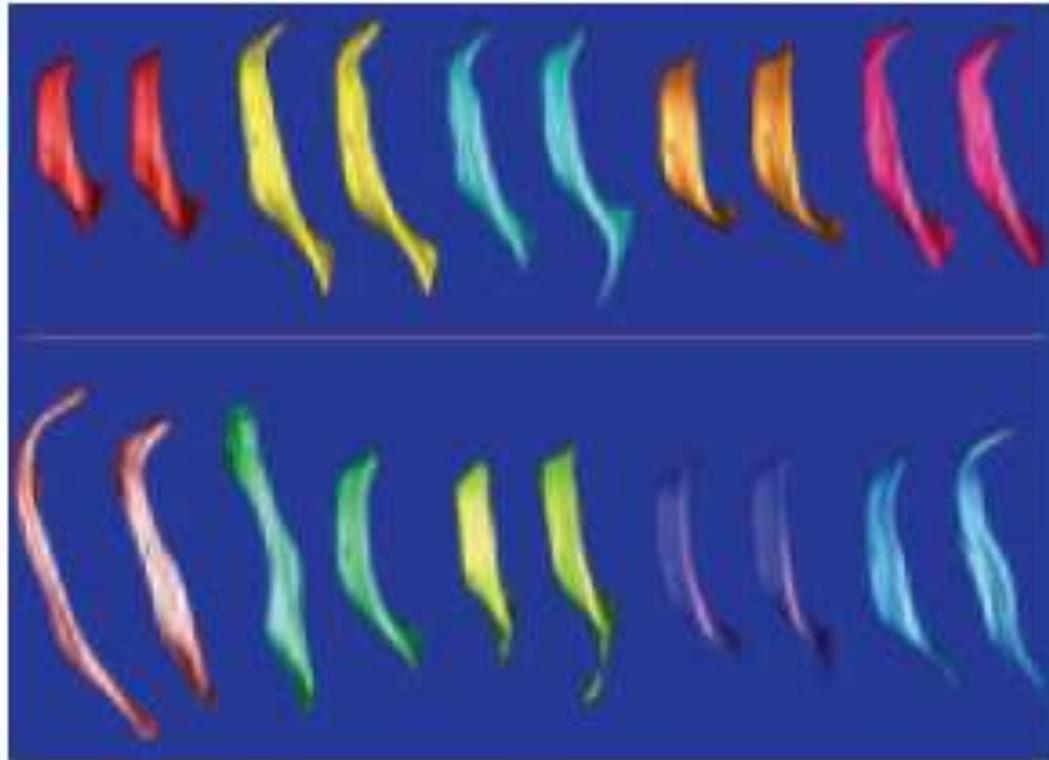
## Brought to Life

Exploring the History of Medicine



[link](#)

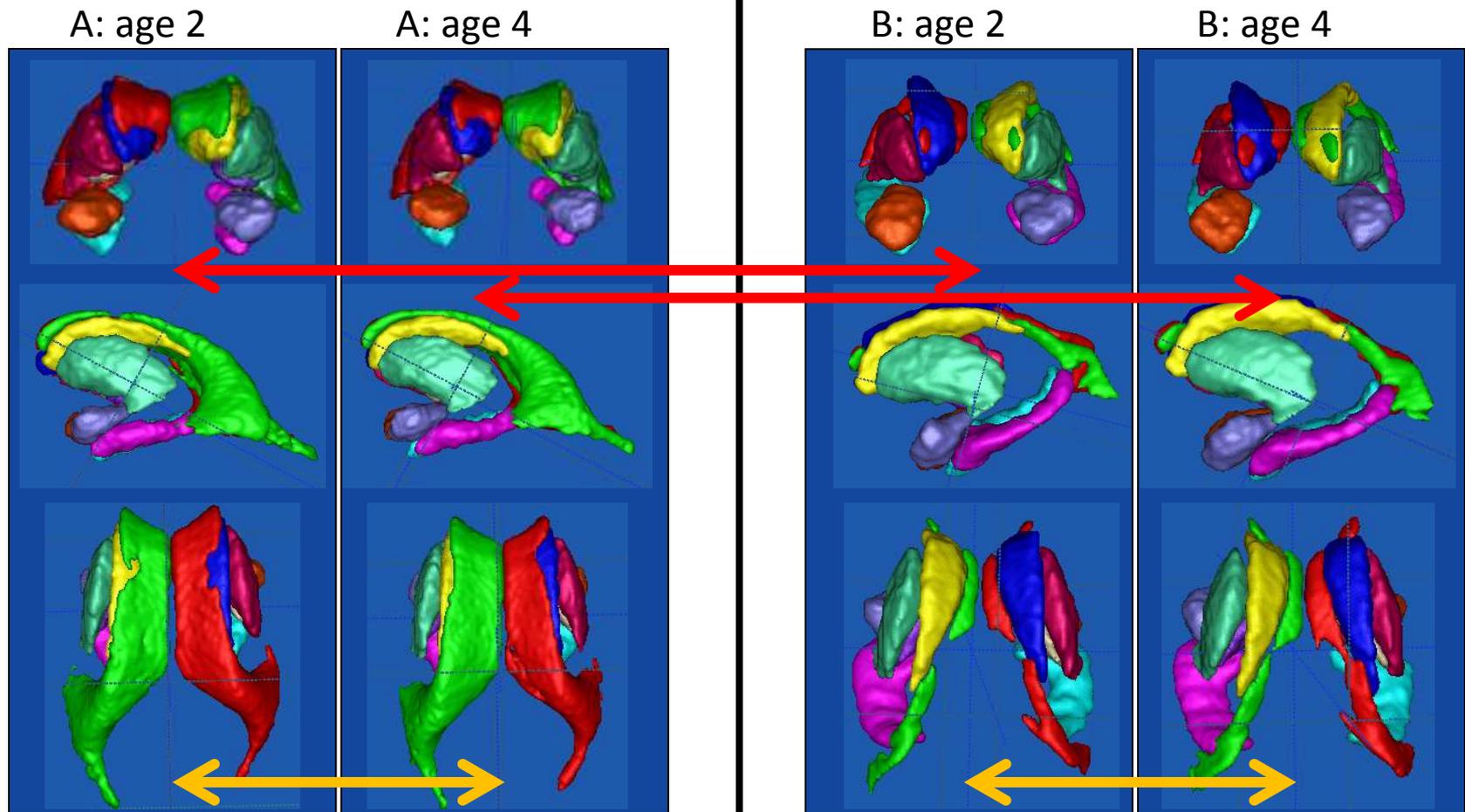
# Shape Similarity in Twins



Upper row: identical twin pairs

Lower row: non-identical twin pairs

# Example Infant Study: Cross-sectional vs. Longitudinal



**Cross-sectional: Huge changes between sets of shapes**

**Longitudinal: Subtle changes of sets of shapes with time**

# Shape >> Volume

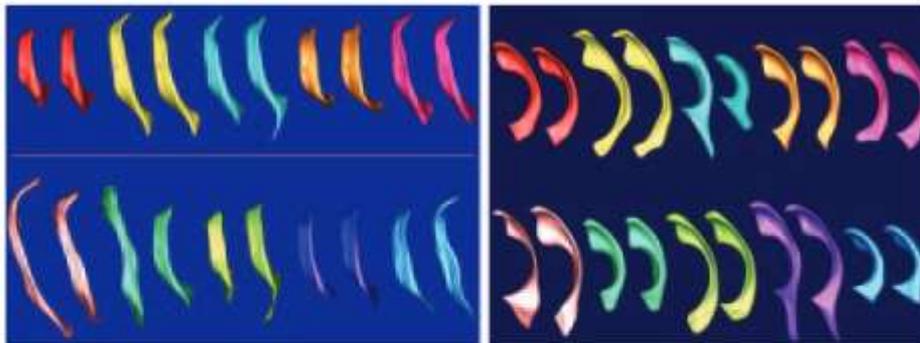
PNAS

## Morphometric analysis of lateral ventricles in schizophrenia and healthy controls regarding genetic and disease-specific factors

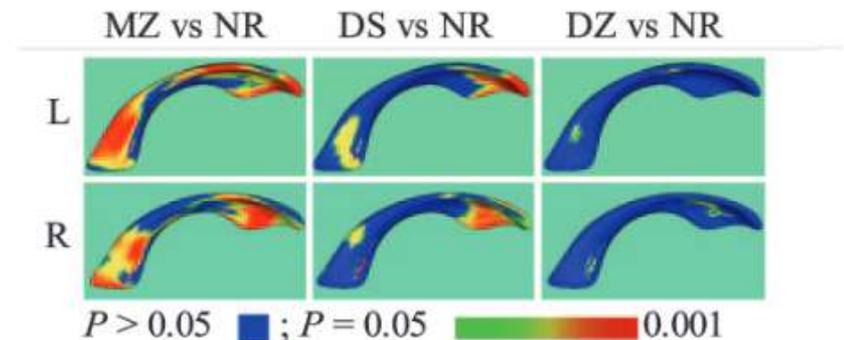
Martin Styner<sup>\*†‡§</sup>, Jeffrey A. Lieberman<sup>†¶</sup>, Robert K. McClure<sup>†¶</sup>, Daniel R. Weinberger<sup>\*\*</sup>, Douglas W. Jones<sup>\*\*</sup>, and Guido Gerig<sup>\*†</sup>

<sup>\*</sup>Department of Computer Science, University of North Carolina, Chapel Hill, NC 27599-3175; <sup>†</sup>Department of Psychiatry, University of North Carolina School of Medicine, Chapel Hill, NC 27599-3175; <sup>\*\*</sup>Clinical Brain Disorder Branch, National Institute of Mental Health, National Institutes of Health, Bethesda, MD 20892; and <sup>§</sup>M. E. Müller Research Center for Orthopaedic Surgery, Institute for Surgical Technology and Biomechanics, University of Bern, CH-3014 Bern, Switzerland

Communicated by Frederick P. Brooks, Jr., University of North Carolina, Chapel Hill, NC, February 9, 2005 (received for review October 21, 2004)

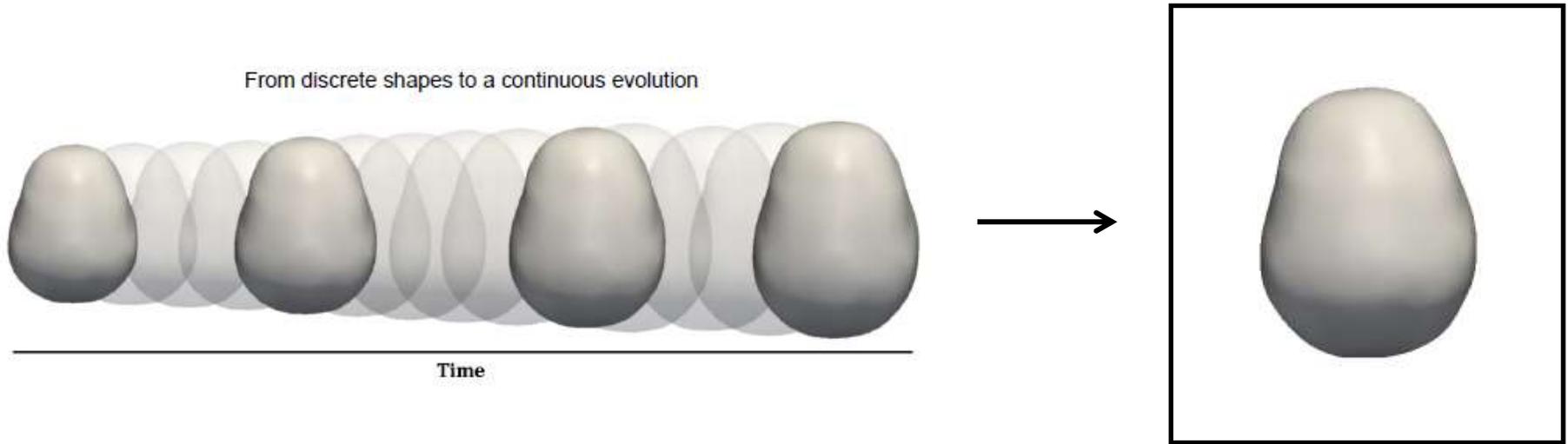


**Fig. 1.** Graphical view of aligned and size-normalized ventricles. (Left) Superior view of left ventricles of five MZ twin pairs (Upper) and five DZ twin pairs (Lower) displayed from the top. Ventricles of co-twins are shown by using the same color. (Right) Sagittal view of right ventricles of 10 DS pairs, with affected and unaffected shown side by side. The third pair (Upper Right) was excluded because of hydrocephaly in the unaffected twin.



**Fig. 6.** Statistical maps displaying the locations of significant differences between groups for the co-twin analysis. The colors indicate the level of significance as shown in the color map. Results for group comparisons not shown in this figure did not have significant regions

# 4D Shape Modeling from Time-Discrete Data



- **Concept:** Given a set of discrete shapes, interpolate a continuous 4D growth model via shape regression.
- **Assumption:** Growth/degeneration of biological tissue is inherently smooth in space and time & nonlinear, locally varying process.
- **Method:** Continuous flow of diffeomorphisms via correspondence-free “currents”. *Cost function = Data Matching + Regularity.*

# Acceleration Controlled Shape Regression

We define the acceleration field  $a(x(t))$  as a vector field of the form

$$a(x(t)) = \sum_{i=1}^N K^V(x(t), x_i(t)) \alpha_i(t)$$

$x_i$ : the shape points carrying a point force vector  $\alpha_i$

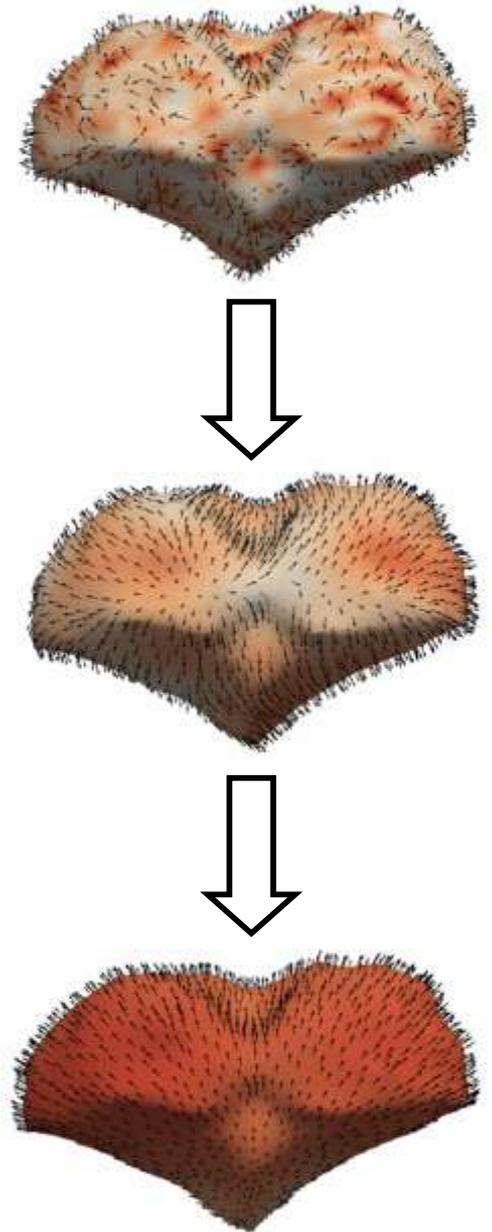
$K^V(x, y) = \exp(-\|x - y\|^2 / \lambda_V^2)$ : a Gaussian kernel with standard deviation  $\lambda_V$

Time varying deformation  $\phi_t(x_i)$  given by:

$$\ddot{\phi}_t(x_i) = a(x_i(t))$$

$x_i(0)$ : initial position

$\dot{x}_i(0)$ : initial velocity



# Regression Criterion

Let  $\mathbf{x}(t)$ ,  $\mathbf{a}(t)$ , and  $\boldsymbol{\alpha}(t)$  be the concatenation of the  $x_i(t)$ 's,  $a_i(t)$ 's, and the  $\alpha_i(t)$ 's.

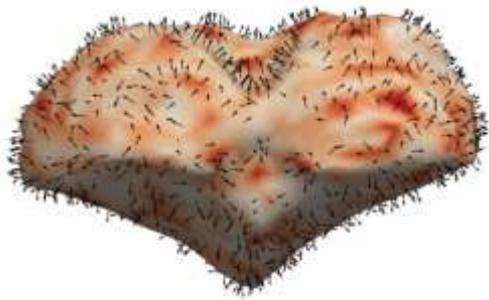
$$E(\dot{\mathbf{x}}(0), \boldsymbol{\alpha}(t)) = \sum_{t_i} \|\phi_{t_i}(\mathbf{x}(0)) - \mathbf{x}(t_i)\|_{W^*}^2 + \gamma \int_0^T \|\mathbf{a}(t)\|_V^2 dt$$

$\|\cdot\|_{W^*}$  is the norm on currents

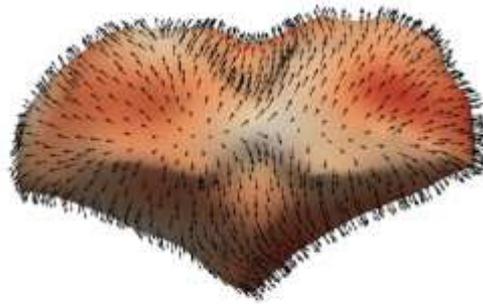
$$\|\mathbf{a}(t)\|_V^2 = \boldsymbol{\alpha}(t) K^V(\mathbf{x}(t), \mathbf{x}(t)) \boldsymbol{\alpha}(t)$$

# Acceleration Controlled Shape Regression

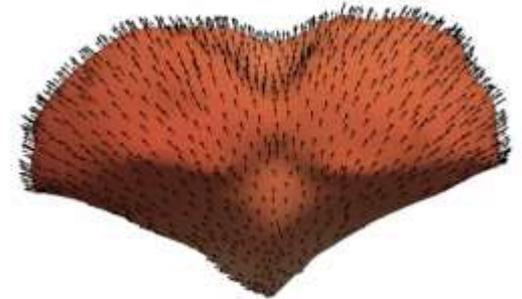
Evolution of cerebellum from 6 to 24 months



Point forces  $\alpha$



Acceleration

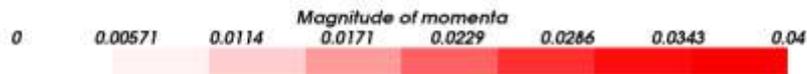
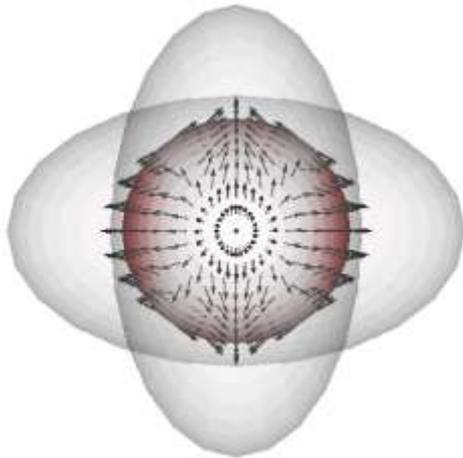


Velocity

# Piecewise Geodesic vs Acceleration Controlled

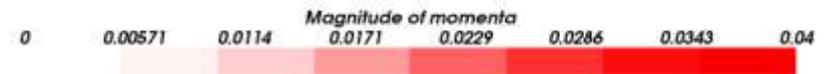
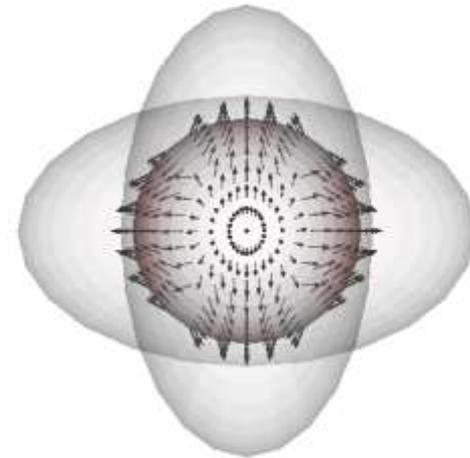
Synthetic experiment comparing piecewise geodesic and acceleration controlled shape regression

Time: 0.00 years



Piecewise geodesic

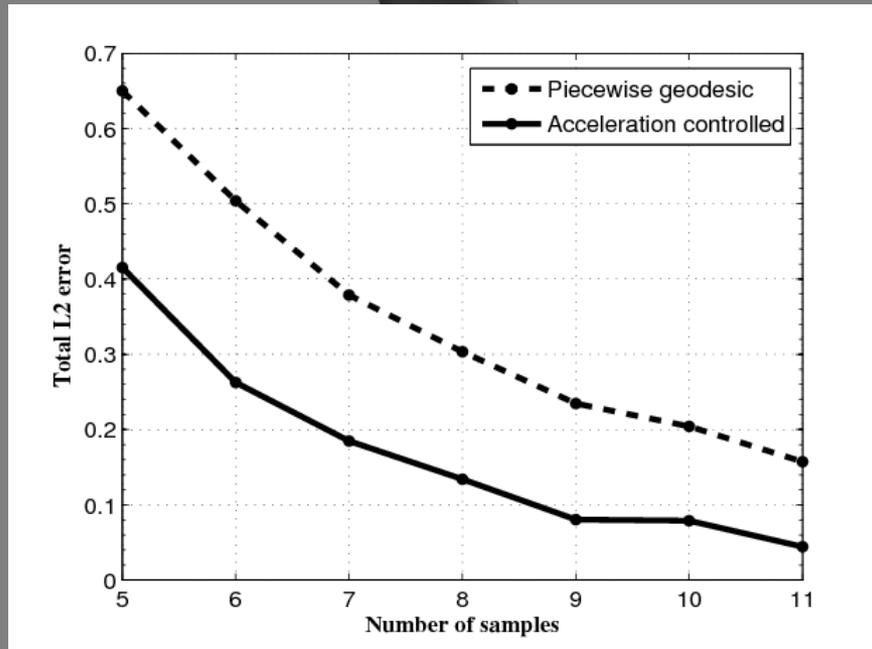
Time: 0.00 years



Acceleration controlled

# Interpolation Properties

## Synthetic evolution



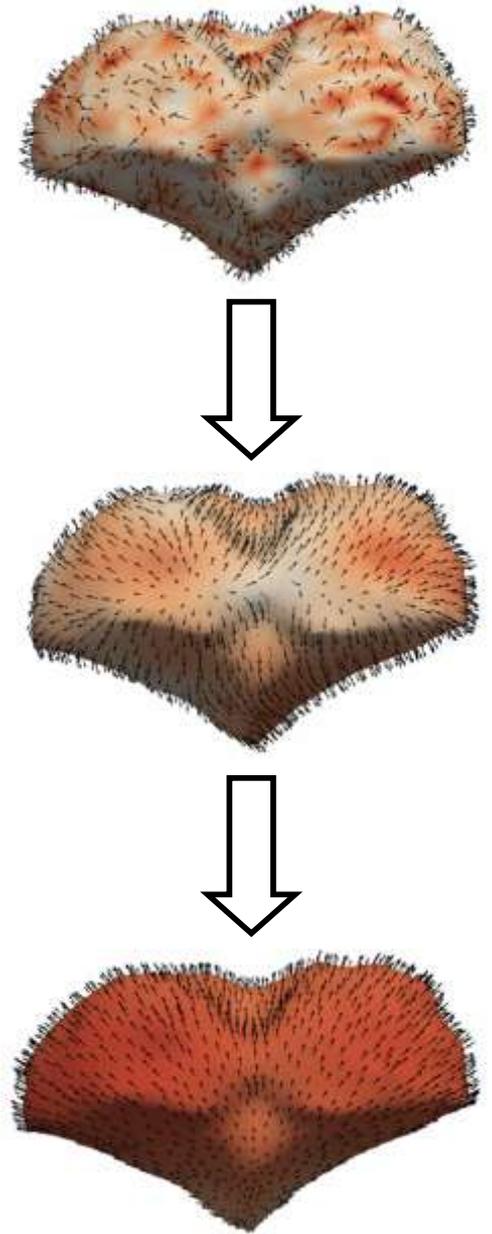
# Summary

## Benefits:

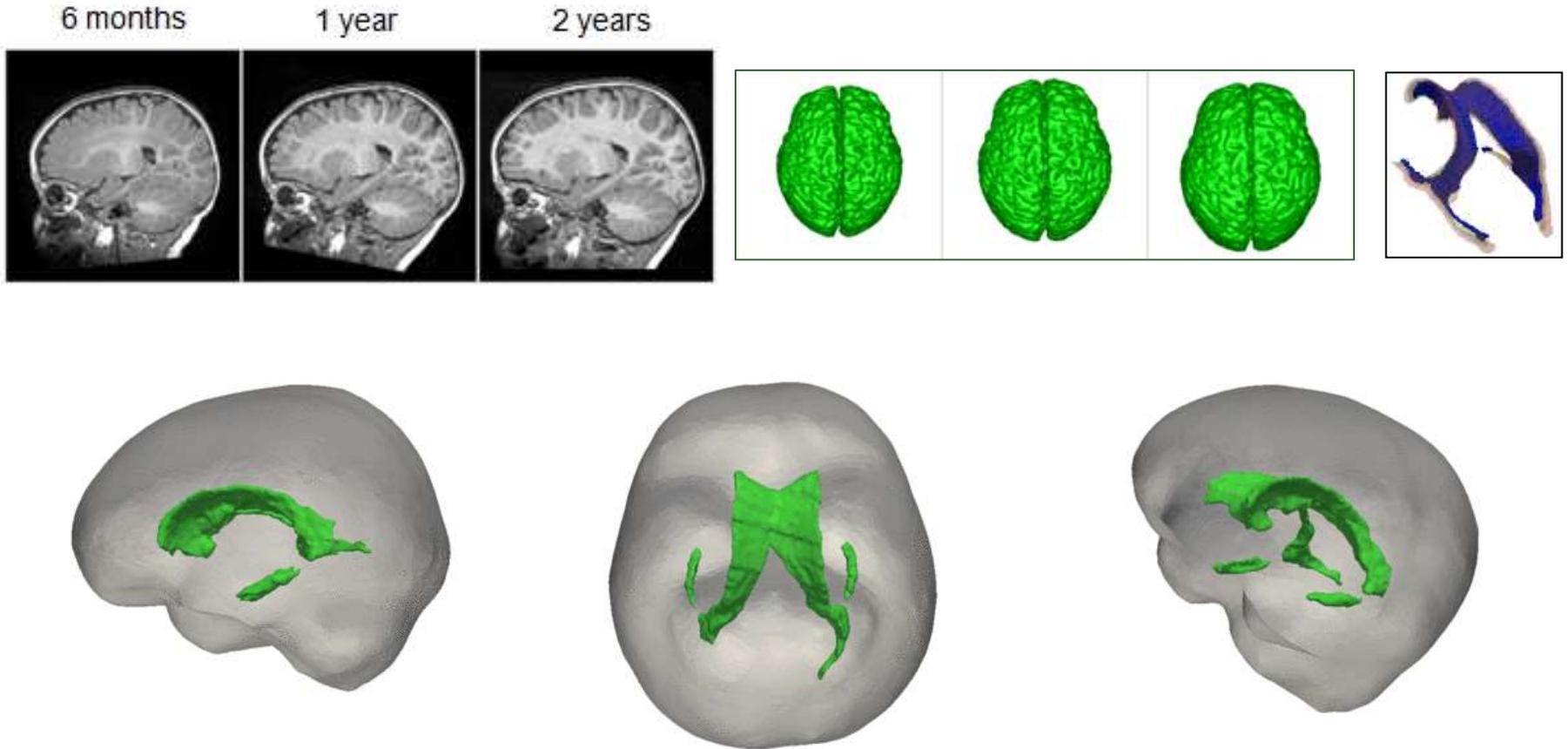
- More biologically realistic trajectories
- Nice interpolation properties

## Drawbacks:

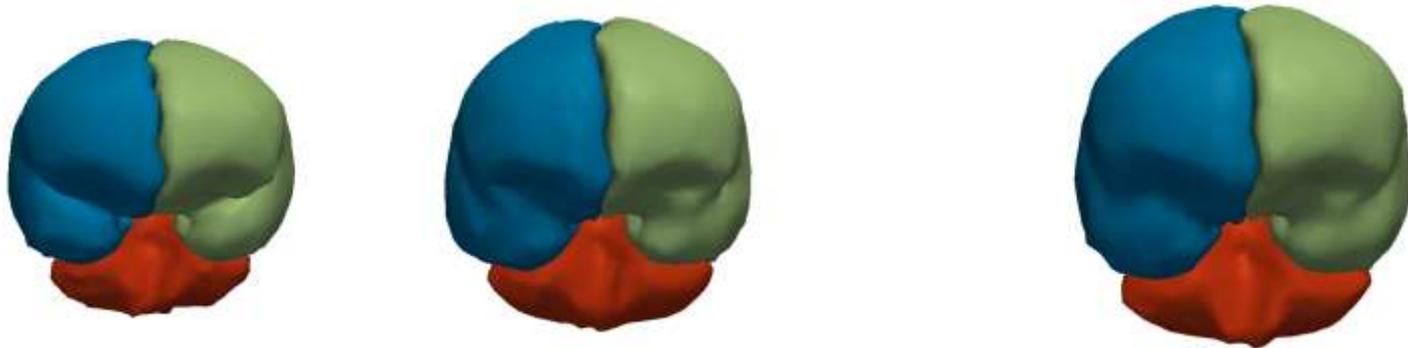
- Not compact or generative



# Longitudinal Shape Regression



# 4D Shape Regression



6

12

24

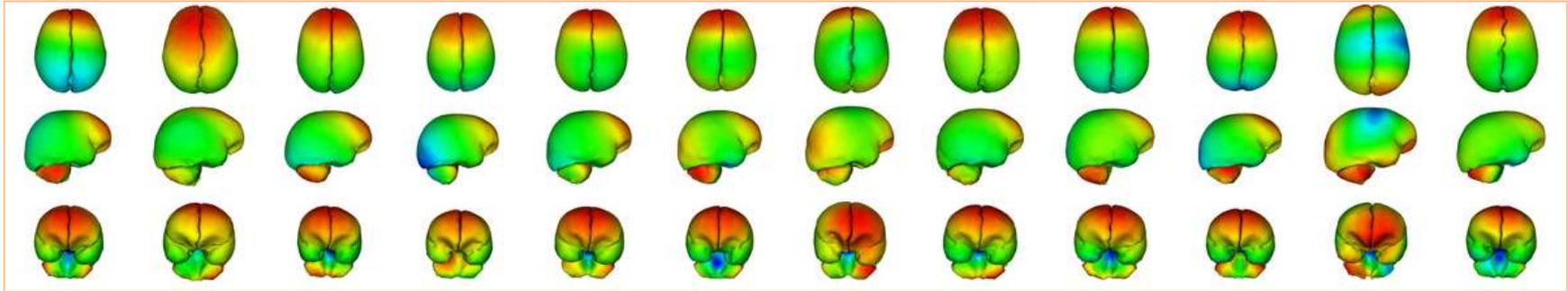
Time (months)

From discrete 3D shapes (6m,12m,24m) to continuous 4D shape model

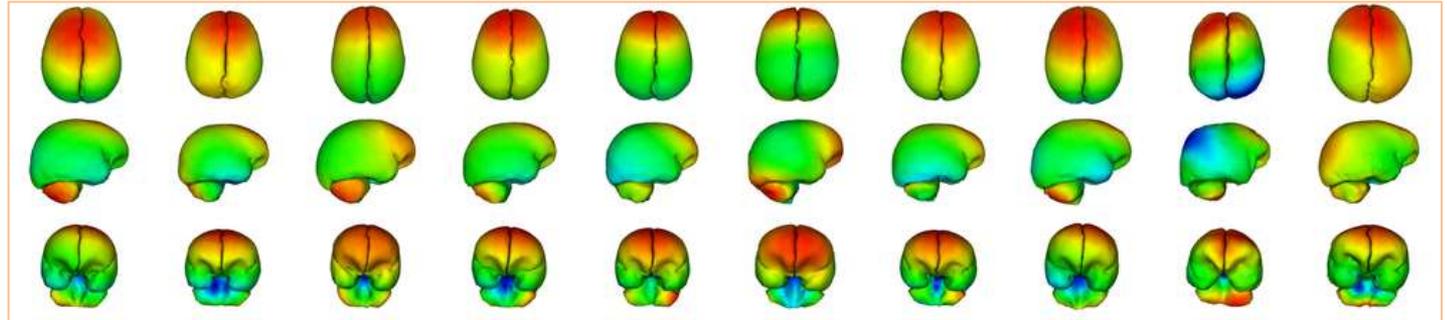


# Individual 4D Growth Profiles

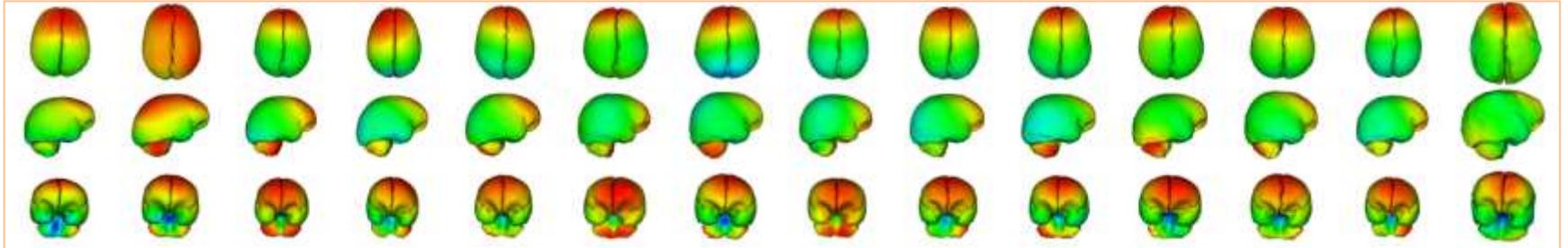
HR+



HR-

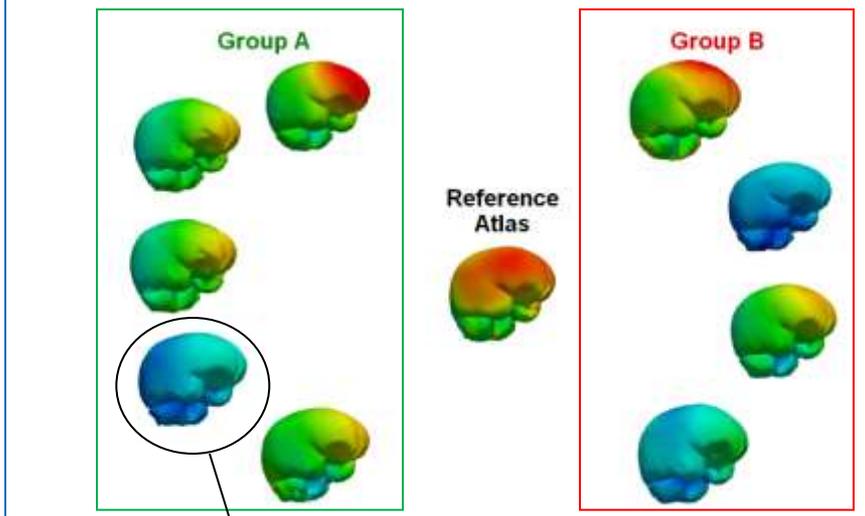


LR-

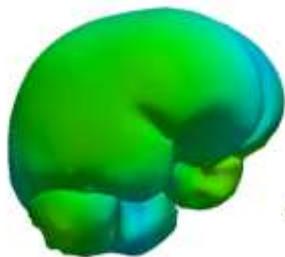
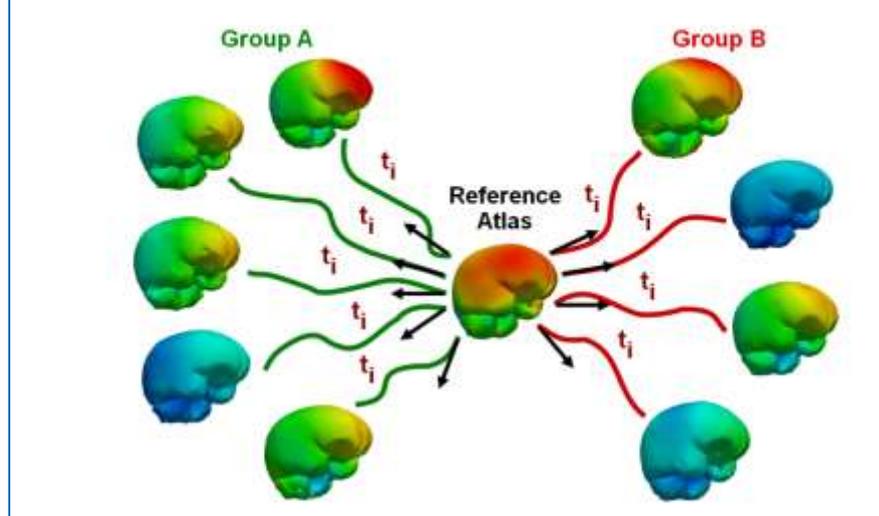


# Statistics of 4-D Shape Trajectories

Personalized **4D models** for subjects in different groups



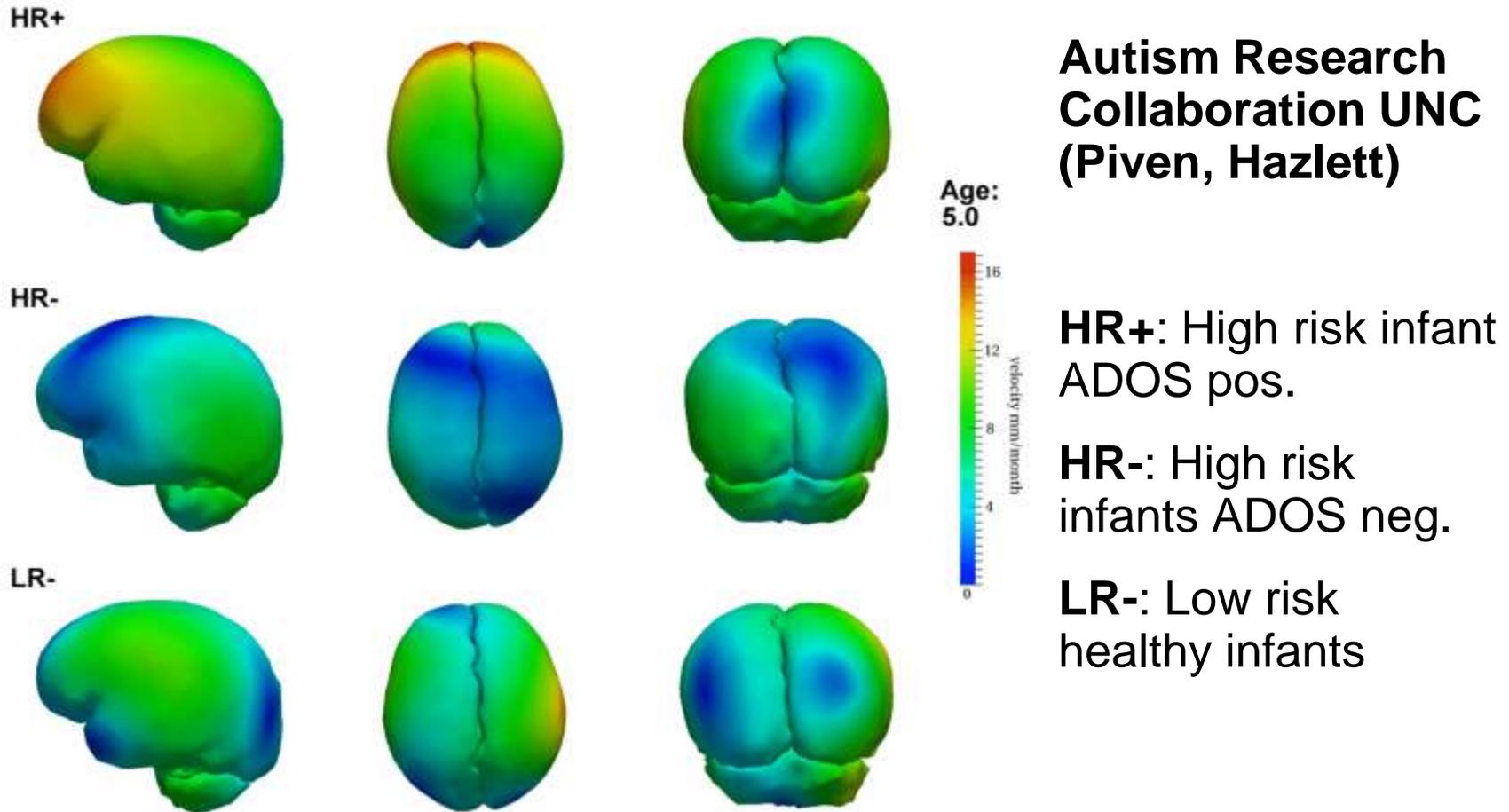
Flow of diffeomorphisms are **geodesic** → initial momenta parameterize deformation → Statistics on Diffeomorphisms



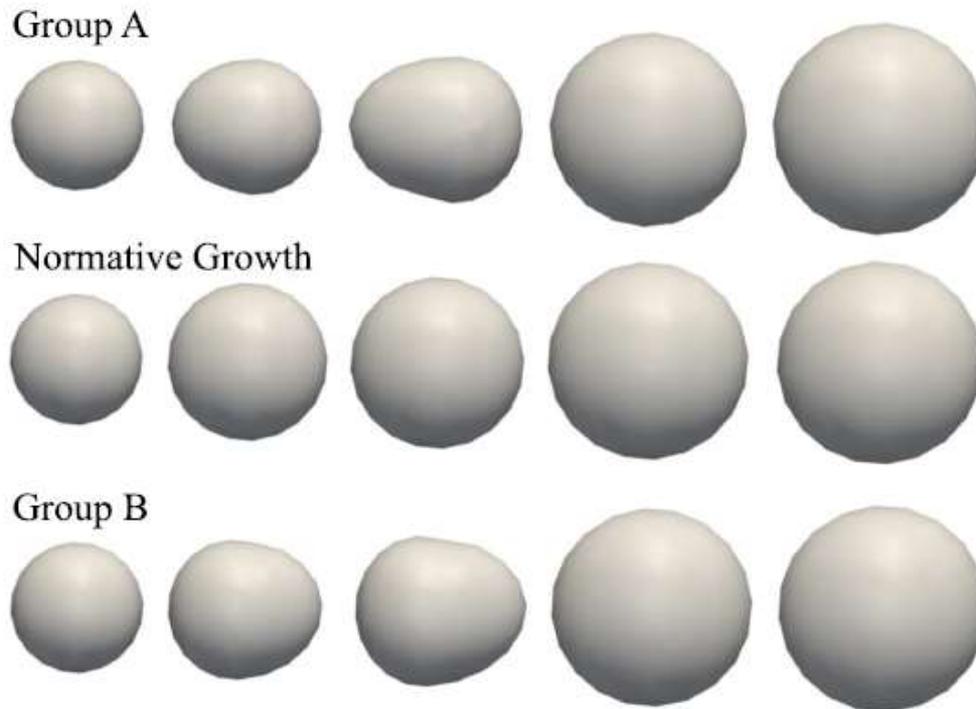
Individual 4D model



# Work in progress: Statistics of 4D growth profiles

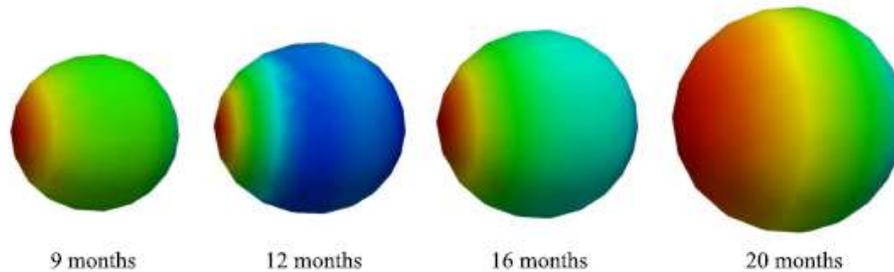


# Quantification of spatio-temporal population differences



**Fig. 2.** The synthetic shape database with observations at 6, 10, 12, 18, and 24 months. **Top:** Typical shape observations for a subject from group A. **Middle:** The normative growth scenario. **Bottom:** Typical shape observations for a subject from group B.

# New: Quantification of spatio-temporal population differences

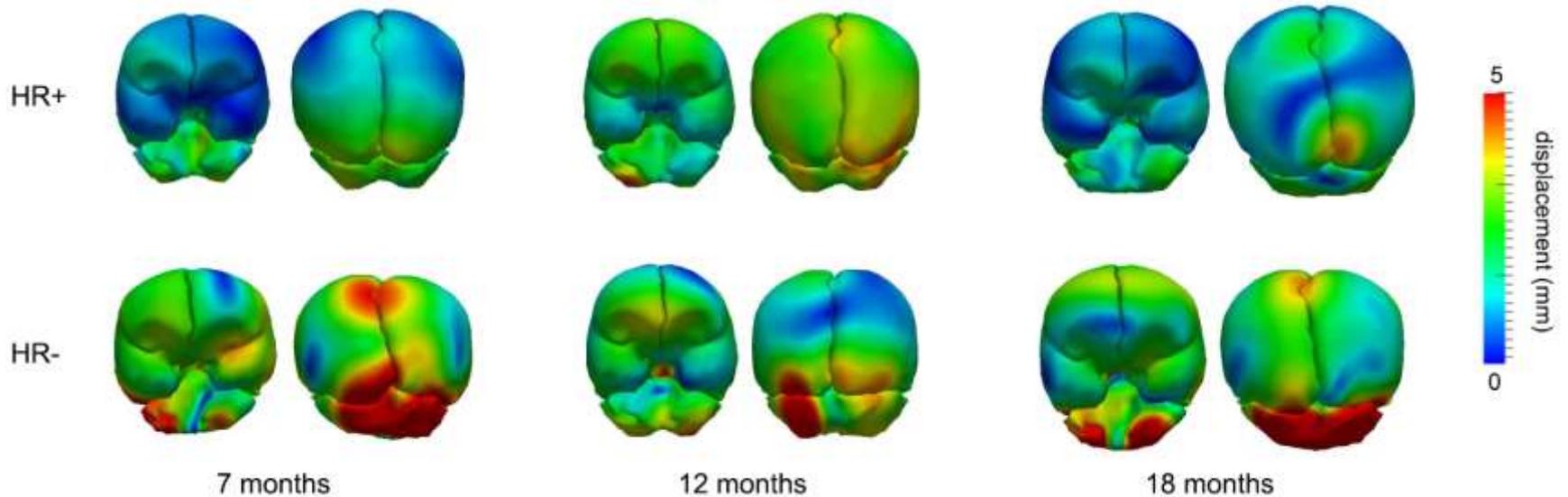


**Fig. 3.** The first major mode of deformation from PCA (mean plus one standard deviation) at selected time points for group A. Color indicates the displacement from the mean shape. The variability in the protuberance is clearly captured.



**Fig. 4.** Significant differences in magnitude of momenta between group A and B at several time points, with p-values displayed on the surface of the reference atlas.

## First mode of deformation from **PCA** per age group



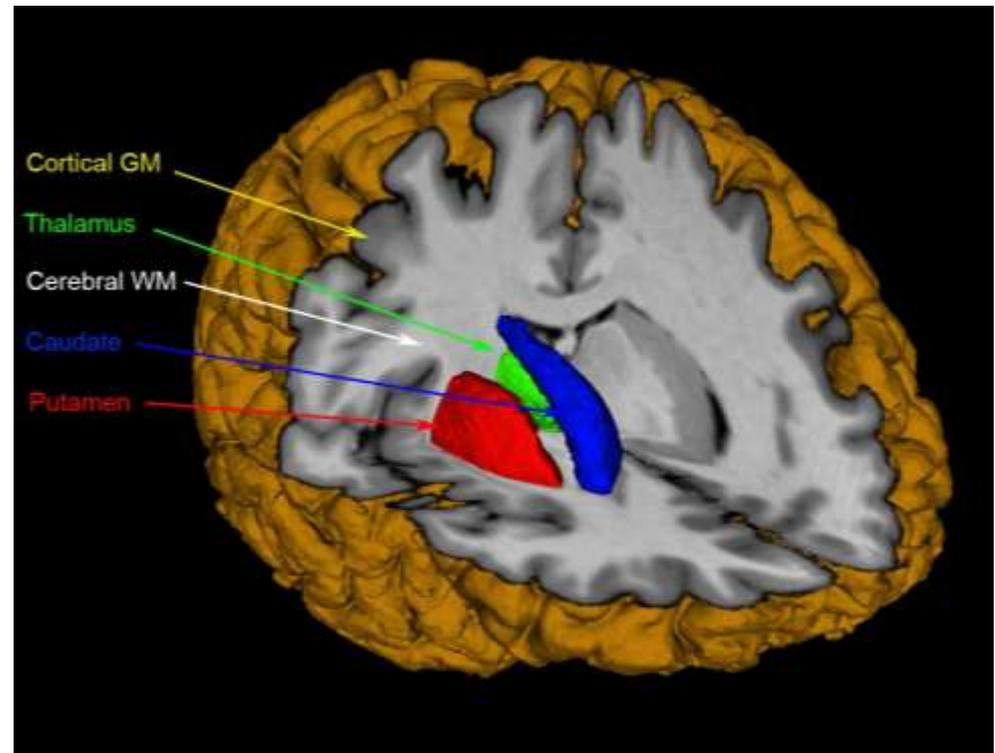
Hypothesis testing → **no significant** differences in magnitude of initial momenta

# PREDICT-HD



Search for noninvasive biomarker with imaging...

- Symptomatic HD imaging findings
  - Atrophied caudate and putamen
  - Disproportionate loss of white matter
- Prodromal HD imaging findings
  - Striatal atrophy correlates with:
    - Neurological impairment
    - Poorer performance on cognitive assessments
    - Years to motor symptom onset

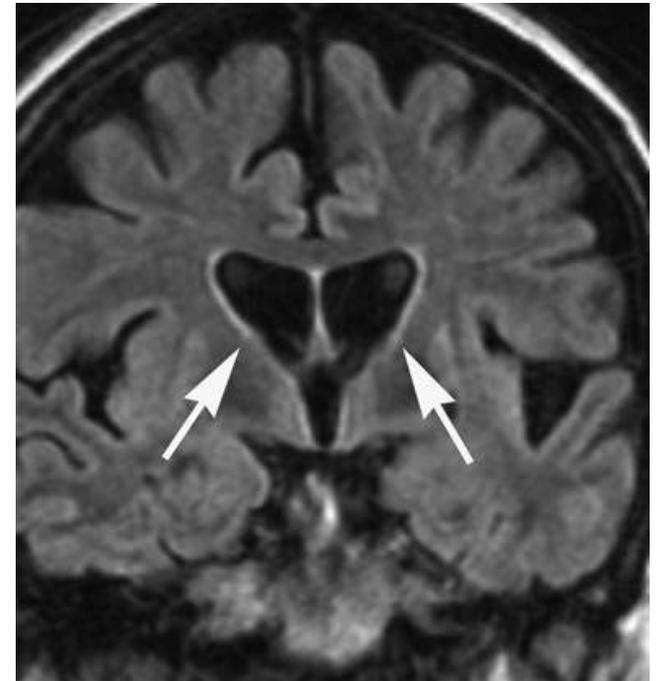


Courtesy Jane Paulsen, Hans Johnson, U-Iowa

# Purpose: Huntington's Disease

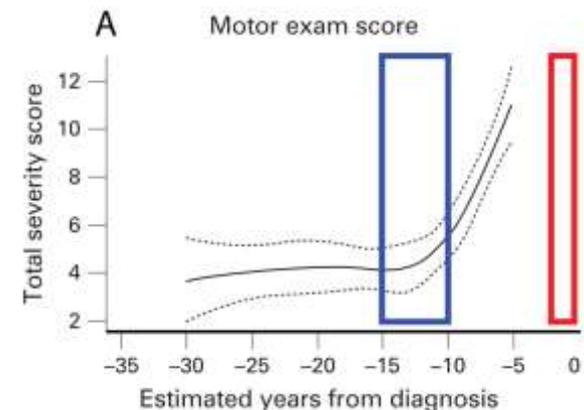
## What is Huntington's disease (HD)?

- Etiology
  - Progressive autosomal-dominant, polyglutamine disease
  - Mutation: Expanded trinucleotide CAG-repeat in huntingtin gene [77]
- Signs and symptoms: Motor, cognitive, and psychiatric disturbances
- Diagnosis
  - Usually made in mid-life (35-42)
  - Onset of motor symptoms with positive family history [76]
  - Confirmed with genetic testing (expanded CAG-repeat)
  - Radiographic feature: Prominently decreased striatum (caudate and putamen) at mid-stage
- Treatment: Symptomatic only
- Prognosis: Duration of disease is 17-30 years after diagnosis, depending on CAG-repeat length

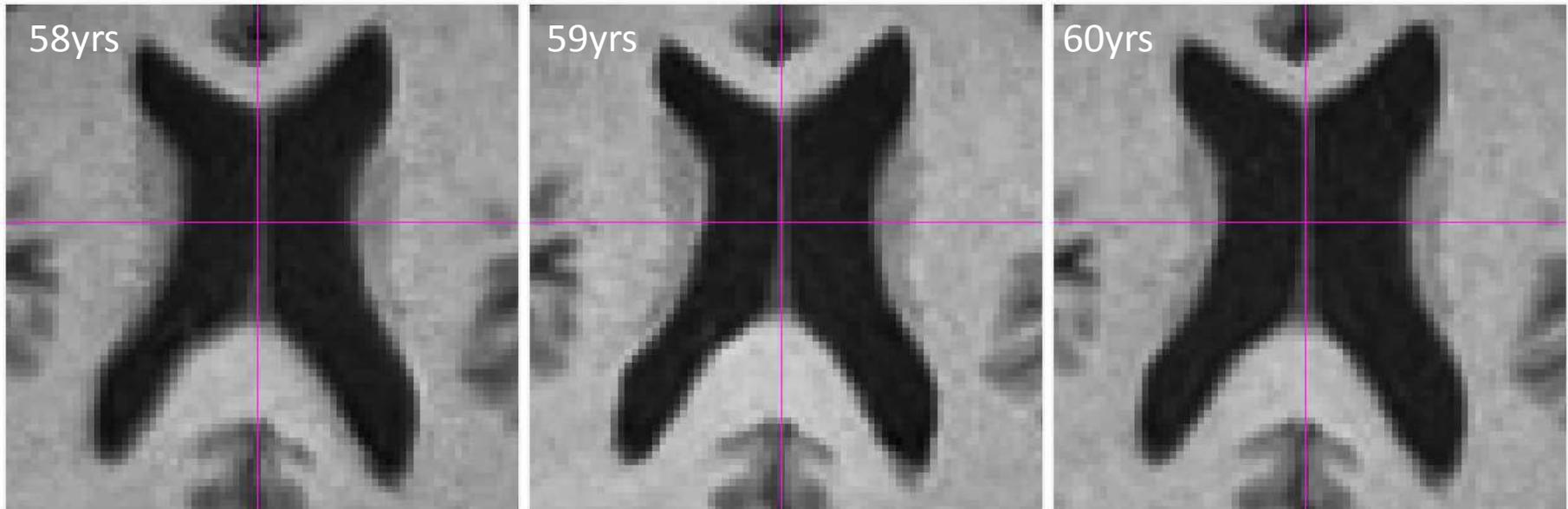


# Purpose: HD treatment

- How can we help HD patients?
  - Present: Symptomatic treatment (no cure)
  - Future: Treatment for pre-symptomatic or **prodromal HD patients** that slow or stop progression **before** debilitating symptoms start
- What do prodromal treatment studies need?
  - Method to **monitor treatment efficacy** when visible symptoms are not present
  - **Solution: Use noninvasive biomarker**
    - Representable on a continuous scale
    - Distinguishes individuals by disease state

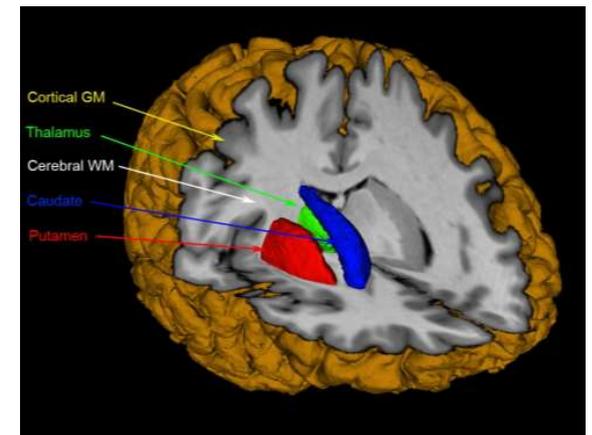


# PREDICT-HD

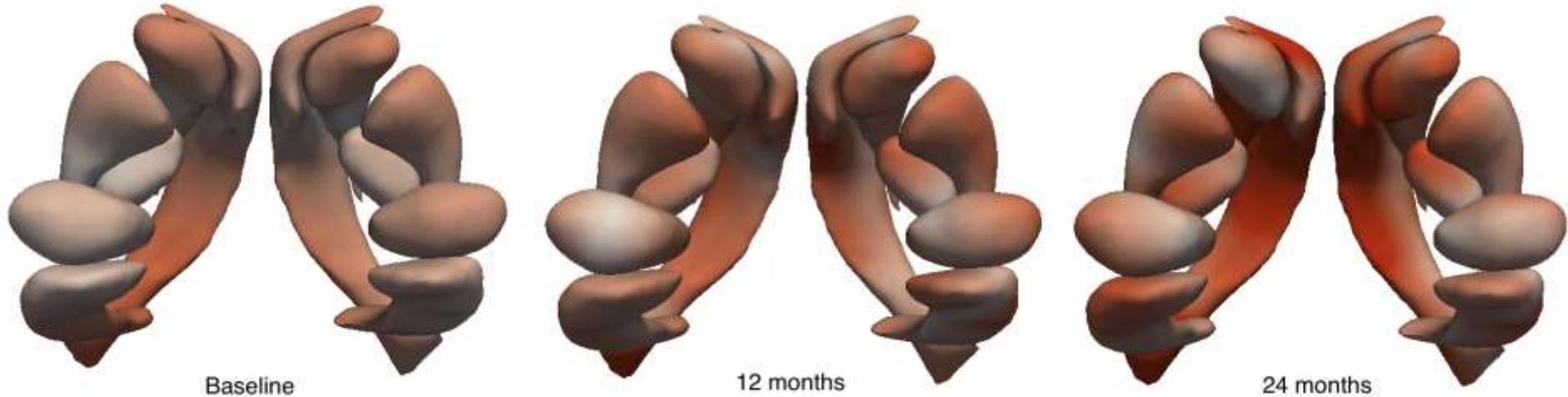


## Huntington's Disease Imaging Study:

- Neurodegenerative, progressive disease
- Longitudinal imaging (MRI)
- Subtle changes over time
- Atrophied caudate and putamen
- Processing: Longitudinal shape regression

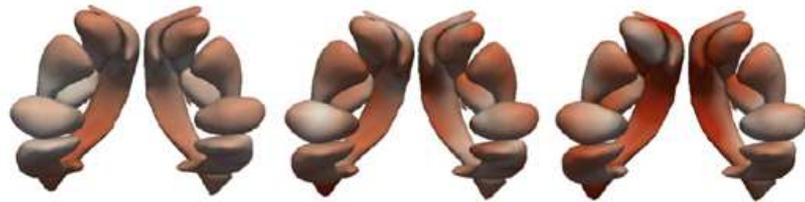


# Huntington's Disease: Joint analysis of sets of anatomical structures



- Data: Iowa Huntington Disease (HD) study (NAMIC)
- Goal: Prediction of onset of HD from longitudinal preclinical imaging

# Clinical Application: Neurodegeneration in Huntington's Disease

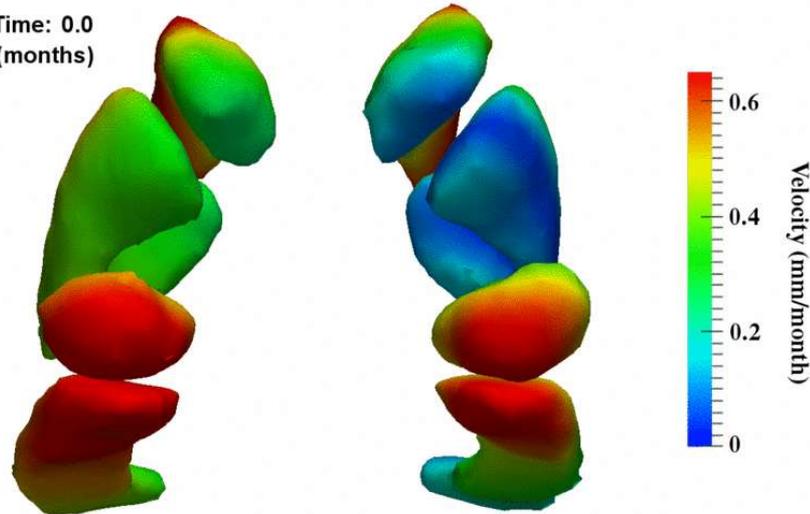


Time point 1

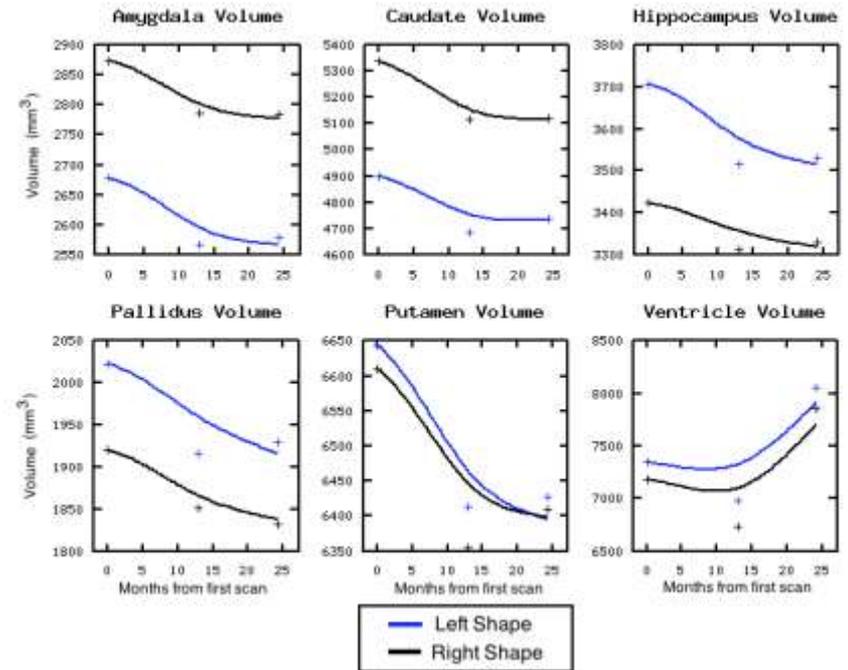
Time point 2

Time point 3

Time: 0.0 (months)

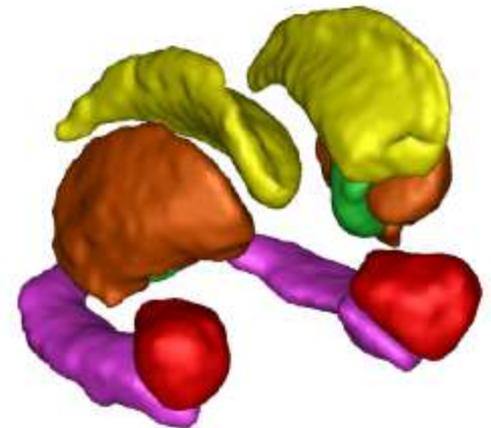
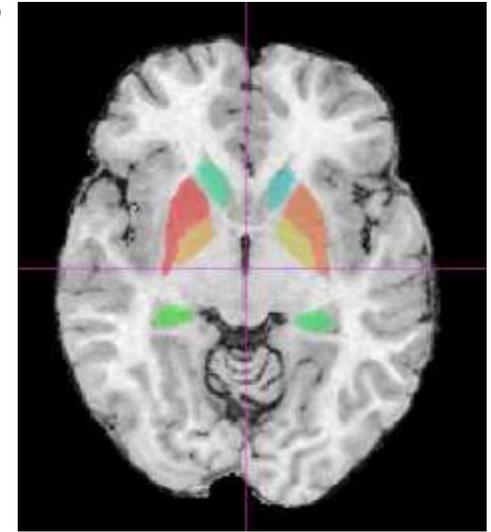
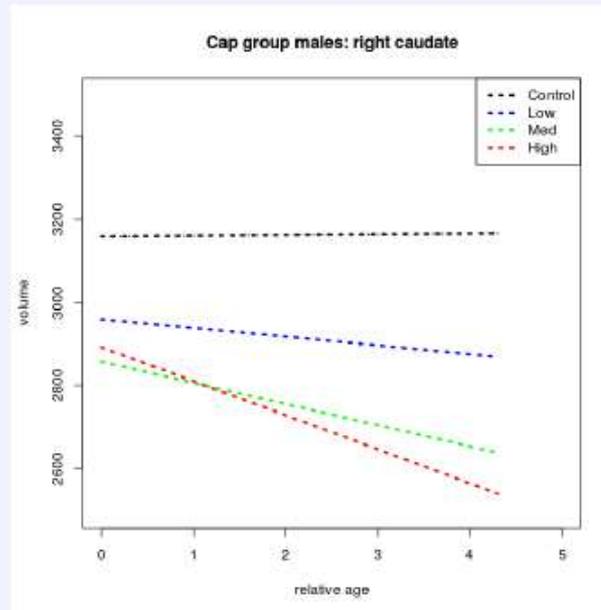
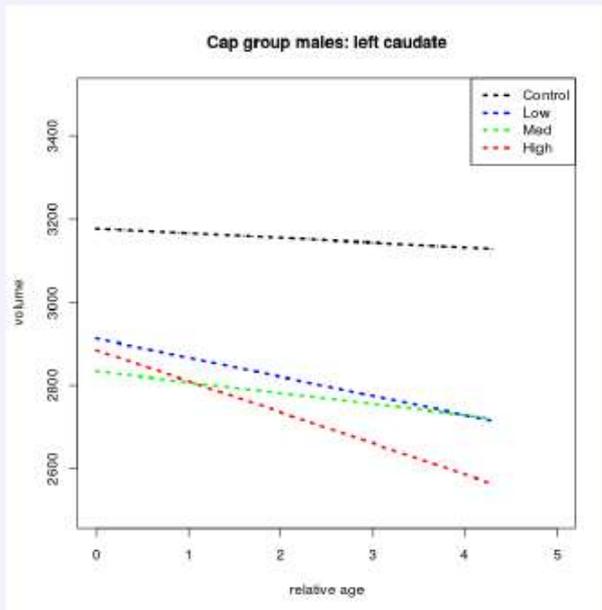


Continuous individual subjects' growth models



Quantitative information derived from 4-D shapes

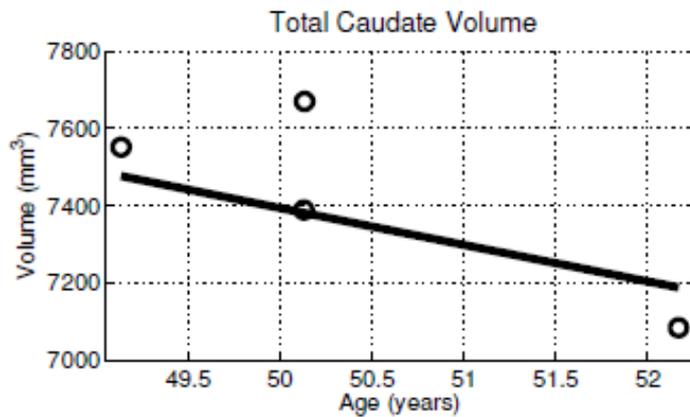
# Degeneration of Caudate Volume by Clinical Risk Groups



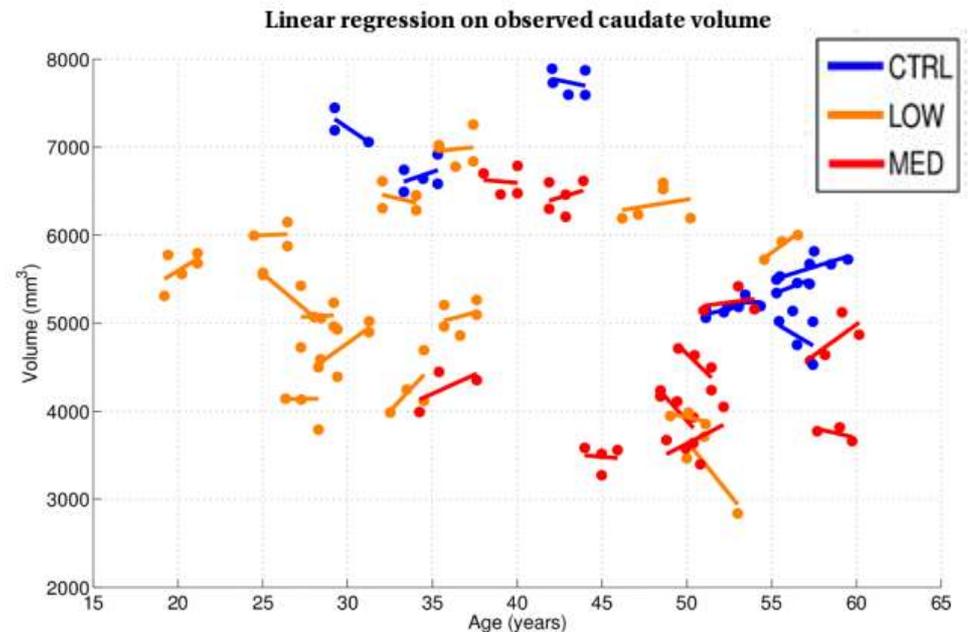
Model:

$$\text{volume} = \beta_0 + \beta_1 (\text{relAge}) + \beta_2 (\text{cap group}) + \beta_3 (\text{relAge} * \text{cap group})$$

# Personalized/Individual Profiles: Problem of Variability in 3D Segmentation



Volumes from one subject



Volumes from multiple subjects with varying disease burden

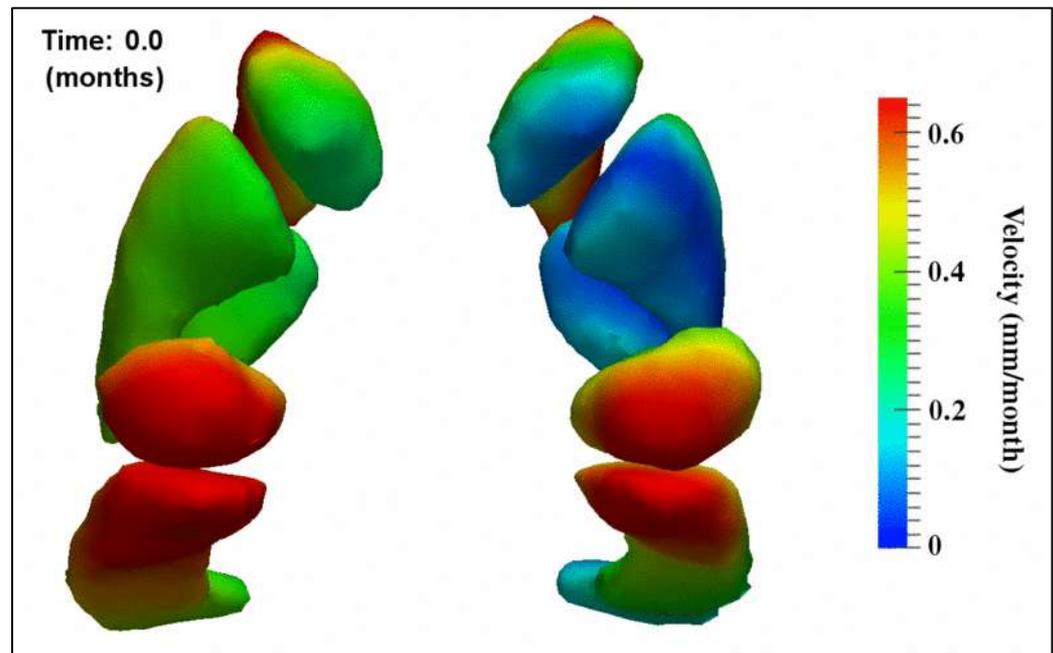
# HD: Joint 4D Modeling of subcortical structures



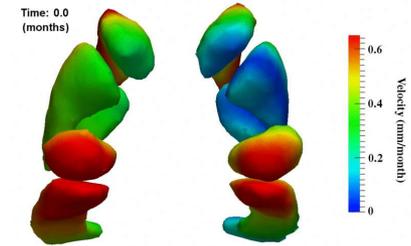
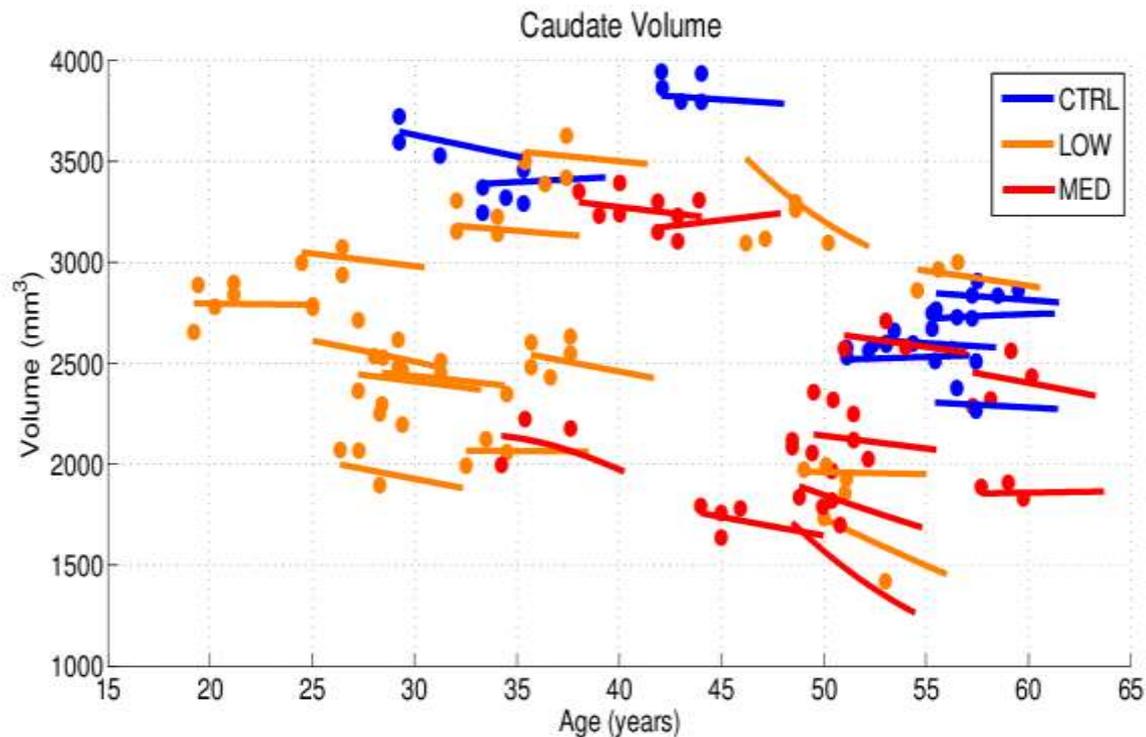
Time point 1

Time point 2

Time point 3



# Subject-Specific Shape Modeling



	CTRL	LOW	MED
Caudate	0.78%	4.22%	6.25%
Hippocampus	0.65%	1.09%	2.18%
Acumben	0.11%	2.13%	3.09%

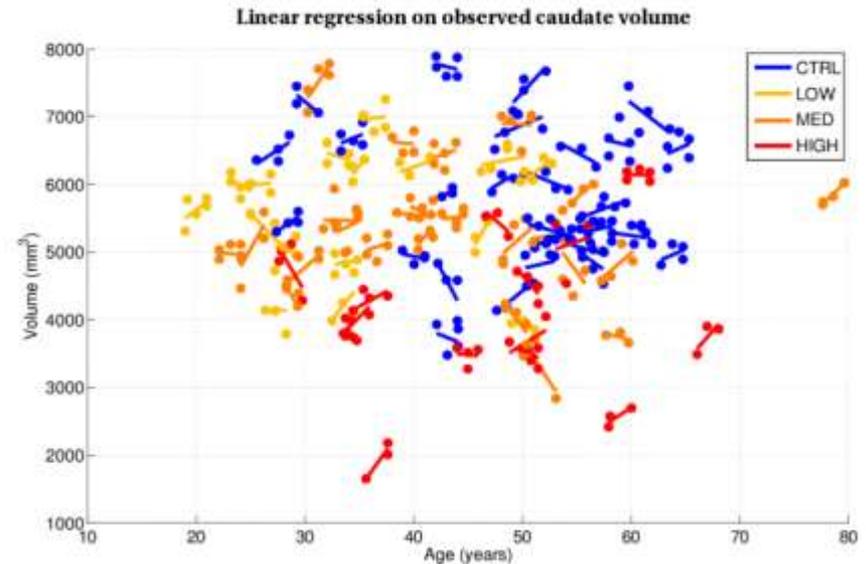
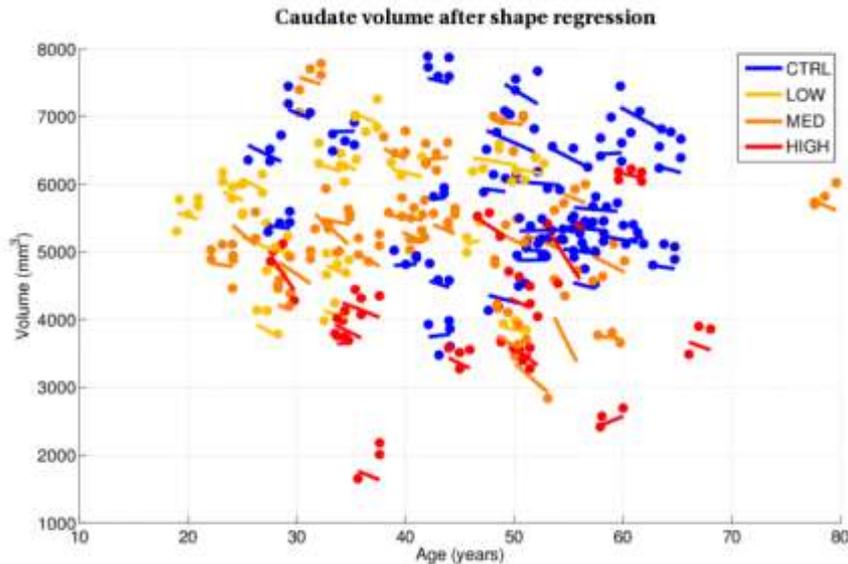
Table 1: Average percentage volume decrease for caudate, hippocampus, and acumben.

- Caudate volume for 32 subjects (3 time pts) extracted after shape regression.
- Observed volumes shown as circles, highlighting the noise in segmentation.
- Our shape regression estimates consistent shape trajectories by considering all shapes simultaneously.
- **Result: Improved subject-specific modeling of neurodegeneration.**

# Longitudinal Segmentation

Huntington's Disease study (30 CTRL, 16 LOW, 24 MED, 14 HIGH)

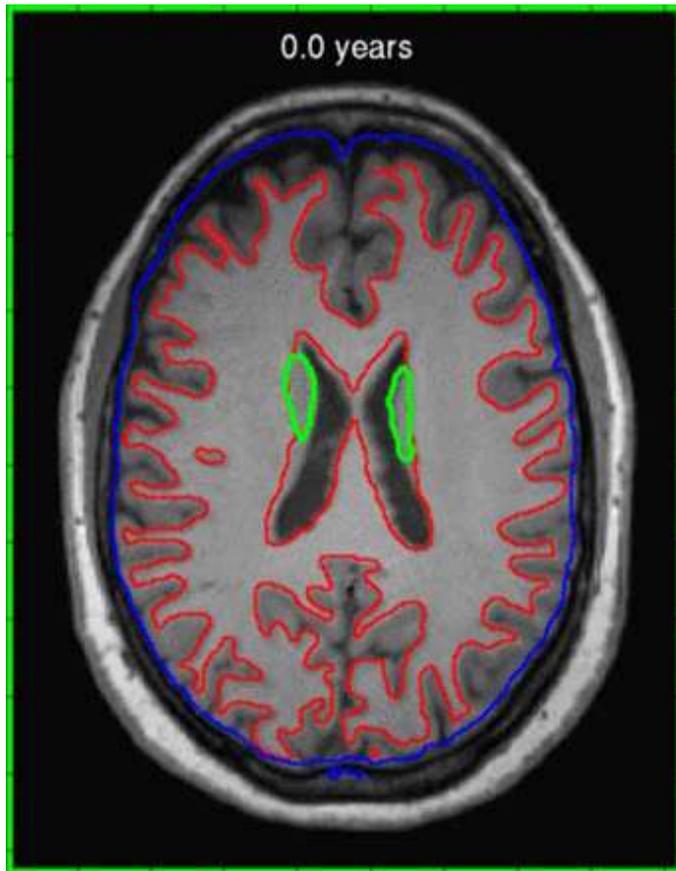
- Models estimated with subcortical shape complexes (12



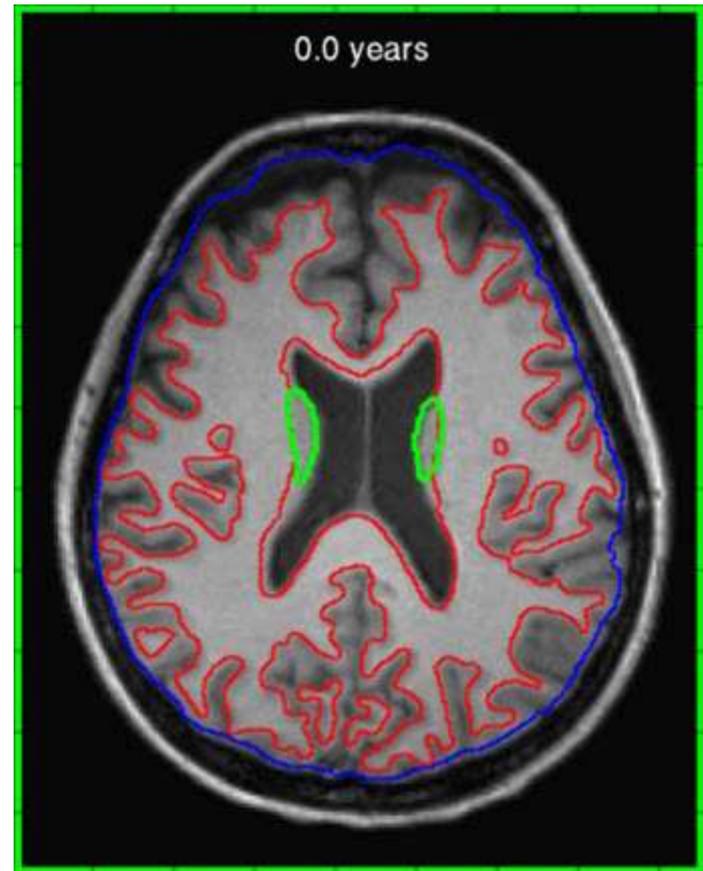
	PERCENT VOLUME CHANGE FROM SHAPE REGRESSION				PERCENT VOLUME CHANGE FROM LINEAR REGRESSION			
	CTRL	LOW	MED	HIGH	CTRL	LOW	MID	HIGH
CAUDATE	-1.41	-2.11	-3.39	-4.84	0.01	1.31	1.00	1.05
PUTAMEN	-3.11	-5.01	-5.42	-6.74	0.29	-0.09	0.06	0.01
HIPPOCAMPUS	-1.55	-1.38	-1.34	-1.55	0.32	0.93	1.23	0.96
THALAMUS	-1.68	-2.47	-1.19	-1.93	0.66	0.49	-0.06	0.40
ACUMBEN	-0.58	-1.52	-1.39	-2.67	-0.04	-2.81	-0.01	1.36
PALLIDUS	-3.82	-5.49	-5.51	-6.76	0.29	-0.25	-0.52	-2.43

# Subject-specific 4-D shape & image regression

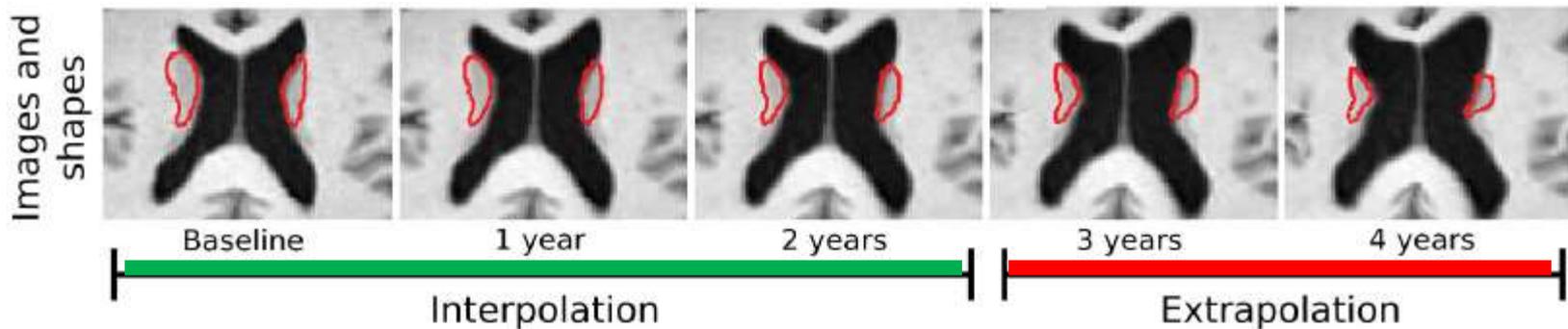
Control 2yrs Interval



Huntington's D. 2yrs Interval



# Huntington's Disease: Joint 4-D Modeling of Shapes and Images



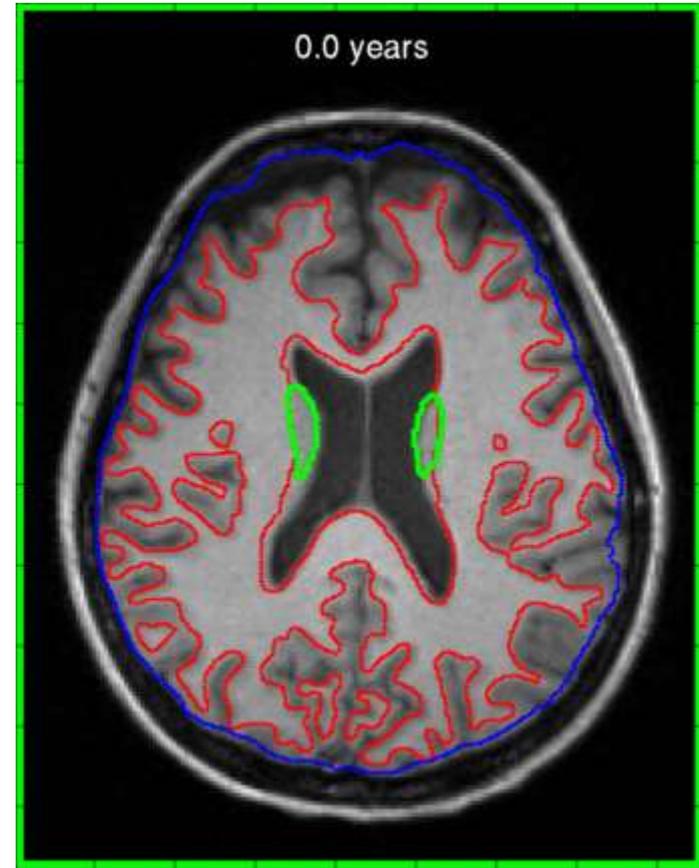
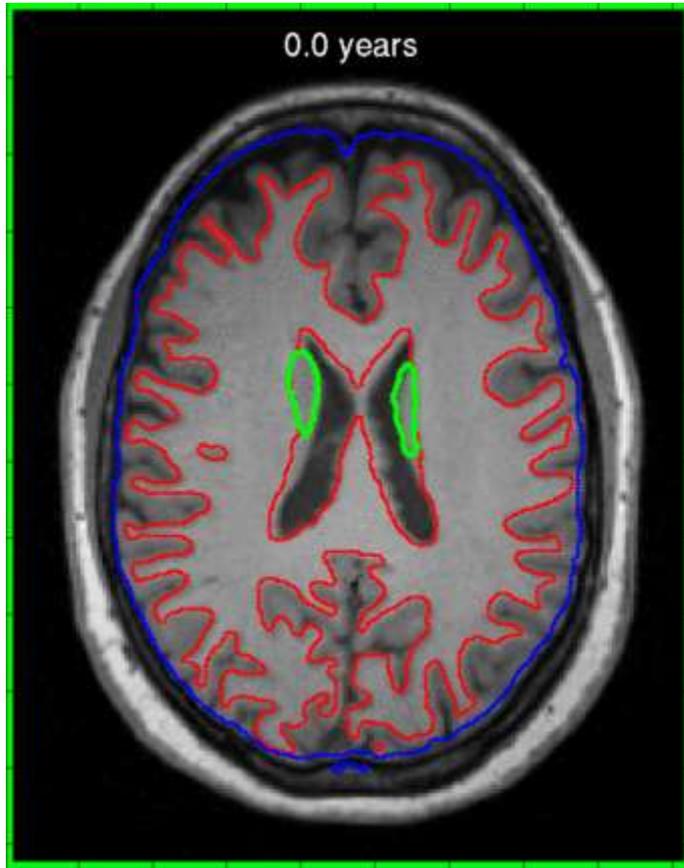
Single subject diagnosed with HD scanned at 58, 59, and 60 years of age.

- T1W images.
- Left/right caudate segmented and manually cleaned.
- Geodesic model can be used to *extrapolate* into the future.

# Work in Progress: Patient-specific 4-D shape & image regression

Control Extrapolated

HD Extrapolated



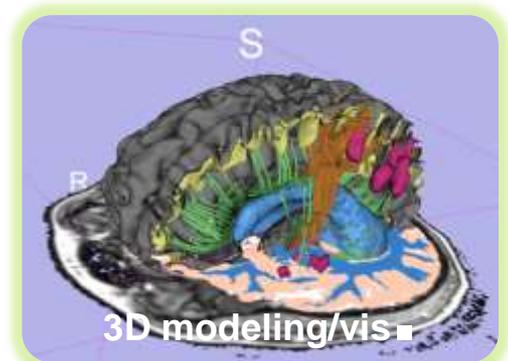
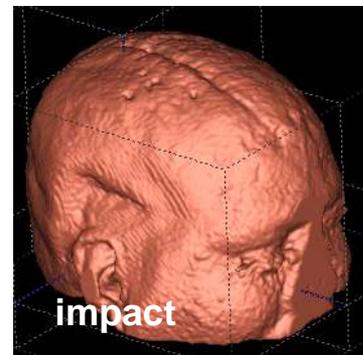
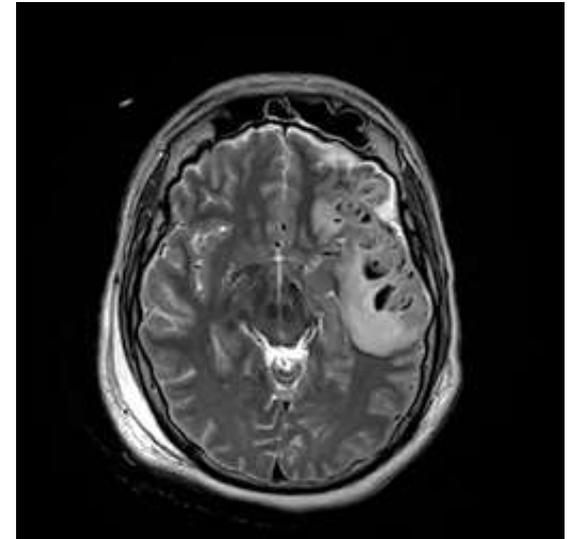
interpolation

extrapolation

time

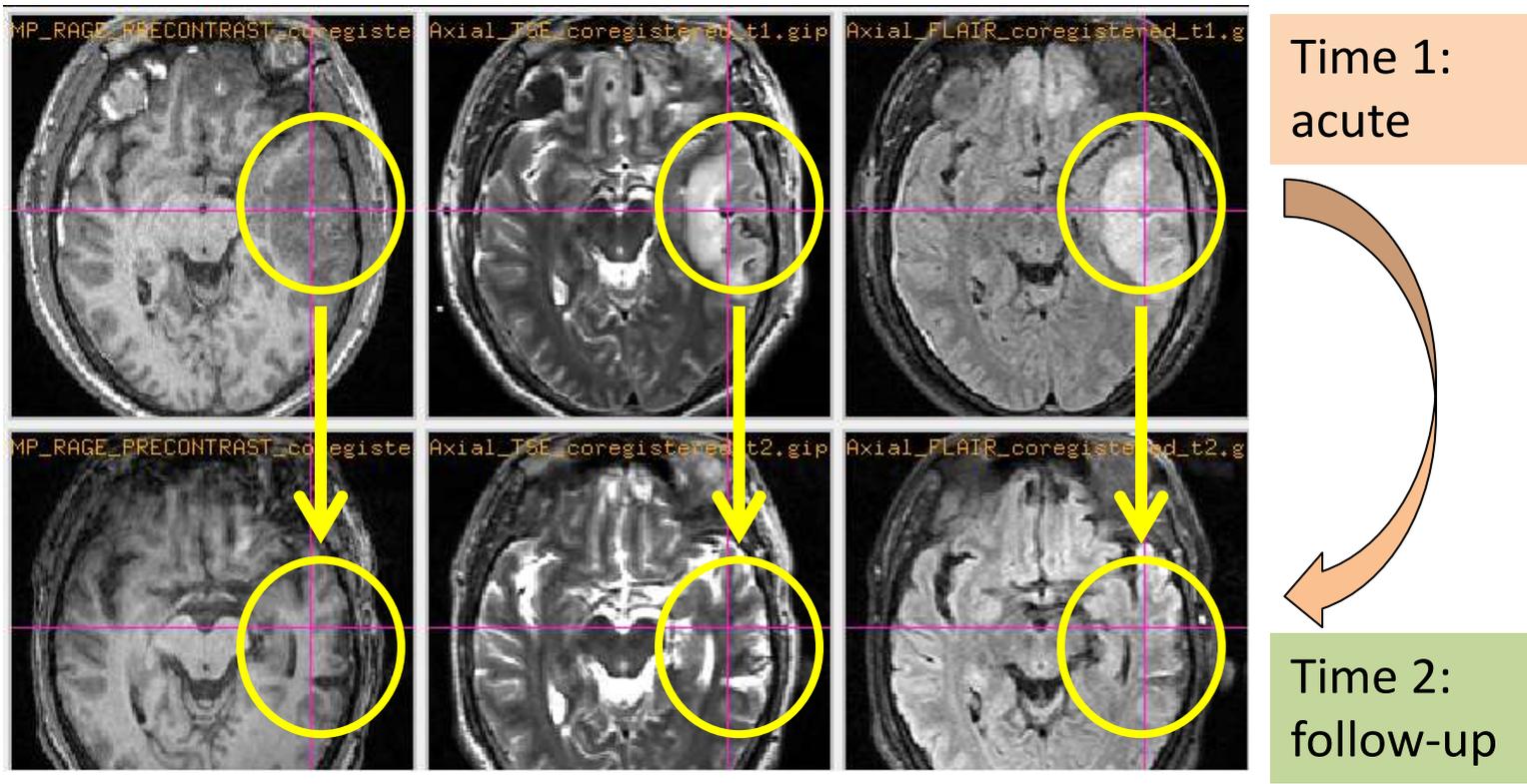
# Traumatic Brain Injury: Patient-specific Modeling of Brain Damage and Recovery

- US: 1.5 Million TBI cases per year, sports, car acc., workplace, veterans, ..
- 650,000 hospitalizations for long-term brain injury: “silent death”.
- **Few treatment options, no proven rehabilitation, only management.**
- **Goal:** Towards rehabilitation experiences that change brain neuroanatomy & function with a reduction/cessation of symptoms.
- Collaboration UCLA TBI, UCLA Neurosurgery, USC LONI, Utah

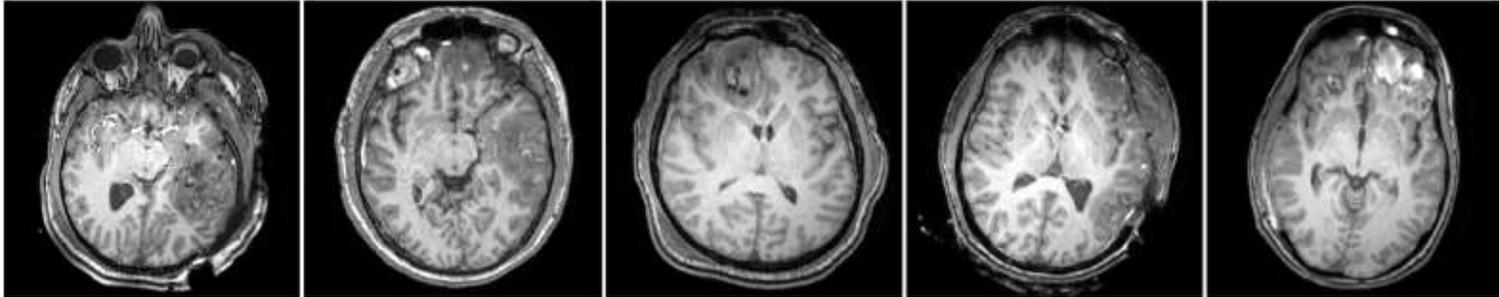


# Multi-contrast & multi-time point image analysis in presence of complex pathology

Change of normal anatomy & lesions over time

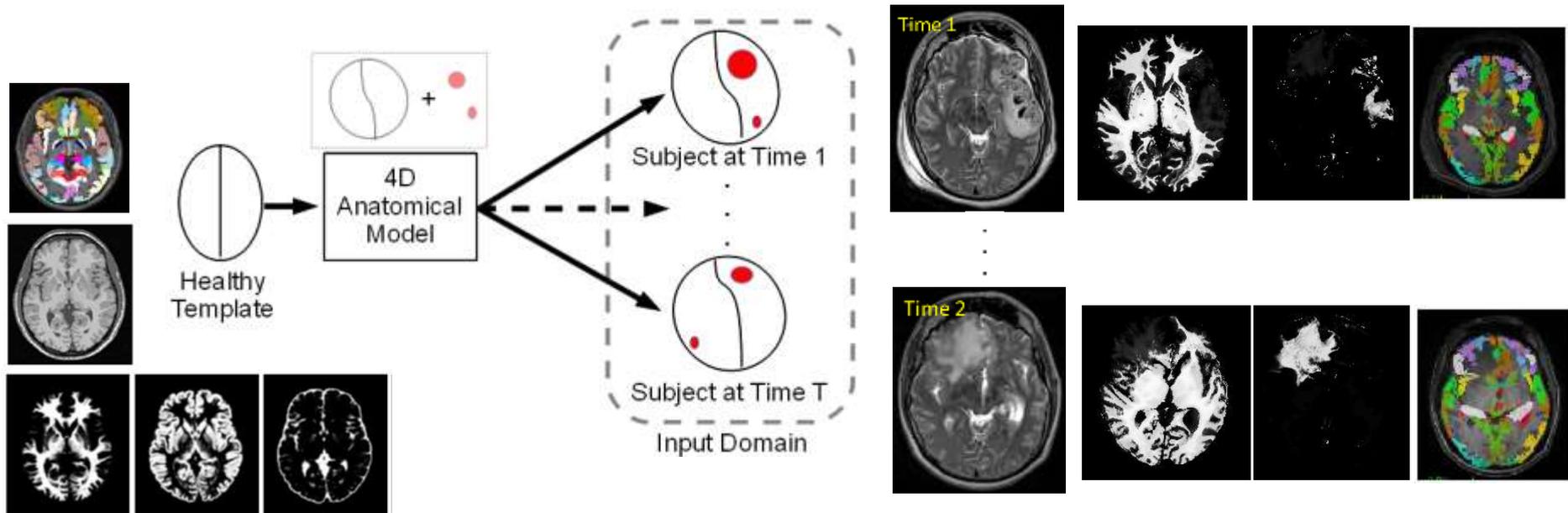


# The “Pathological Anatomy”

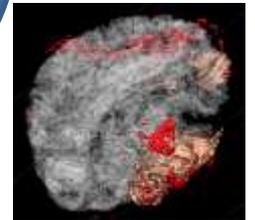


Axial views of acute T1 images of five TBI subjects

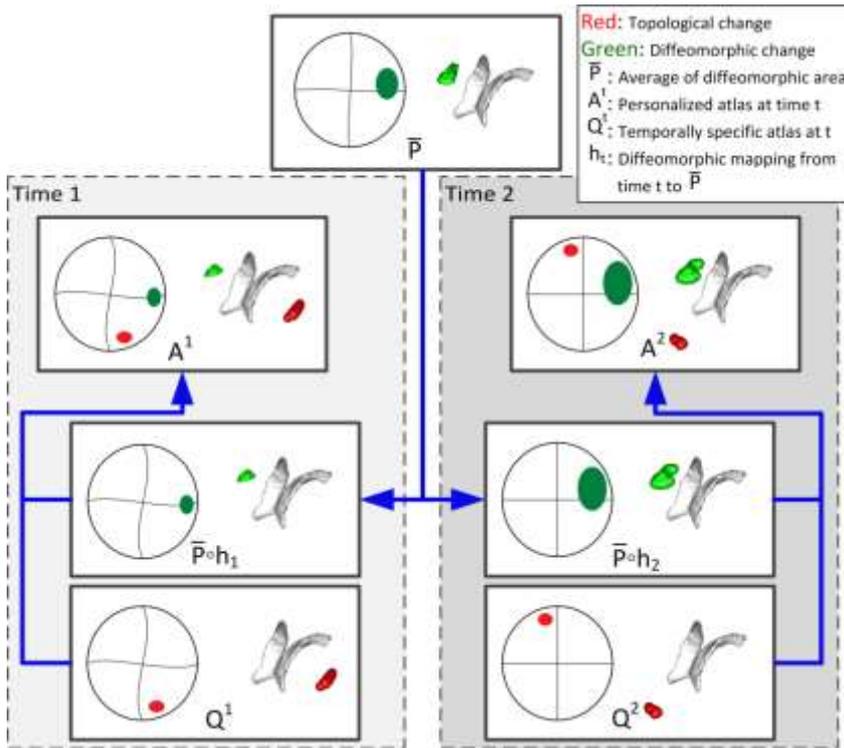
# The “Pathological Anatomy”



Map “pathological images”  
into reference frame of “normals”



# 4D Registration/Segmentation



- Personalized atlas: Smooth subdivision of posteriors into diffeomorphic and non-diffeomorphic regions using the probability of topological change.
- Diffeomorphic component: Temporally global atlas.
- Non-diffeomorphic components: Temporally local pdfs.
- [IEEE ISBI 2012:Wang et al.](#)

The personalized atlas at time point  $t$  is defined as:

$$A^t = (1 - \Gamma^t) \bar{P} \circ h_t + \Gamma^t Q^t.$$

where  $\Gamma^t$  is the probability of topological change.

The personalized atlas construction is formulated as a minimization of the energy function  $\Psi$ :

$$\Psi = \sum_t \left( (1 - \Gamma^t) \| P^t - \bar{P} \circ h_t \|^2 + \Gamma^t \| P^t - Q^t \|^2 + w \| \Gamma^t \|^2 + R(h_t) \right).$$

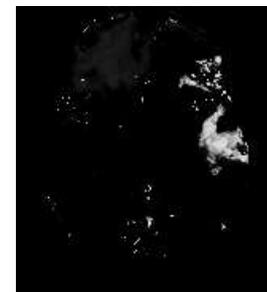
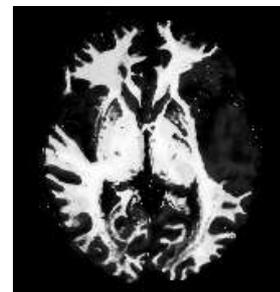
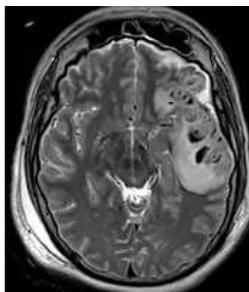
# 4D-PARSeR (Pathological Anatomy Regression via Segmentation and Registration)

- Split diffeomorphic from non-diffeomorphic changes
- Spatial prior  $P_t^c$  for class  $c$  at time point  $t$ :  $P_t^c = A^c \circ \phi_t + Q_t^c$ 
  - $A$  is the tissue class probability
  - $Q_t$ : non-diffeomorphic probabilistic change at time  $t$
  - Subject-specific atlas

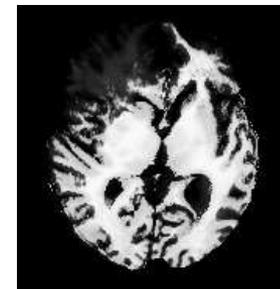
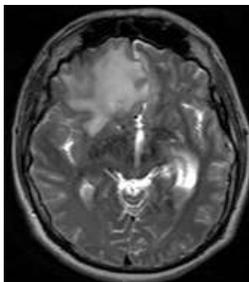


Normative brain template

Time 1



Time X



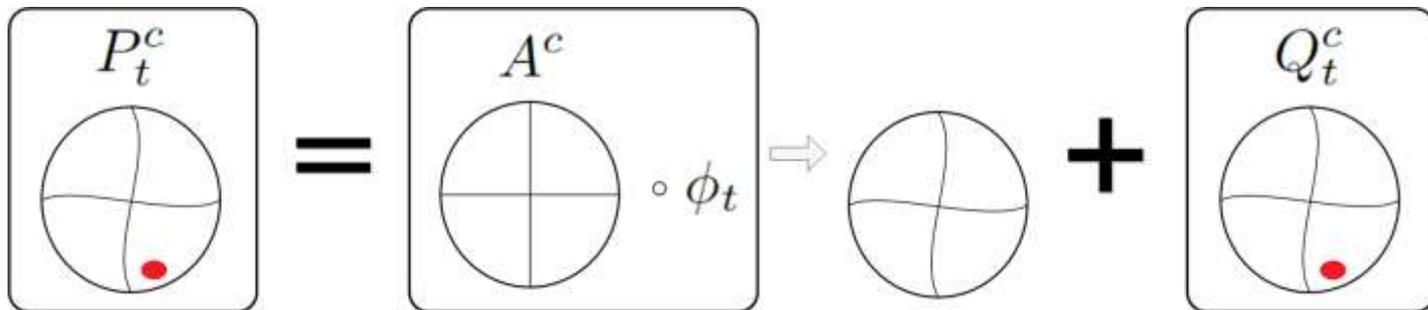
# Spatial Prior

The spatial prior  $P_t^c$  is modeled as:

$$P_t^c = A^c \circ \phi_t + Q_t^c$$

where  $A^c$  is the tissue class probability that is initially associated with the healthy template,  $\phi_t$  is the diffeomorphic deformation from time  $t$  to the atlas, and  $Q_t^c$  is the non-diffeomorphic probabilistic change for time  $t$  (e.g. lesions).

**Concept:**



# Modeling Pathological Anatomy

Given the model and 4D multimodal images  $I_t$  at timepoints  $t$ , we estimate model parameters that minimizes the following functional:

$$\operatorname{argmin}_{A, \phi_t, Q_t, \theta_t} \mathcal{F}(A, \phi_t, Q_t, \theta_t) + \mathcal{R}_1(Q) + \mathcal{R}_2(A) + \mathcal{R}_3(\phi)$$

where  $\mathcal{F}$  is data functional (negative total log-likelihood):

$$\mathcal{F}(A, \phi_t, Q_t) = - \sum_{t=1}^T \sum_{x=1}^N \log \left( \sum_{c=1}^C P_t^c(x) p(I_t(x)|c, \theta_t^c) \right)$$

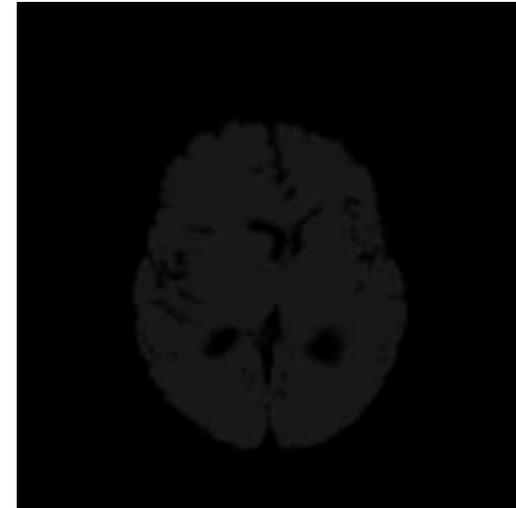
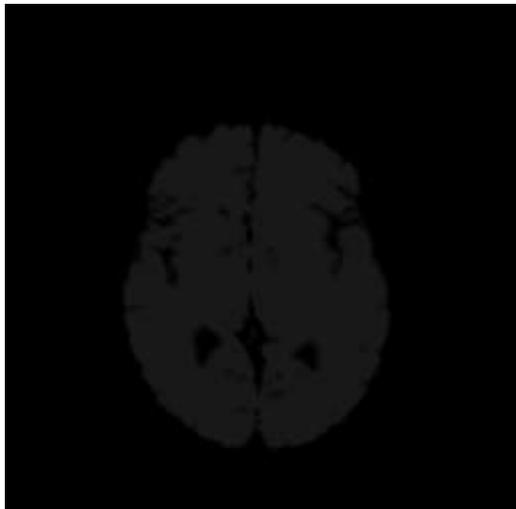
where  $P_t^c$  is spatial prior,  $\mathcal{R}$  represents the regularity terms. User input or **domain adaptation** can be used to initialize data likelihood.

# Pathological Anatomy Regression

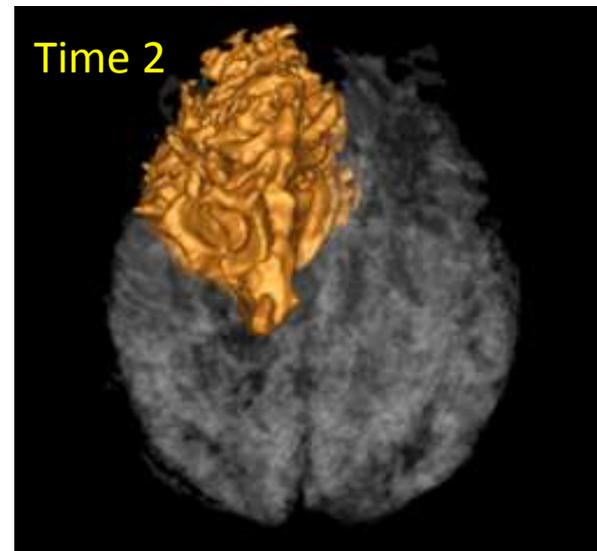
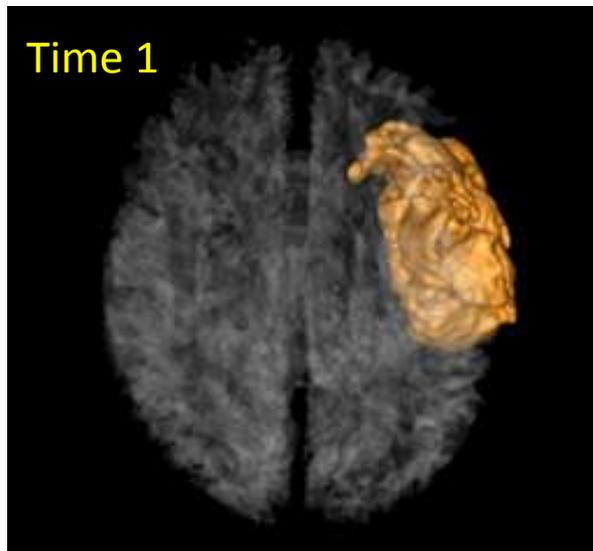
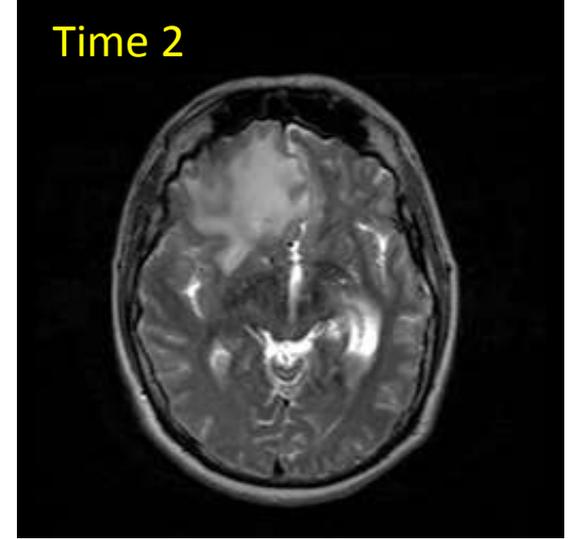
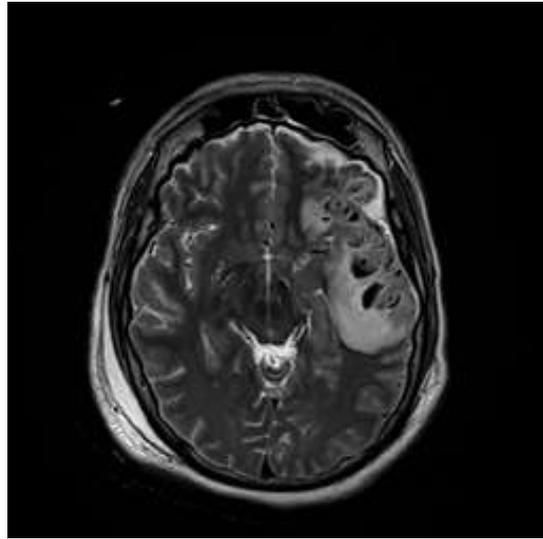
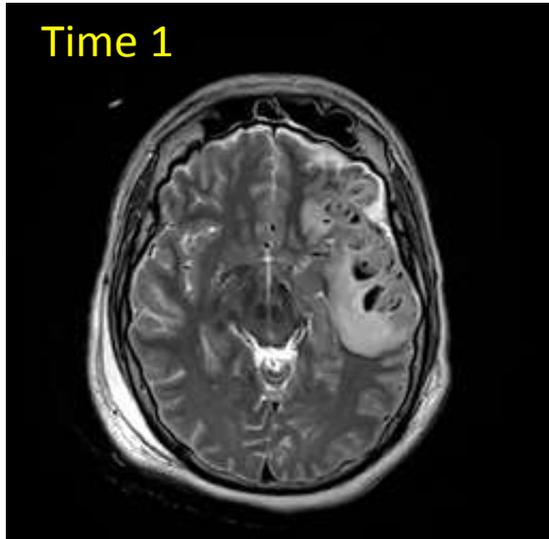
Time 1



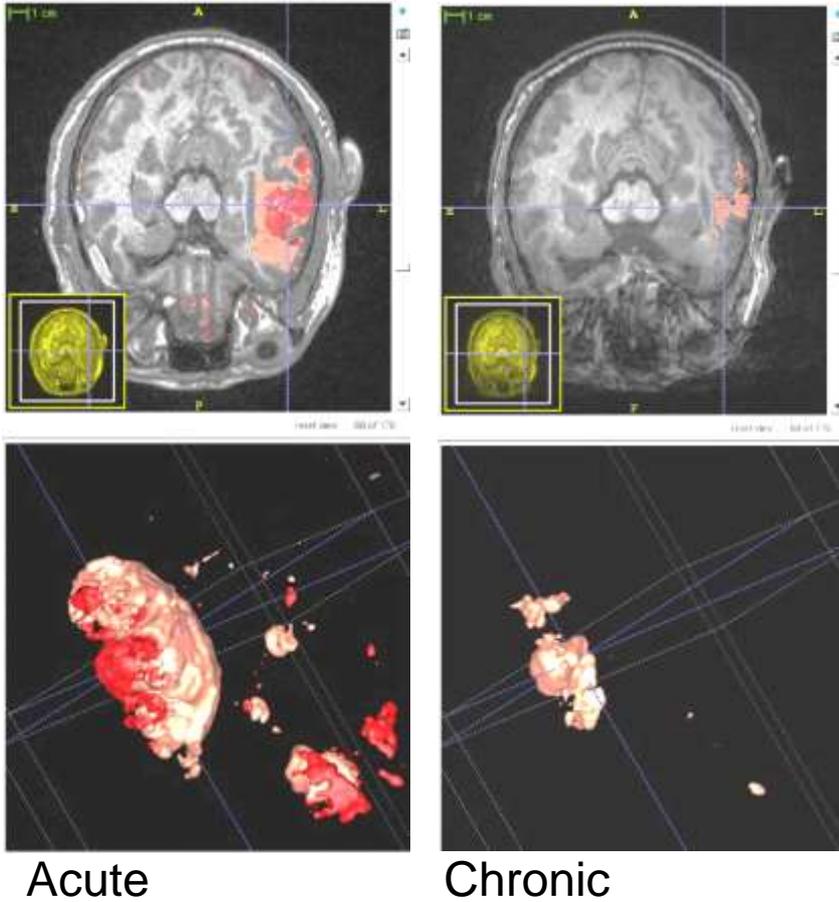
Time 2



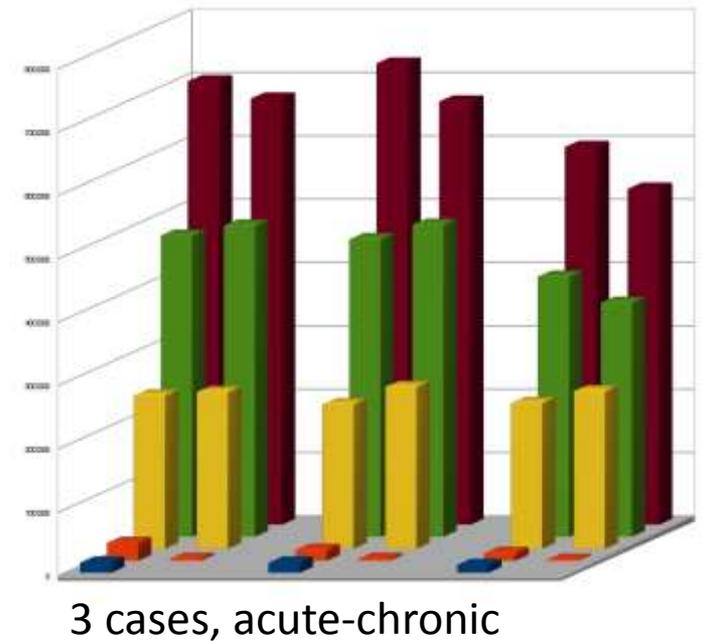
# TBI Case (UCLA)



# Quantitative Results 4-D TBI Imaging



- Hemorrhagic lesion
- Non-hemorrhagic lesion
- Cerebrospinal fluid (CSF)
- White matter (WM)
- Grey matter (GM)



# Conclusions

- Spatio-temporal Image & Shape Analysis: Emerging field:
  - Multidisciplinary by definition.
  - Actively developing field driven by new imaging technologies and novel biomedical driving problems.
  - Challenging fundamental, algorithmic and statistical problems.
  - Research progress enables new scientific discoveries.
- Clinically highly relevant for quantitative analysis of subject-specific, personalized changes due to disease or therapy.
- **Main take home message:** Longitudinal image data significantly benefits from 4-D processing and modeling.
- **Todo:** Integrate geometrical with physiological & functional modeling (N.Ayache et al., P. Hunter et al.).

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- **NIH-NIBIB:** 2U54EB005149-06 , NA-MIC: National Alliance for MIC
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- **NIH NIBIB 1R01EB014346-01:** ITK-SNAP
- **NIH NINDS R01 HD067731-01A1:** Down's Syndrome
- **NIH P01 DA022446-011:** Neurobiological Consequences of Cocaine Use
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- Maria Escolar, Children's, Pittsburgh



# Freely available Software

**ExoshapeAccel:** C/C++ NAMIC toolkit SW for estimating continuous evolution from a discrete collection of shapes,  
James Fishbaugh [Public download](#)



*Deformetrica*

Stanley Durrleman

<http://www.deformetrica.org/>

